

# Diffusion MRI: Lecture 1 of 2

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Today

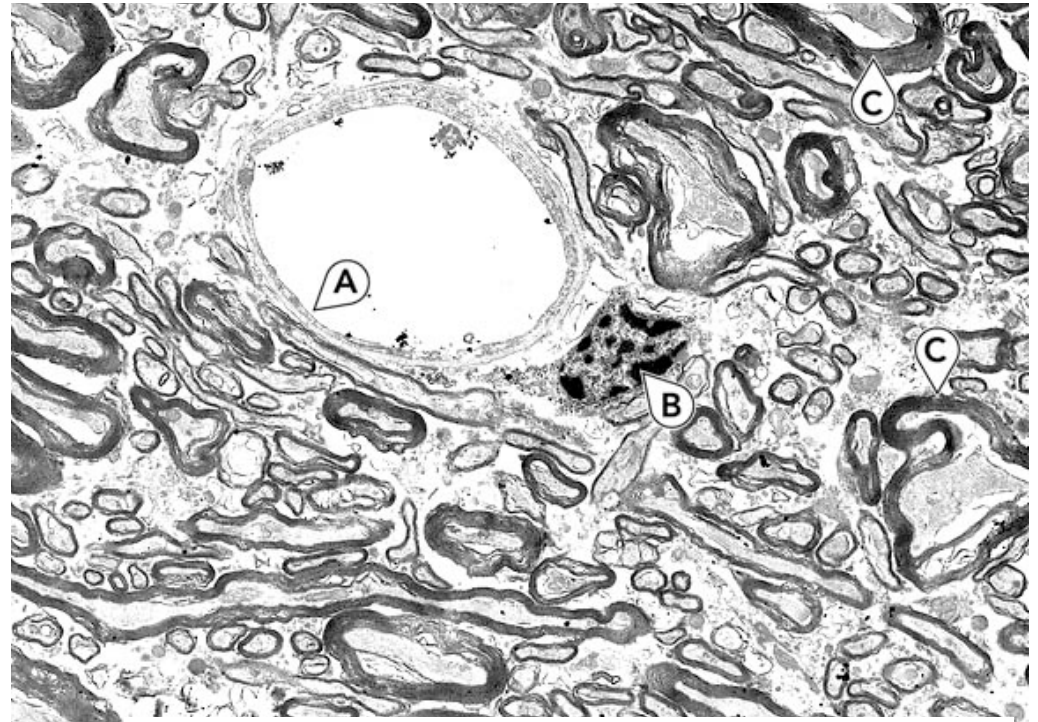
- Diffusion MRI: a marker of tissue microstructure.
- What is diffusion and how do we model it?
- Sensitizing the MRI signal to diffusion.
- Diffusion MRI signal equations.
- Mapping diffusion coefficients.
- Effects of motion.
- Eddy currents.



# Diffusion MRI: a marker of tissue microstructure

- Patterns of water diffusion in tissue reflect the tissue microstructure .

- membranes
- permeability of membranes
- macromolecules
- packing density
- compartment sizes



Darwin, M. et. al. 1995.

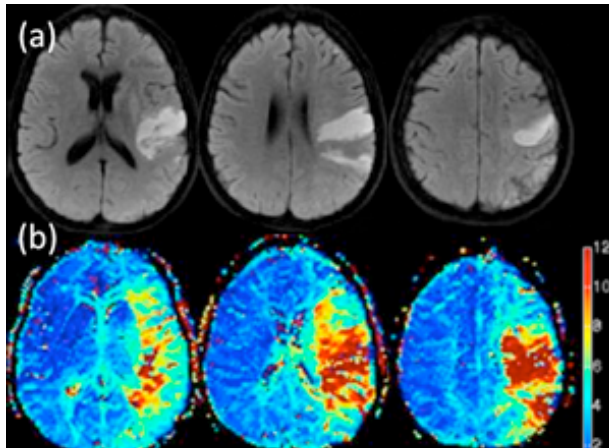
- Sensitizing the MRI signal to water diffusion is a way to indirectly get information about tissue microstructure.

# Diffusion MRI in the Brain

## Clinical Applications

Stroke

*Diffusion*



*Perfusion*

Zaharachuk G, et. al. 2012.

Intracranial Infections

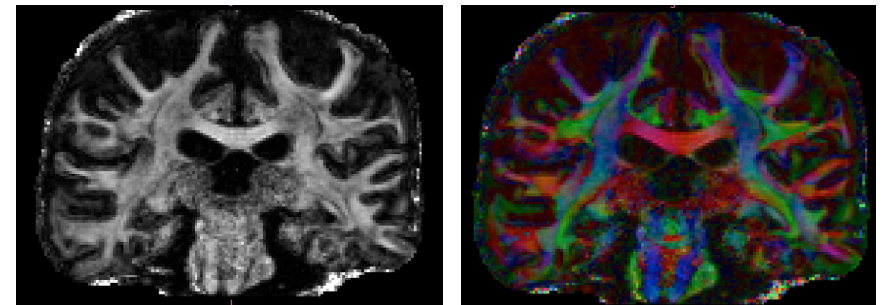
Brain Tumours

Trauma

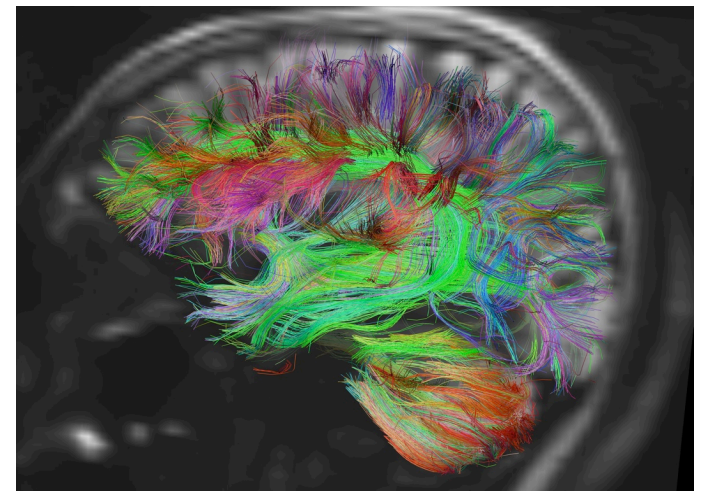
Edema

## Neuroscience

White Matter Pathways

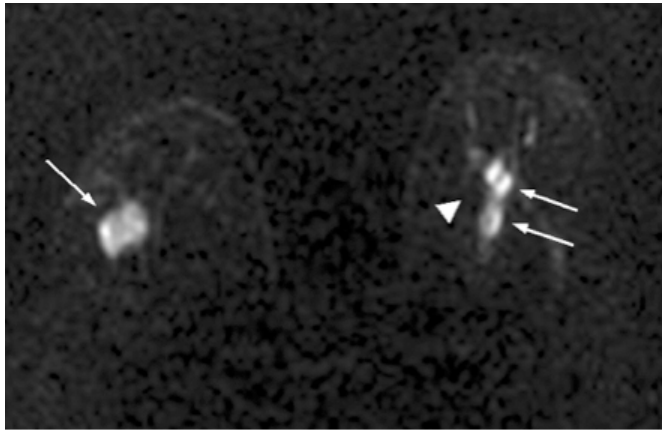


Structural Connectivity



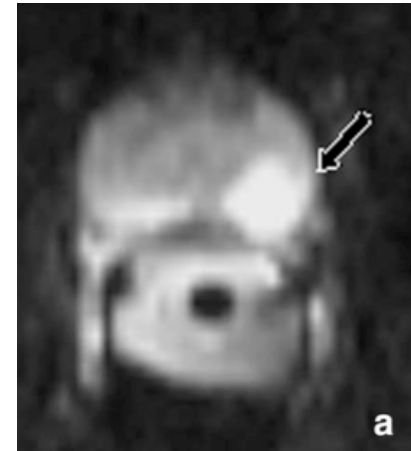
# Diffusion MRI in the Body

## Breast



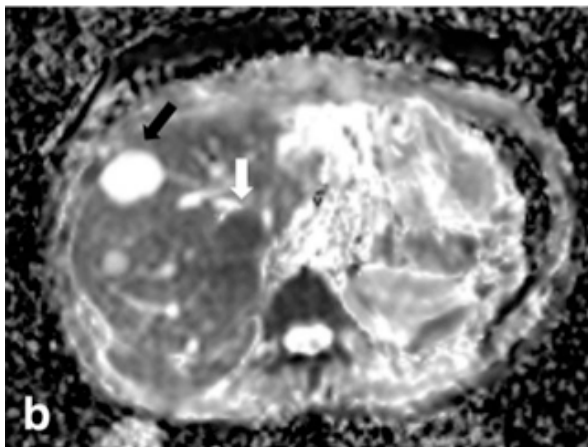
Park M-J et. al. 2007

## Prostate



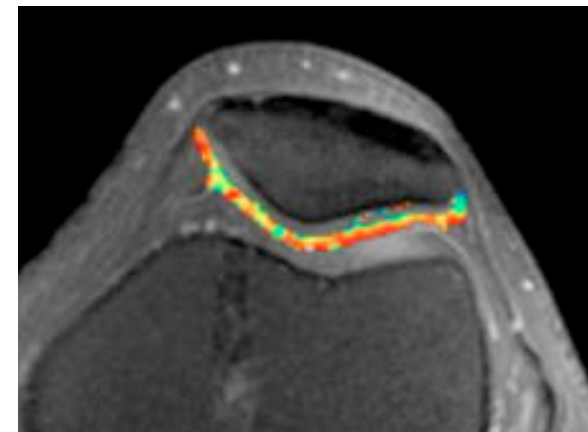
Bonekamp S, et. al. 2012

## Liver



Bonekamp S, et. al. 2012

## Musculoskeletal



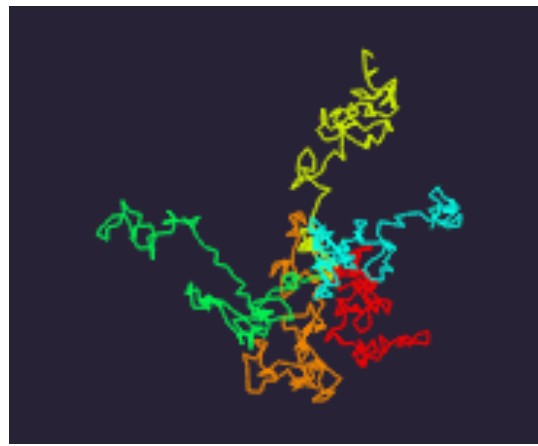
Staroswiecki E, et. al. 2012



# What is diffusion?

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- The result of random collisions between molecules in liquids and gases.
- A form of passive transport that causes mixing but no bulk motion.
- A spontaneous, random process.



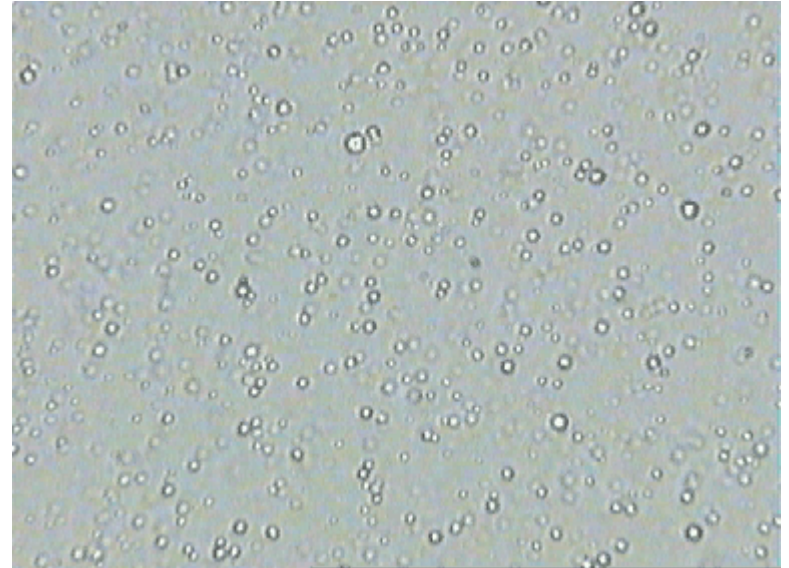
# Observation of Diffusion

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Robert Brown  
1828



Brownian Motion



Film Clip Courtesy of  
Dave Walker.

# Fick's First Law

Adolf Fick

1855

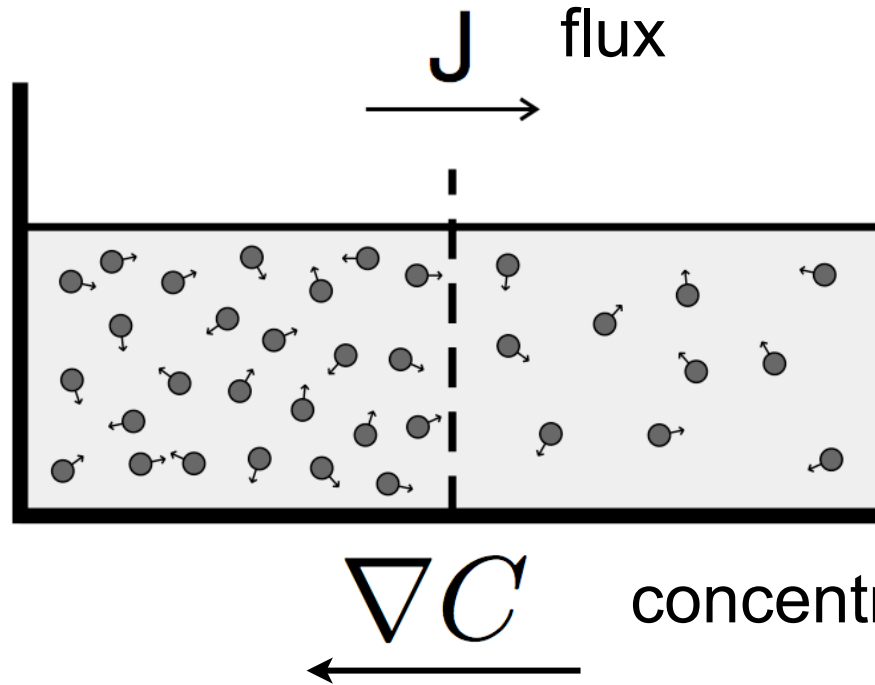


Diagram: Diffusion  
MRI textbook,  
Johansen-Berg and  
Behrens.

Flux of particles is proportional to concentration gradient.

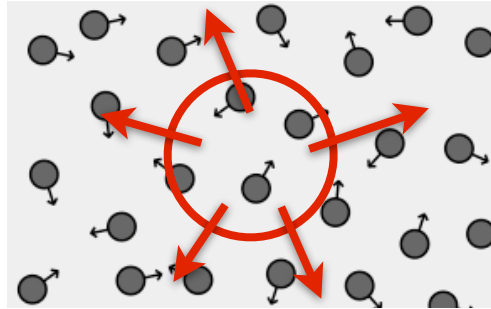
$$J = -D \nabla C$$

from high concentration to low concentration  
diffusion coefficient



# Fick's Second Law

Adolf Fick  
1855



**For an elemental volume:**

Rate of change in concentration is equal to the net flux across its boundaries.

$$\frac{\partial C}{\partial t} = -\nabla \cdot J$$

$(J = -D\nabla C)$





# Diffusion Equation

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Adolf Fick

1855



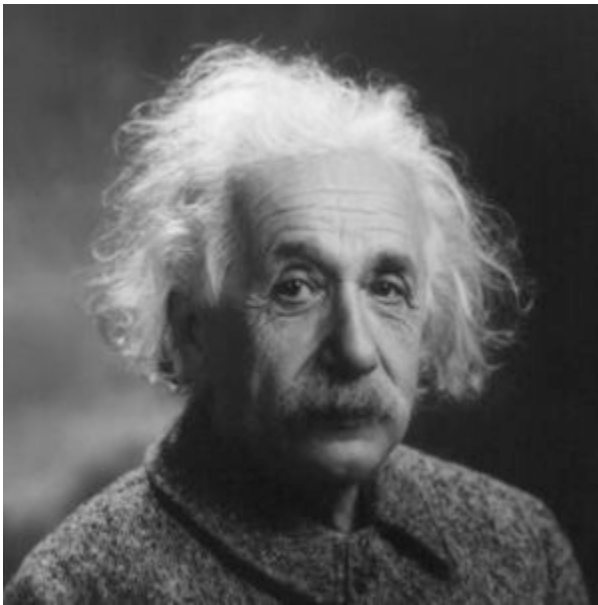
$$\frac{\partial C}{\partial t} = D \nabla^2 C$$

# Self-Diffusion and Probabilities

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Albert Einstein

1905

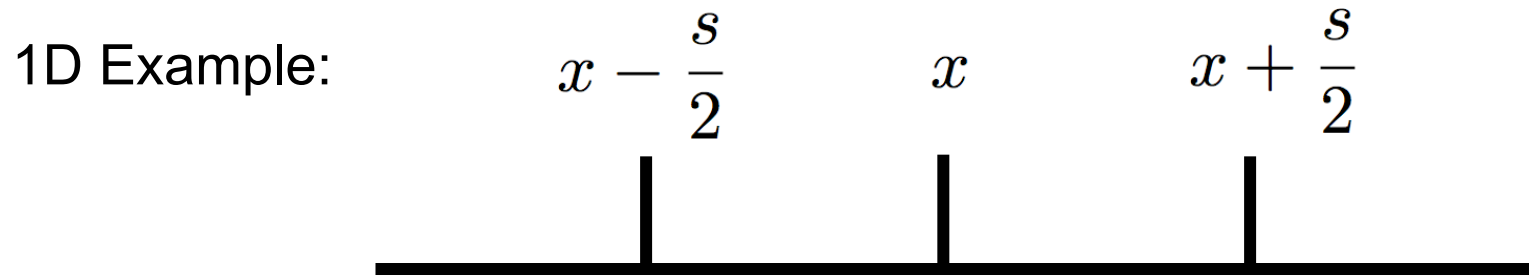


- Fick's Laws describe particles drifting from higher to lower concentration (*mutual diffusion*).
- Einstein applied the same idea to the case without a macroscopic concentration gradient (*self-diffusion*).
- Einstein ascribed Fick's Laws an interpretation based on probabilities.



# Diffusion as a Random Walk

At each time-point,  $\tau$ , a molecule moves a distance “s” in a random direction.



Particle concentration at point  $x = C(x)$

$$J^+ = \frac{s}{\tau} \frac{C(x - \frac{s}{2})}{2} \quad J^- = \frac{s}{\tau} \frac{C(x + \frac{s}{2})}{2} = \frac{s}{\tau} \frac{C(x - \frac{s}{2}) + s \frac{dC}{dx}}{2}$$

Net Flux:  $J = J^+ - J^- = \frac{s^2}{2\tau} \frac{dC}{dx}$

Einstein Relation

Recall Fick's Law:  $J = -D \frac{dC}{dx}$

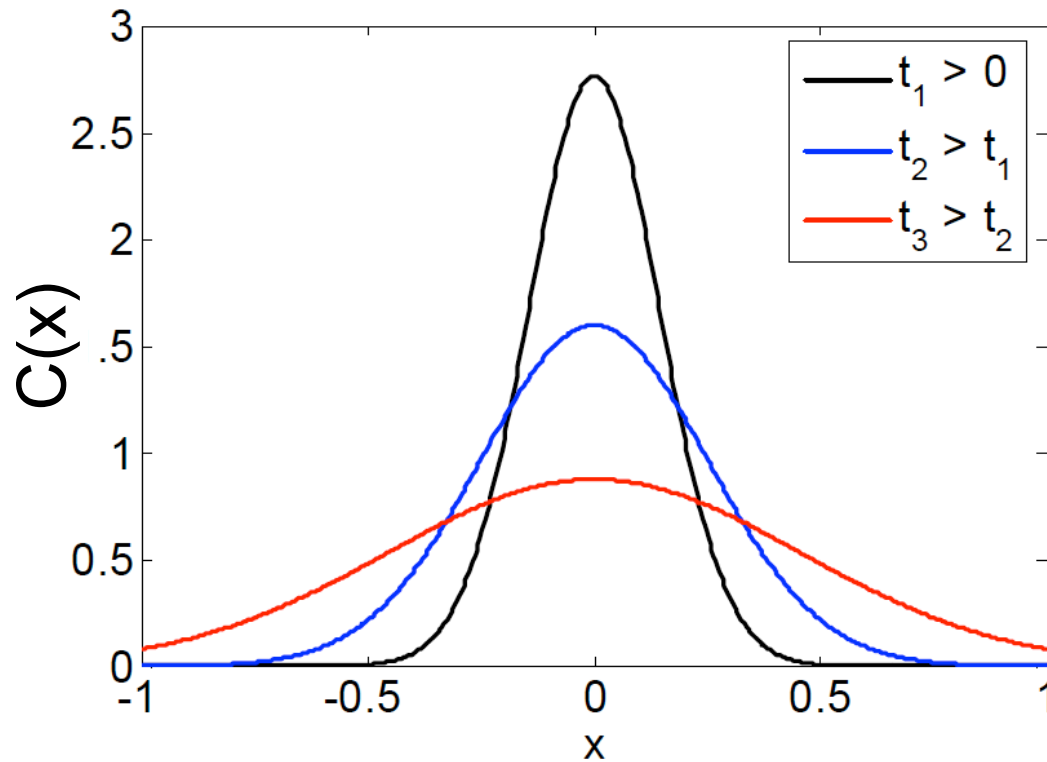
Thus,  $D = \frac{s^2}{2\tau}$

$s^2 = 2Dt$



# Gaussian Spread of Particles

Mean squared displacement given by the Einstein relation can also be interpreted as the variance of the spread of positions after a period of time.



$$\sigma^2 = 2Dt$$

For  $n$  dimensions :

$$\sigma^2 = 2nD\Delta$$



# Solving the Diffusion Equation

The Diffusion Equation: 
$$\frac{\partial C}{\partial t} = D \nabla^2 C$$

For boundary condition, for all times:  $C(x, t) \rightarrow 0$  as  $x \rightarrow \pm\infty$

initial condition:  $C(x, 0) = \delta(x)$

**Gaussian Function:**

solution: 
$$C(x, t) = \frac{1}{\sqrt{2\pi\sigma^2}} \exp\left(-\frac{x^2}{2\sigma^2}\right)$$

with:  $\sigma^2 = 2Dt$  ← Einstein Relation

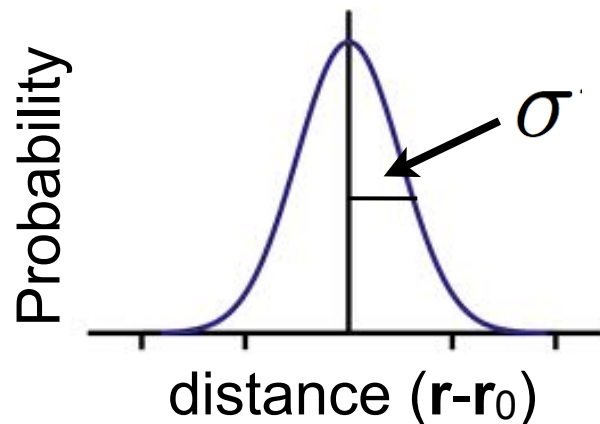




# Diffusion Propagator

Gaussian function can be used to determine probability of a particle being displaced from  $\mathbf{r}_0$  to  $\mathbf{r}$  in time  $t$ .

$$P(\mathbf{r}_0|\mathbf{r}, t) = \frac{1}{\sqrt{2\pi\sigma^2}} \exp\left(-\frac{(\mathbf{r} - \mathbf{r}_0)^2}{2\sigma^2}\right)$$

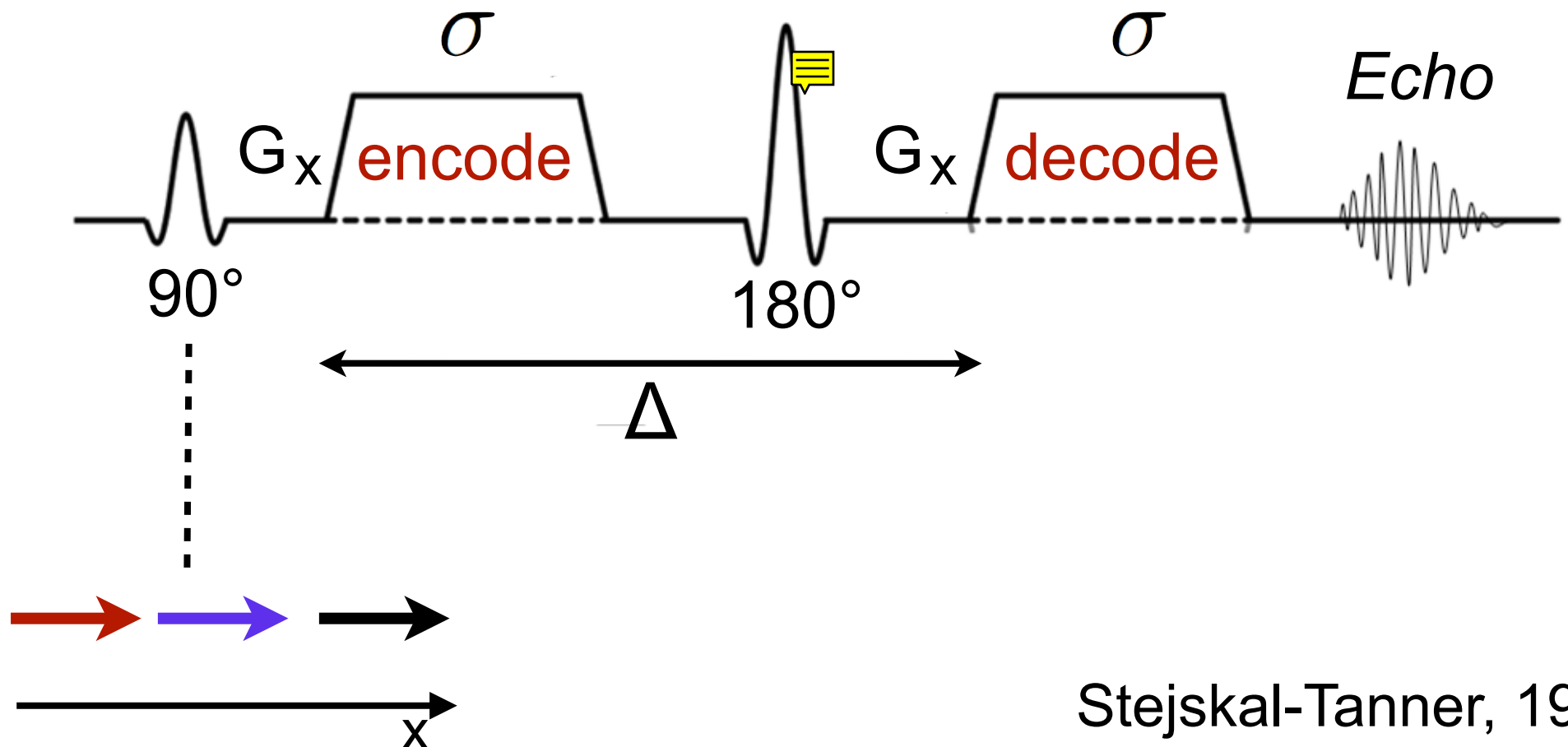


$$\sigma^2 = 2nD\Delta$$

# Sensitizing the MRI Signal to Diffusion

Hahn 1950.  
Carr and Purcell 1954.

## Case #1: Without Diffusion Weighted Spin Echo

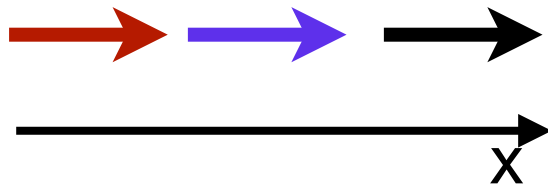
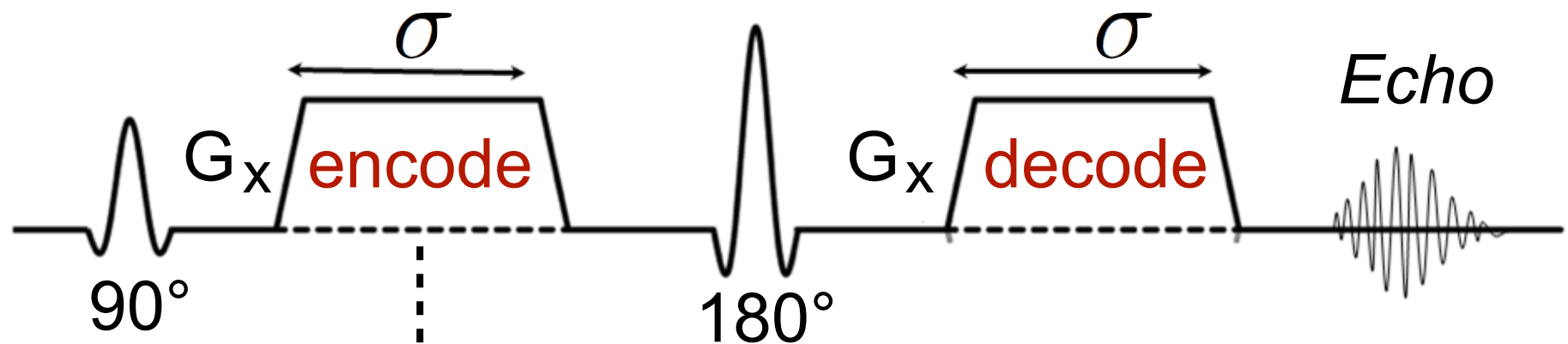


Stejskal-Tanner, 1965.



# Sensitizing the MRI Signal to Diffusion

## Case #1: Without Diffusion



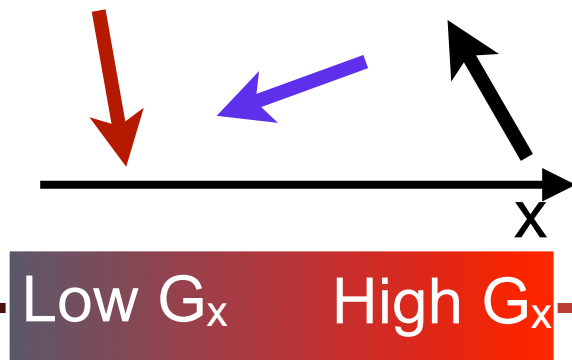
Low  $G_x$  High  $G_x$

Stejskal-Tanner, 1965.



# Sensitizing the MRI Signal to Diffusion

## Case #1: Without Diffusion

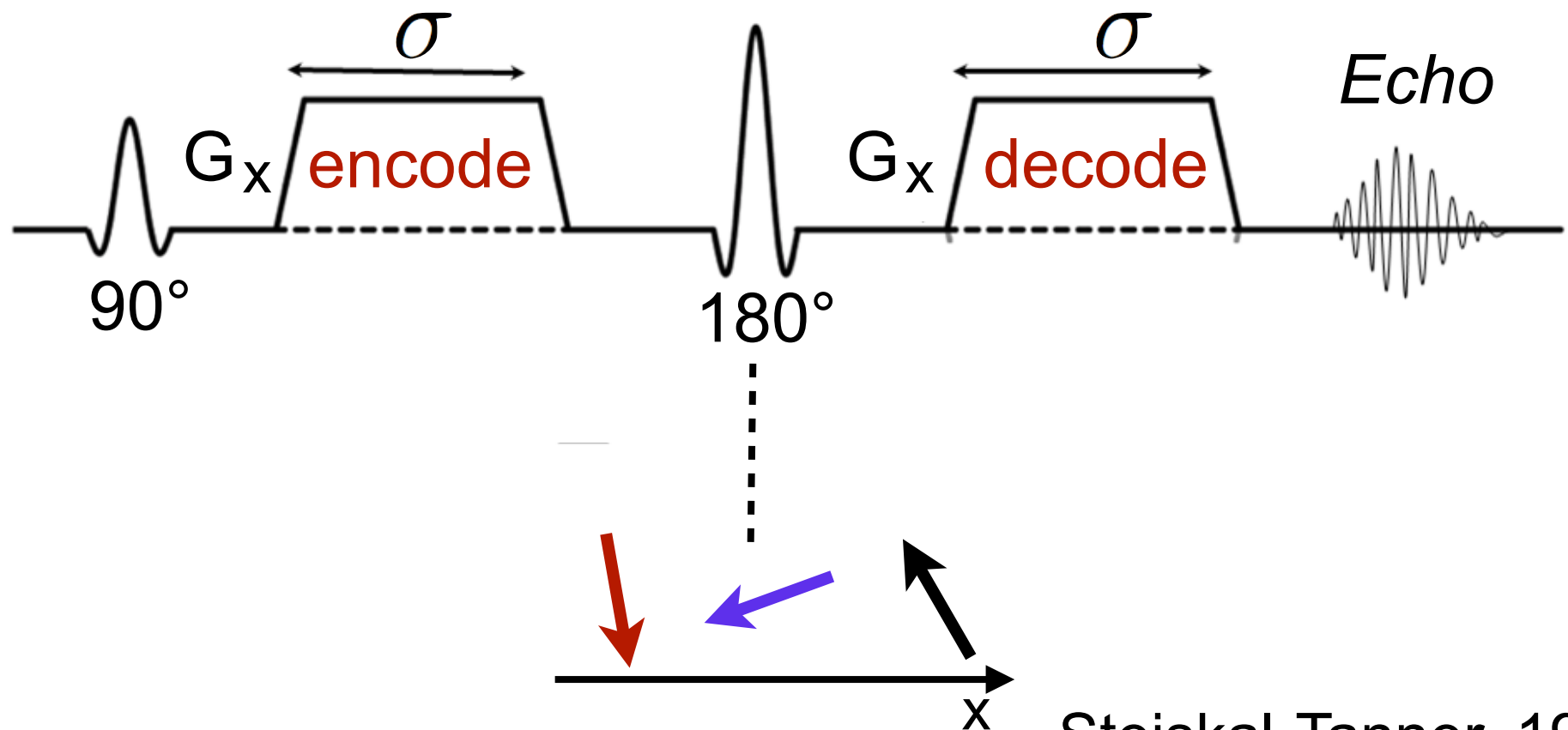


Stejskal-Tanner, 1965.



# Sensitizing the MRI Signal to Diffusion

## Case #1: Without Diffusion

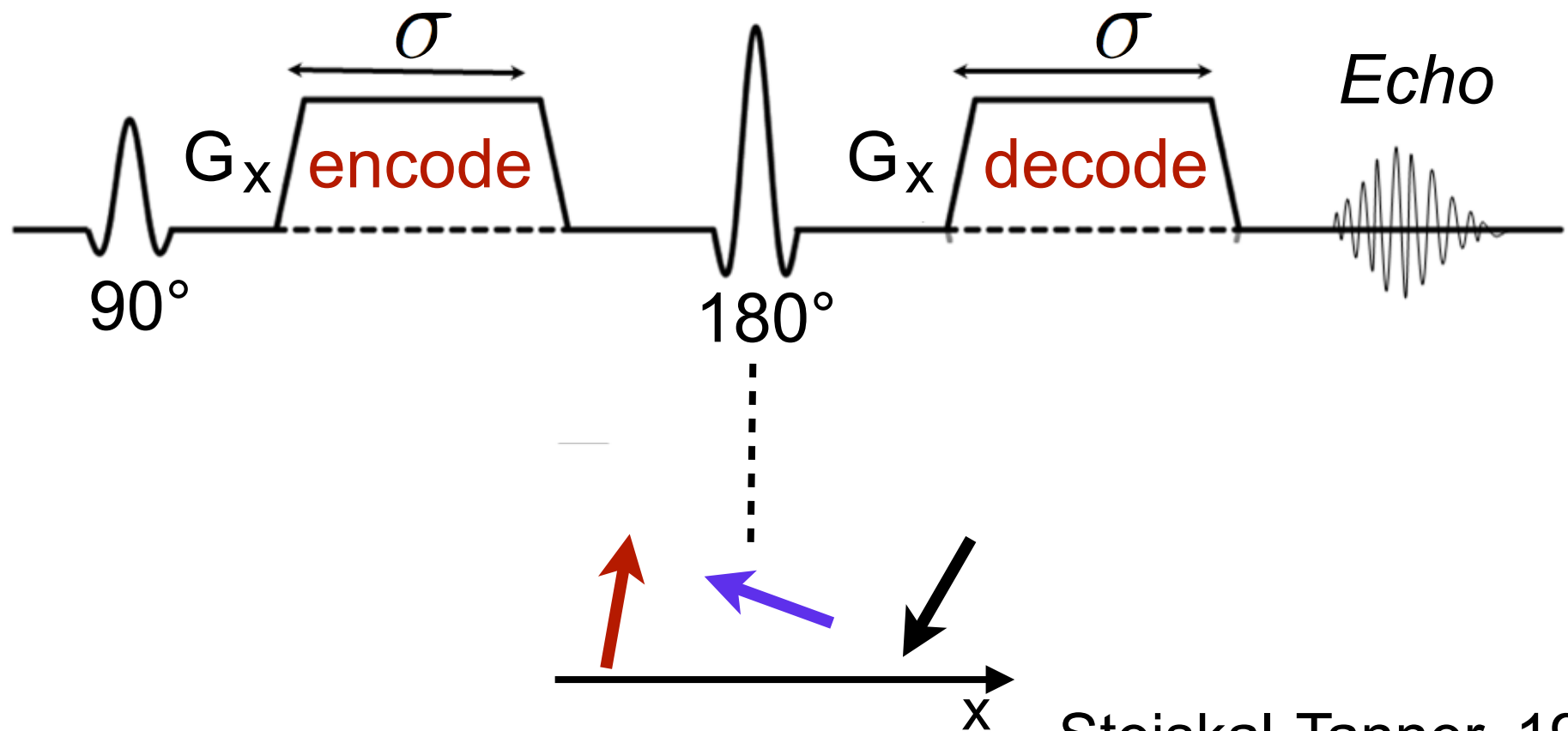


Stejskal-Tanner, 1965.



# Sensitizing the MRI Signal to Diffusion

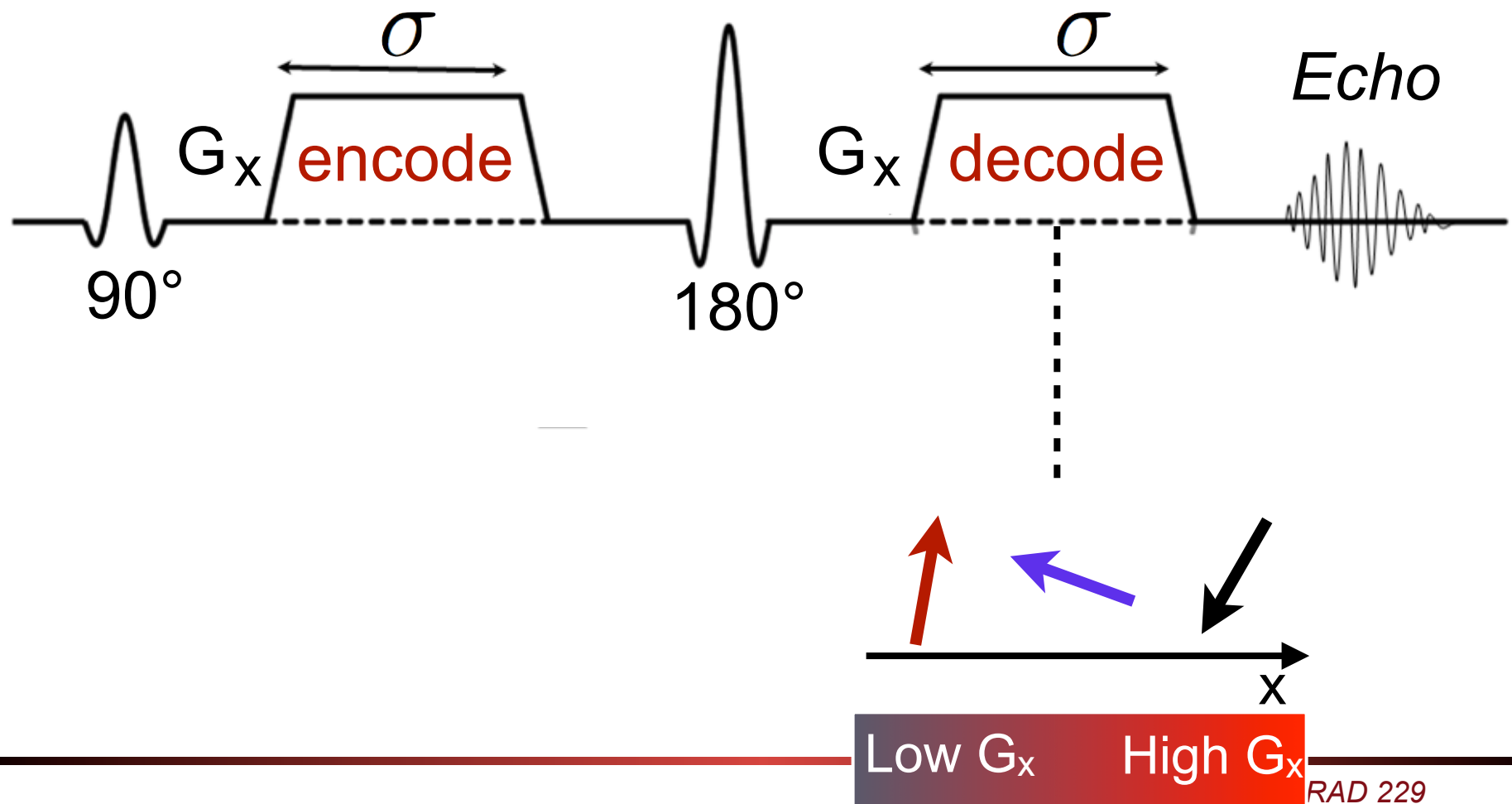
## Case #1: Without Diffusion



Stejskal-Tanner, 1965.

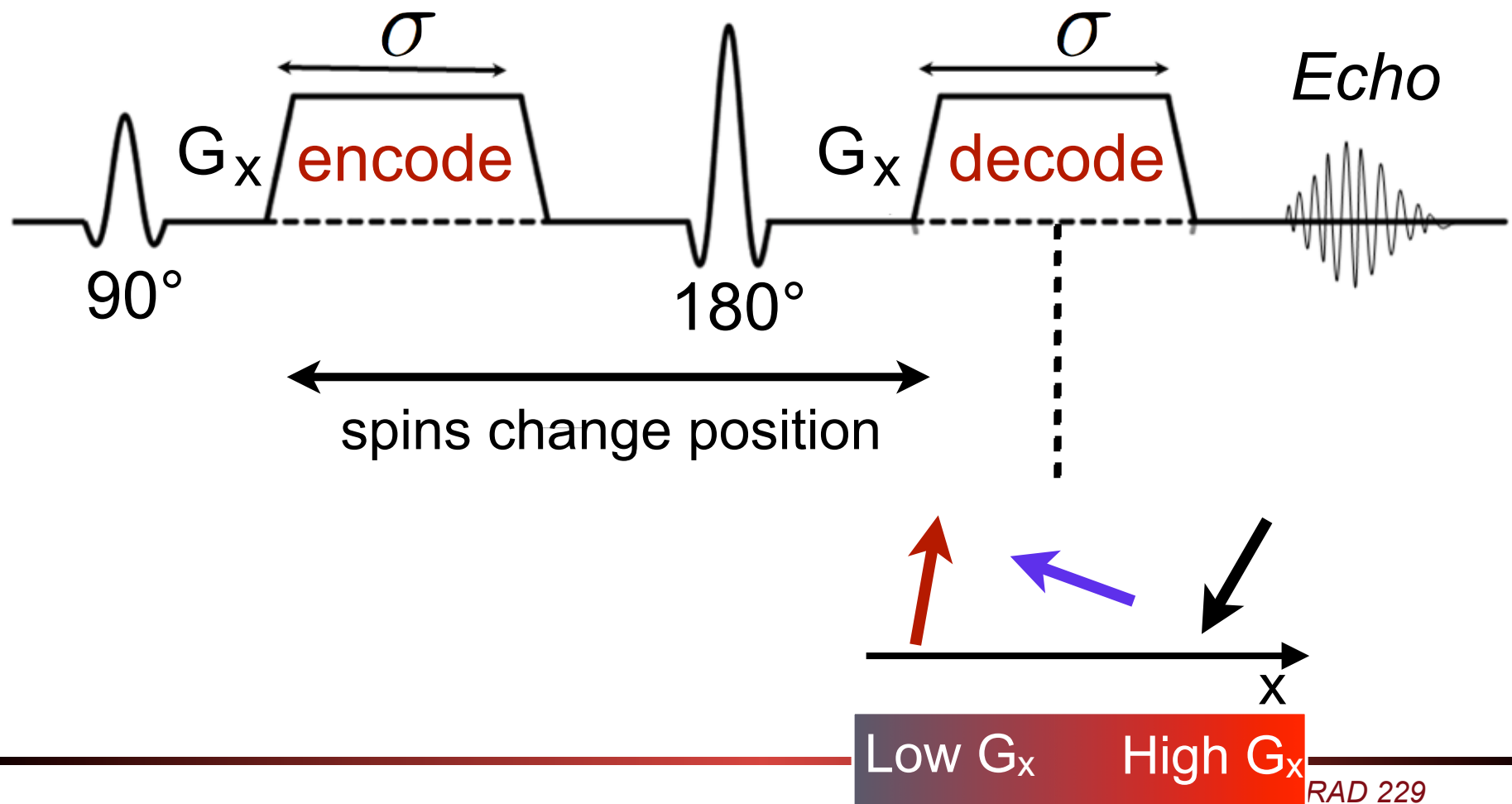
# Sensitizing the MRI Signal to Diffusion

## Case #1: Without Diffusion



# Sensitizing the MRI Signal to Diffusion

## Case #1: With Diffusion



# The Bloch Equation

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$$\frac{d\mathbf{M}}{dt} = \gamma(\mathbf{M} \times \mathbf{B}_0) + \begin{pmatrix} -\frac{M_x}{T_2} \\ -\frac{M_y}{T_2} \\ \frac{M_0 - M_z}{T_1} \end{pmatrix}$$

torque due to  $B_0$



relaxation



# The Bloch-Torrey Equation

Torrey H.C. *Physical Review* 1956.

$$\frac{d\mathbf{M}}{dt} = \gamma(\mathbf{M} \times \mathbf{B}_0) + \begin{pmatrix} -\frac{M_x}{T_2} \\ -\frac{M_y}{T_2} \\ \frac{M_0 - M_z}{T_1} \end{pmatrix} + \boxed{D\nabla^2\mathbf{M}}$$

Recall the diffusion equation:

$$\frac{\partial C}{\partial t} = \boxed{D\nabla^2 C}$$





# The Bloch-Torrey Equation

Torrey H.C. *Physical Review* 1956.

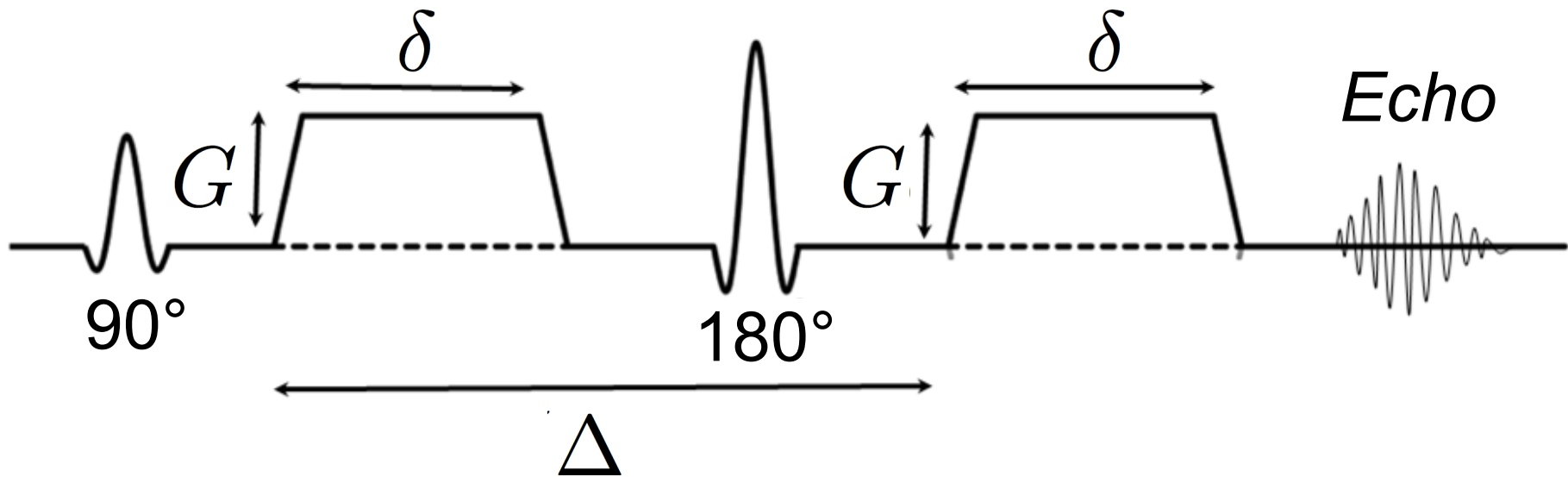
$$\frac{d\mathbf{M}}{dt} = \gamma(\mathbf{M} \times \mathbf{B}_0) + \begin{pmatrix} -\frac{M_x}{T_2} \\ -\frac{M_y}{T_2} \\ \frac{M_0 - M_z}{T_1} \end{pmatrix} + D\nabla^2\mathbf{M}$$

$$\mathbf{M}_+ = M_0 e^{\frac{-t}{T_2}} e^{-bD}$$

$$\text{with } b = \gamma^2 \int_0^{TE} \left( \int_0^t G(t') dt' \right)^2 dt$$



# b-value



$$b = \gamma^2 \int_0^{TE} \left( \int_0^t G(t') dt' \right)^2 dt$$

$$b = (\gamma G \delta)^2 \left( \Delta - \frac{\delta}{3} \right)$$

# Measuring the Diffusion Coefficient

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b-value:

$$b = (\gamma G \delta)^2 \left( \Delta - \frac{\delta}{3} \right)$$

Non-Diffusion-Weighted Signal:  $S_0$

Diffusion-Weighted Signal:  $S(b) = S_0 \exp(-bD)$

Diffusion Coefficient:

$$D = \frac{\ln \frac{S(b)}{S_0}}{-b}$$



# Apparent Diffusion Coefficient

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- For Diffusion MRI, the diffusion coefficient is referred to as the “Apparent” Diffusion Coefficient (ADC).  
Why?



# Motion Sensitivity for Diffusion MRI

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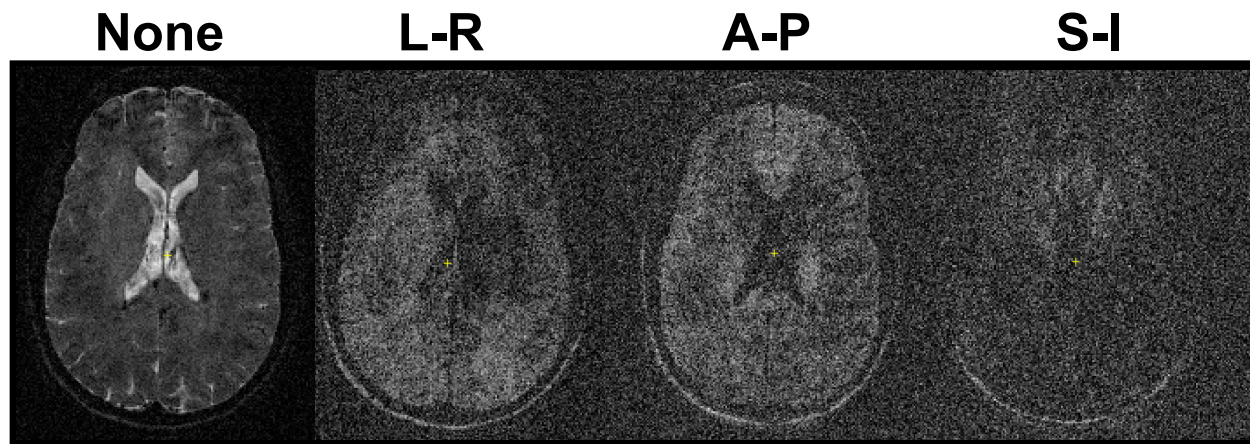
- Motion effects on diffusion MRI are different compared to other types of MRI pulse sequences.
- For diffusion MRI we are purposely sensitizing the MRI signal to motion of only a few microns.
- Therefore, any motion (bulk or physiological) during the time between the diffusion gradients will cause phase-offsets between read-outs.
  - Phase-encoding across multiple shots/read-outs does not work well.
  - This is why single-shot read-outs such as EPI or spiral are the preferred for diffusion MRI.



# Motion Sensitivity for Diffusion MRI

- Phase-encoding across multiple shots/read-outs does not work well.

## Diffusion-Weighted MRI with a segmented EPI read-out Diffusion-Encoding



- This is why single-shot read-outs are the preferred for diffusion MRI.

# Motion Artifacts for Diffusion MRI

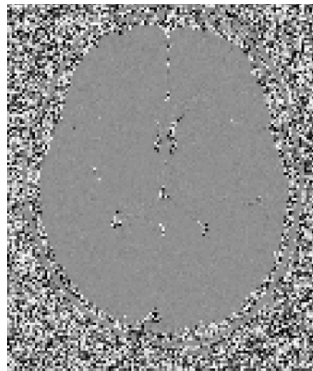
**A simple example:** Head rotation about through-plane (S-I) orientation (i.e. nodding motion) while diffusion encoding along L-R orientation causes a linear phase ramp along A-P.

No motion

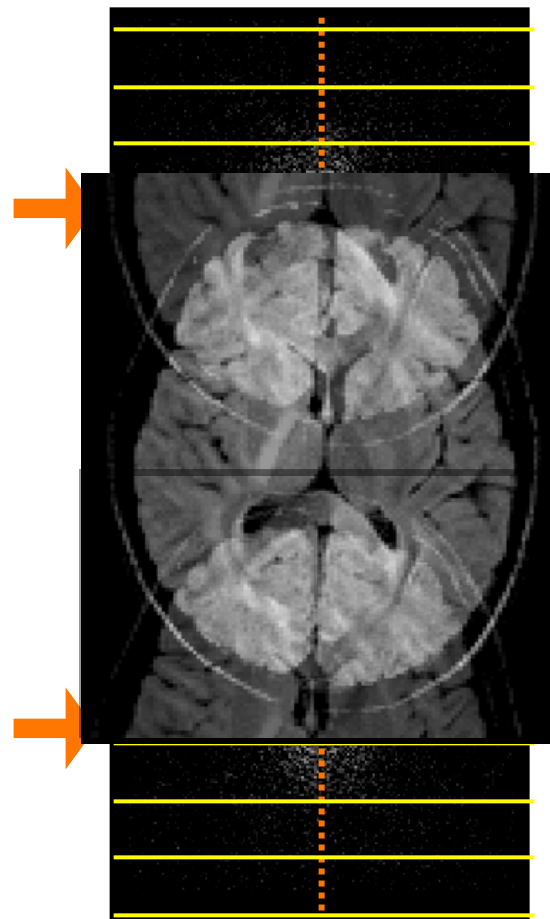
Magnitude



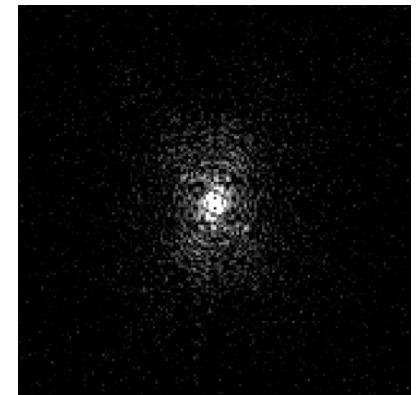
Phase



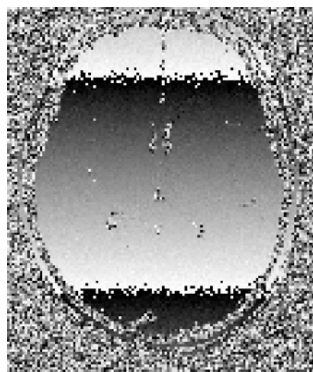
k-space segments



Sampled k-space

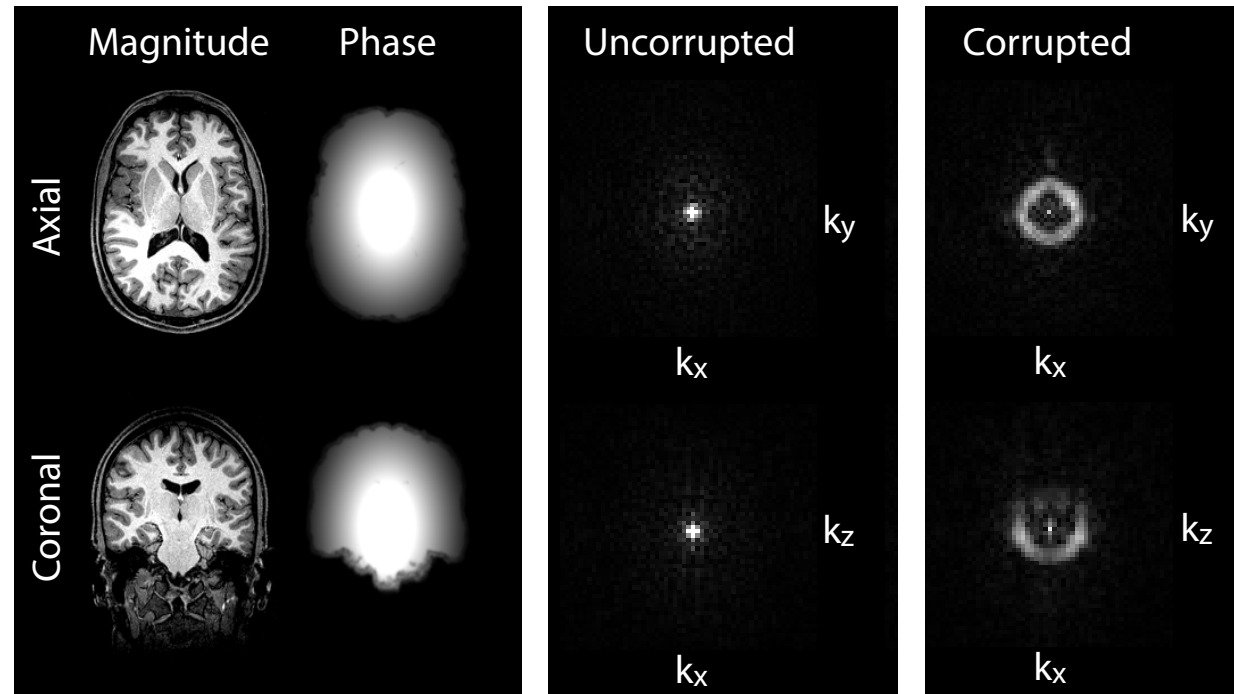
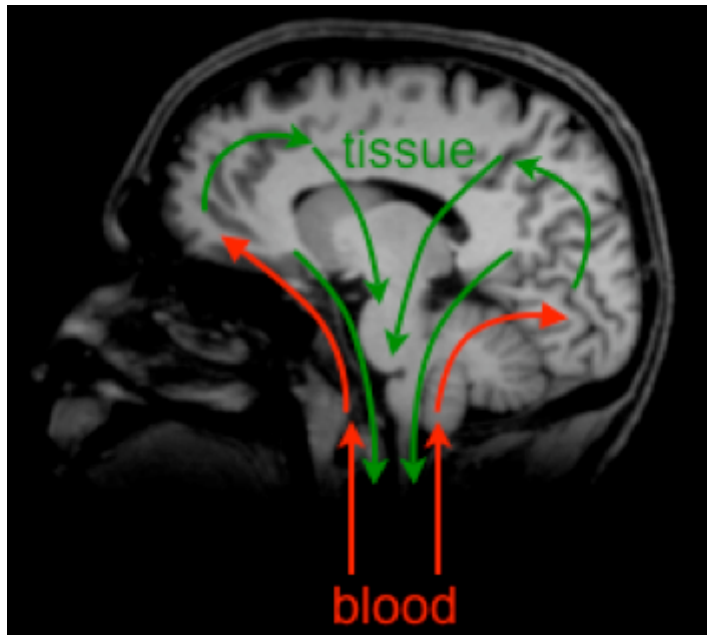


Motion



# Nonlinear Phase Offsets

## Non-Rigid Motion

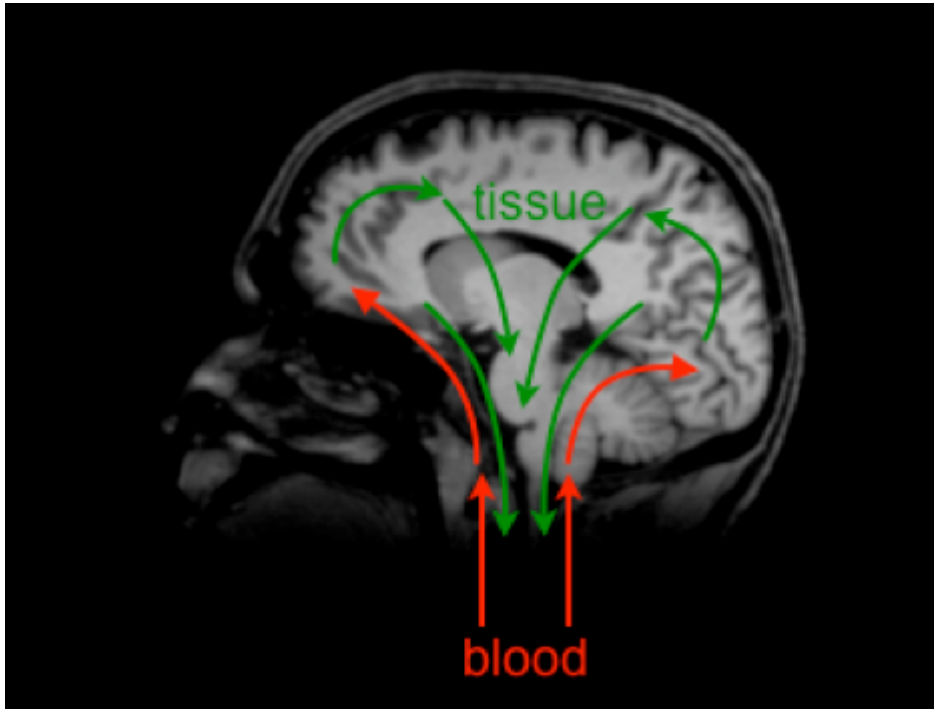


Subject restraints can reduce bulk motion, but ....in the brain, there is significant non-rigid motion from cardiac pulsatility that causes nonlinear phase-offsets.

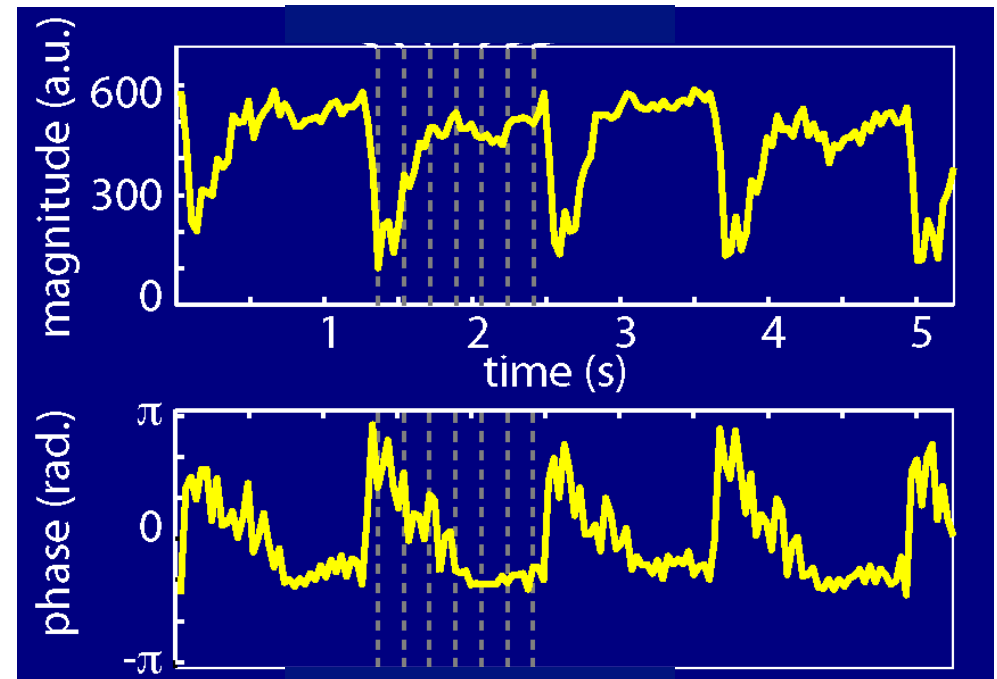


# The Brain is Never Still

## Non-Rigid Motion



## Time Course of Diffusion-Weighted Signal



Miller KL. MRM 2003.

Cardiac gating helps, but the brain is never still!

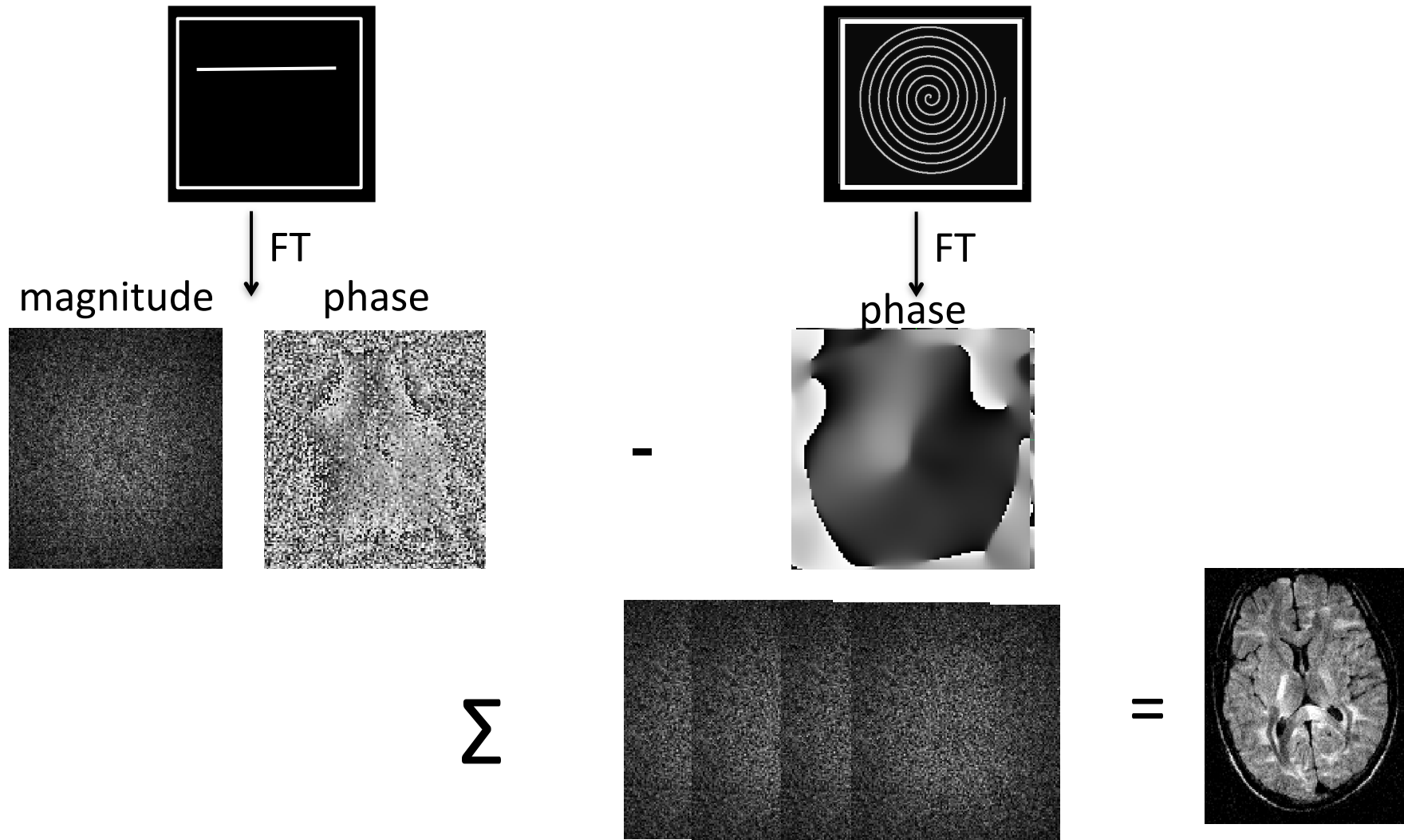
# Navigation for Multi-Shot Diffusion

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- Navigator: External or Internal (Self-Navigated)
- Examples:
  - ➔ PROPELLER
  - ➔ read-out segmented EPI
  - ➔ variable density spiral
  - ➔ variable density EPI (EPI with Keyhole)
- 0th, 1st or 2nd Order Linear and/or Non-Linear Corrections



# Nonlinear Phase Correction



Miller and Pauly, MRM 2003.

# Eddy Currents

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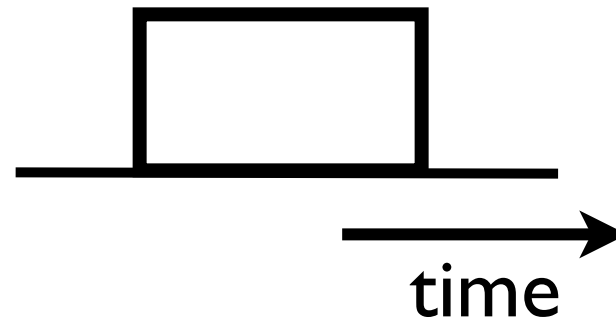
- The time-varying magnetic fields created by the magnetic gradient pulses in MRI sequences induce currents in the conducting structures within the magnet.
- These induced currents are called eddy currents and create unwanted magnetic fields that are detrimental to image quality.



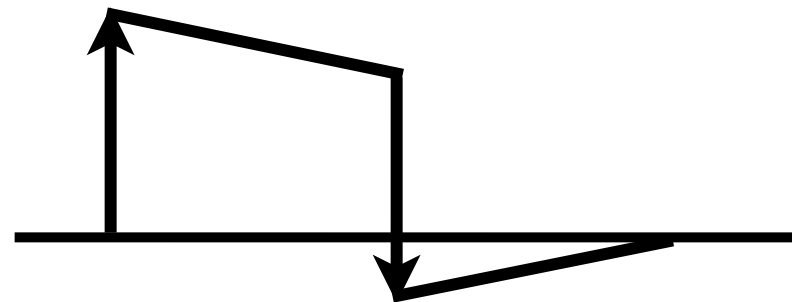
# Eddy Currents

- Eddy currents build up during the time varying portion of the gradient waveforms and decay during the constant portions.

Applied Gradient

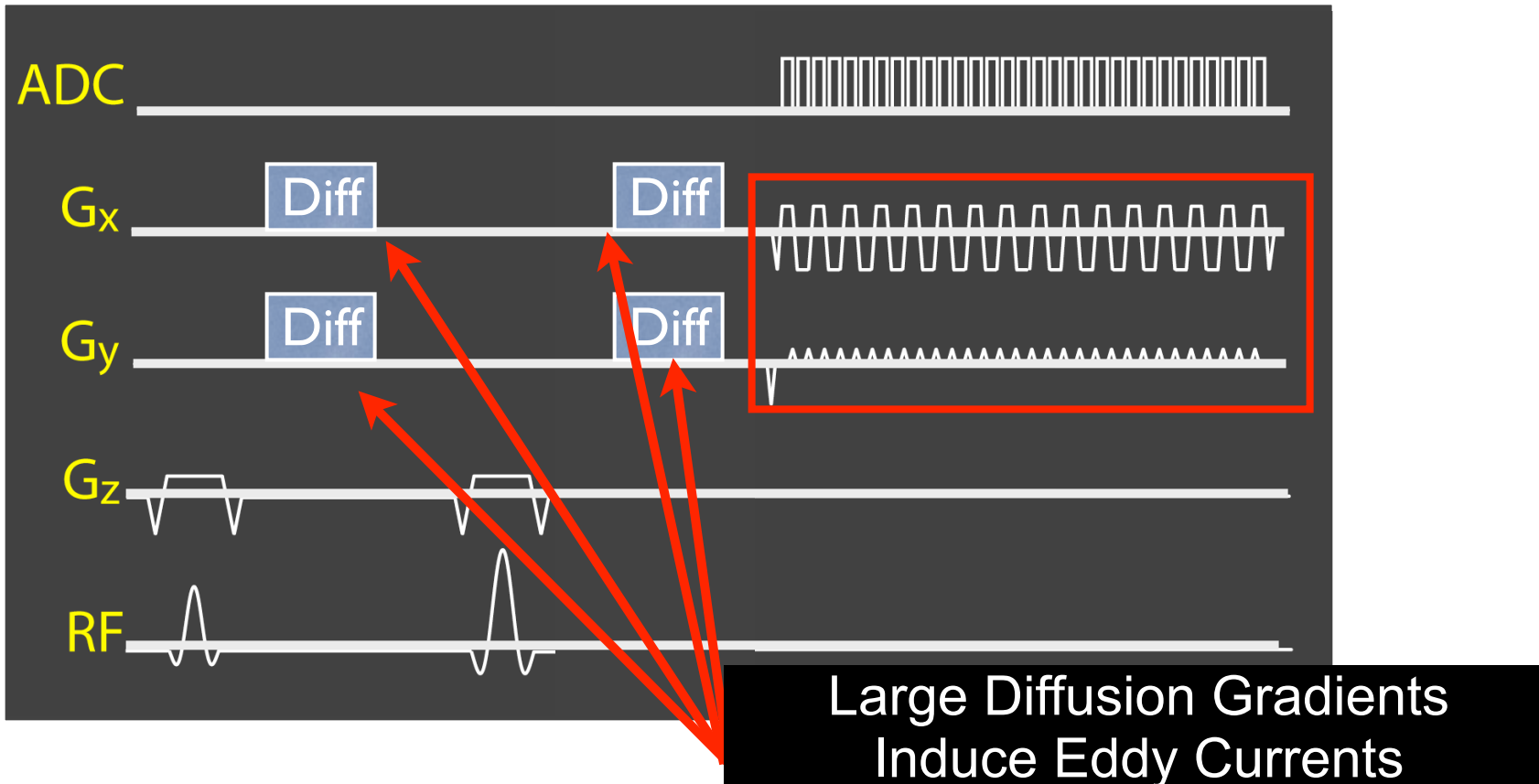


Eddy Current



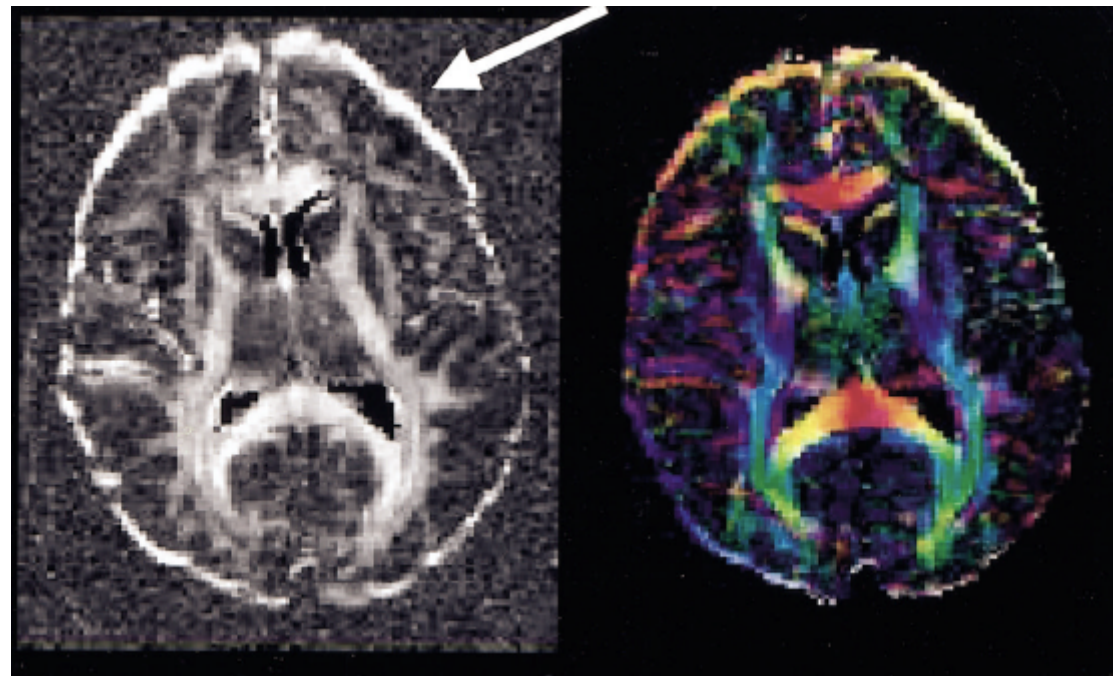
# Eddy Currents

- Eddy currents are more significant for diffusion imaging because the diffusion encoding gradients have high amplitude and can cause eddy currents that are still decaying during the read-out.



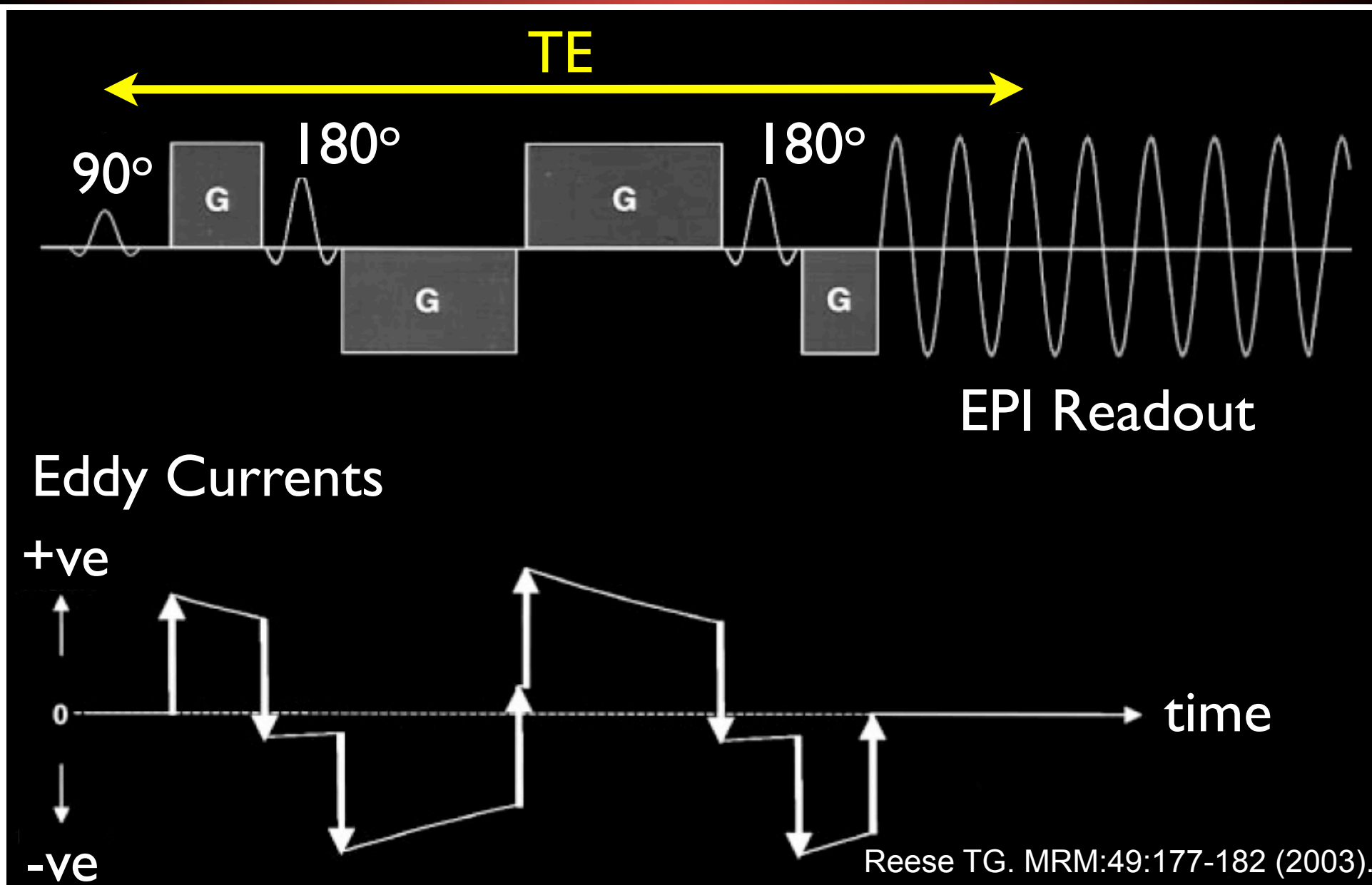
# Eddy Currents

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Movie courtesy R. Nunes

# Twice Refocused Spin Echo



Reese TG. MRM:49:177-182 (2003).





# Eddy Current Correction in PostProcessing

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Image registration of raw DWIs using FLIRT to correct for stretches and shears in your images.

Can be difficult for images with very low SNR.

Check your results carefully!

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- Sensitizing the MRI signal to diffusion.
- Diffusion MRI signal equations.
- Mapping diffusion coefficients.
- Effects of motion.
- Eddy currents.

