

The use of oscillatory signals in the study of genetic networks

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The structure of a genetic network is uncovered by studying its response to external stimuli (input signals). We present a theory of propagation of an input signal through a linear stochastic genetic network. We found that there are important advantages in using oscillatory signals over step or impulse signals and that the system may enter into a pure fluctuation resonance for a specific input frequency.

systems biology | synthetic biology | stochastic processes

The nature of a physical system is revealed through its response to external stimulation. The stimulus is imposed on the system, and its effects are then measured (Fig. 1*a*). This approach is widely used in biology: a cell culture is perturbed with a growth factor, a heat shock, etc. The data measured contain the initial information encoded into the stimulus and the information about the intrinsic characteristics of the system. The more parameters the experimentalist can adjust to craft the perturbation stimulus, the more information about the system can be revealed. In recent years we have witnessed a tremendous increase in measurement capabilities (e.g., microarray and proteomic technologies, better reporter genes). However, the success of the systems approach to molecular biology depends not only on the measurement instruments, but also on an effective design and implementation of the input stimulus, which has not been thoroughly explored. Traditionally, two types of time-dependent stimuli are at work in molecular biological experiments (1, 2). For example, a step stimulus is obtained when at one instant of time a growth factor is added to the medium (Fig. 1*a*, graph *a*). The stimulus from graph *b* in Fig. 1*a* is a superposition of two step stimuli. The investigator can control the height of the step stimulus (the concentration of the growth factor) or the time extension of the heat shock. The cells respond to these stimuli only transiently. The response is dampened after some time and becomes harder to detect because of noise. To overcome the noise, the concentration of the stimulus is typically increased to the point where the strength of the stimulus raises far above its physiological range.

We propose to implement a molecular switch at the level of gene promoter and use it to impose an oscillatory stimulus. In the absence of experimental noise, any stimulus can be used to determine the input-output properties of a genetic network. However, in the presence of experimental noise, oscillatory input has many advantages: (i) the measurements can be extended to encompass many periods so the signal-to-noise ratio can be dramatically improved; (ii) the measurement can start after transient effects subside, so that the data become easier to incorporate into a coherent physical model; and (iii) an oscillatory stimulus has more parameters (period, intensity, slopes of the increasing and decreasing regimes of the stimulus) than a step stimulus. As a consequence, the measured response will contain much more quantitative information. Experimental results from neuroscience prove that oscillatory stimulus can modulate the mRNA expression level of genes. For example, the *c-fos* transcription level in cultured neurons is enhanced 400% by an electrical stimulus at 2.5 Hz and reduced by 50% at 0.01 Hz

(3). Also, the mRNA levels of cell recognition molecule L1 in cultured mouse dorsal root ganglion neurons change if the frequency of the electric pulses is varied. The expression level of L1 decreases significantly after 5 days of 0.1-Hz stimulation but not after 5 days of 1-Hz stimulation (4). To extend the oscillatory approach to other types of cells, a two-hybrid assay (5) can be used to implement a molecular periodic signal generator (Fig. 1*c*). The light switch is based on a molecule (phytochrome in ref. 5) that is synthesized in darkness in the Q1 form. When the Q1 form absorbs a red light photon (wavelength 664 nm) it is transformed into the form Q2. When Q2 absorbs a far red light (wavelength 748 nm) the molecule Q goes back to its original form, Q1. The transitions take milliseconds. The protein *P* interacts only with the Q2 form, thus recruiting the activation domain to the target promoter. In this position, the promoter is open and the gene is transcribed. After the desired time has elapsed, the gene can be turned off by a photon from a far red light source. Using a sequence of red and far red light pulses the molecular switch can be periodically opened and closed.

There are four input parameters that can be varied: the period (*T*), the time separation between the pulses (*s*), and the amplitude (*A*) of the red and the far red pulses. The mRNA concentration profile will depend on these parameters and can be measured with high-throughput technology (6). Protein levels also will depend on the input signal. The proteins can be recorded with 2D PAGE analysis or MS. If one single gene product is targeted, than a real-time luminescence recording can be used (7). A periodic generator can be used to investigate biological systems for which the mRNA and protein concentrations naturally oscillate in time. An example of such a system is the circadian clock that drives a 24-h rhythm in living organisms from human to cyanobacteria. The core oscillator is a molecular machinery based on an autoregulatory feedback loop involving a set of key genes (*Bmal*, *Per1*, *Per2*, *Per3*, *Cry1*, *Cry2*, etc.) (8). Experimental procedures used to elucidate the clock mechanism are based on measuring the circadian wheel-running behavior of mice under normal light/dark cycles or in constant darkness (dark/dark) conditions. Experimental evidence demonstrates that laws of quantitative nature govern the molecular clock. For example (9), the internal clock of *Cry1* mutants have a free-running (i.e., dark/dark conditions) period of 22.51 ± 0.06 h, which is significantly lower than the period of 23.77 ± 0.07 h for WT mice. In contrast, a *Cry2* mutant has a significantly higher period of 24.63 ± 0.06 h. In light/dark conditions, both mutants follow the 24-h period of the entrained light cycles. A double *Cry1,2* mutant is arrhythmic in dark/dark conditions and follows a 24-h rhythm in light/dark conditions. To explain these experimental values we suggest using a light-switchable generator to drive the expression level of *Cry1* and *Cry2* and measure the dynamics of transcription and the translation for the rest of the key clock genes. Another application of the periodic generator is to modulate a constitutively expressed gene by superimposing an oscillatory profile on top of its

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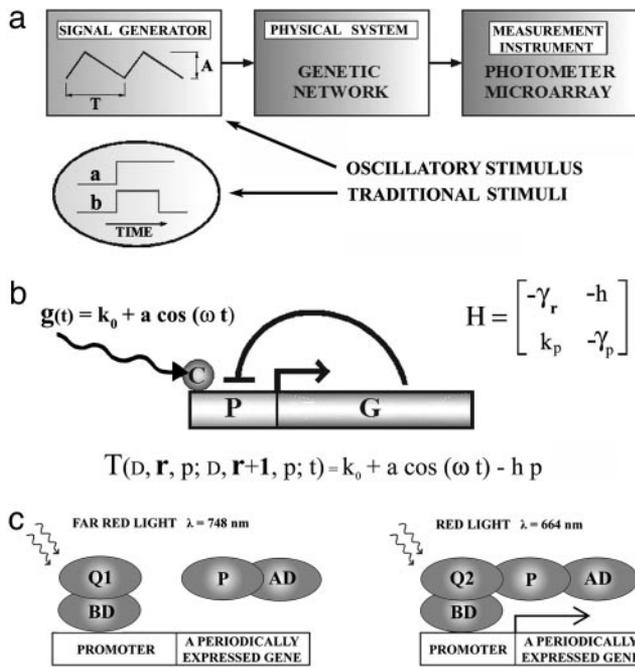


Fig. 1. Genetic networks stimulated by signal generators. (a) Genetic network response depends on the type of the applied stimulus. (b) An autoregulatory network. The gene G is under the influence of a cofactor C that rhythmically modulates the activity of the promoter P . The matrix H contains the parameters that dictate the transition probabilities of the stochastic model. The transition probability per unit time from r to $r + 1$ mRNA molecules, $T(D, r, p; D, r + 1, p; t)$, is modulated by the oscillatory signal generator. The DNA, D , and the protein, p , do not change in this transition. (c) The gene is turned on with a red light pulse of wavelength $\lambda = 664 \text{ nm}$. With a far red light of wavelength $\lambda = 748 \text{ nm}$ the gene is turned off. Adapted from ref. 5. AD, activation domain; BD, binding domain; Q, a protein that changes its form upon light exposure, from Q1 to Q2 and back; P, a protein that interacts only with form 2 of protein Q (Q2).

flat level. Then, the genes that show a modulation with a frequency equal to the generator's frequency will be detected by a microarray experiment. Why is this approach different from the one where a step stimulus is used? Because the frequency of the generator is not an internal parameter of the biological system. The genes that interact with the driven gene will be modulated by the input frequency. The rest of the genes will have different expression profiles dictated by the internal parameters of the biological system. This point of view is supported by our findings (6) that the circadian clock (which is an endogenous periodic signal generator) propagates its output to only 8–10% of the transcriptome in mice peripheral tissues (liver or heart). In contrast to the oscillatory input, when a step stimulus is applied, all of the expression profiles are dictated by the internal parameters of the biological system. Except for the height of the step stimulus (the dose of the factor applied) there is no external parameter implemented into the input signal. As such, it is difficult to separate those genes that directly respond to the input signal and consequently avoid artifacts. With the applications described in mind, we study the propagation of an input signal through a stochastic genetic network.

The Response of a Stochastic Genetic Network to an Input Stimulus

The effects of an oscillatory input have been studied on specific biological systems by using models based on differential equations (10–12). The stochastic character is embedded into these equations as an exterior additive term. In contrast, we compute the generator's effects on the mean and fluctuation of the gene products with

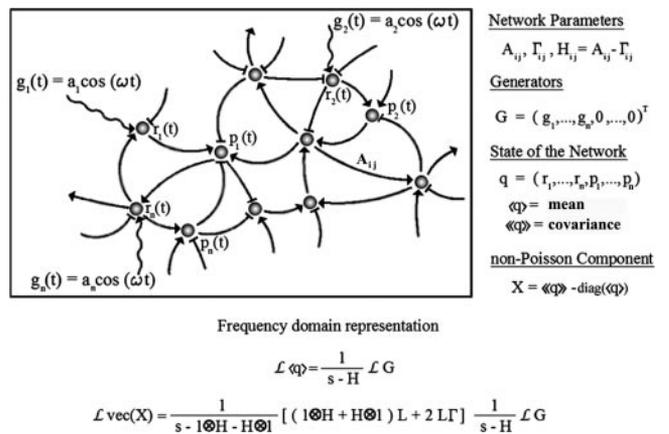


Fig. 2. Response of a stochastic genetic network to an oscillatory input. The Laplace transform \mathcal{L} changes the dynamic variable from time to frequency. In the $\text{vec}(X)$ all of the elements of matrix X are arranged in a column vector.

a stochastic model (13–15). In this way, the generated stimulus and the noisy nature of the cell are entangled in the stochastic genetic model. For a network of n genes (Fig. 2) the state of a cell is described by the mRNA and protein molecule numbers: $q = (r_1, \dots, r_n, p_1, \dots, p_n)$. We assume that, during any small time interval Δt , the probability for the production of a molecule of the i th type is $(\sum_{j=1}^{2n} A_{ij} q_j + G_i(t)) \Delta t$, i.e., q_i is increased by 1 with the above probability. The function $G_i(t)$ represents the time-varying input signal and modulates the mRNA production only: $G = (g_1(t), \dots, g_n(t), 0, \dots, 0)^T$ (the superscript T is the transposition operation that transforms G into a column vector for notational convenience in what follows). The parameter A_{ij} represents the influence of the j th type of molecule on the production rate of a molecule of the i th type. Similarly, there is a matrix of parameters Γ_{ij} governing the degradation rates of the molecules. For simplicity, we assume that the input stimulus directly affects only the production rates. The mean $\mu = \langle q \rangle$ and the covariance matrix $\nu = \langle\langle q \rangle\rangle = \langle\langle (q - \langle q \rangle)(q - \langle q \rangle)^T \rangle\rangle$ of the state q are driven by the generator G .

The transfer of the signal from the generator through the genetic network to the output measured data is encapsulated in a set of transfer matrices. Specifically, let $H = A - \Gamma$ and denote the Laplace transforms of μ and G by $\mathcal{L}\mu$ and $\mathcal{L}G$. Here and in what follows, μ and G are represented as column vectors. The connection between the mean and the generators is given by formula 1, which is typical for a deterministic linear system. However, the genetic system is stochastic and the measure of the intrinsic noise is quantified by the covariance matrix ν . The effect of the stimulus generators is most transparent if we split ν in a Poisson and a non-Poisson component: $\nu = \text{diag}(\mu) + X$. Here $\text{diag}(\mu)$ represents a matrix with the components of the vector μ on its diagonal, with all of the other terms being zero. For a Poisson process, $X = 0$ and thus the term $\text{diag}(\mu)$ is called the Poisson component of ν . The non-Poisson component $X = \nu - \text{diag}(\mu)$ can be expressed in terms of the generators (Appendix and Supporting Text, which is published as supporting information on the PNAS web site):

$$\mathcal{L}\mu = \frac{1}{(s - H)} \mathcal{L}G, \quad [1]$$

$$\mathcal{L}\text{vec}(X) = \frac{1}{s - 1 \otimes H - H \otimes 1} [-(1 \otimes H + H \otimes 1)L + 2L\Gamma] \frac{1}{s - H} \mathcal{L}G. \quad [2]$$

suggest that there are natural conditions for a strong height fluctuation resonance (Fig. 3). However, for a sharp fluctuation resonance (small half width), we need $h > \gamma_r$ or γ_p , a condition that does not appear in all genetic networks. It is through the experimental study that we will clarify how some biological systems can sustain fluctuation resonance and others can not. Besides resonance, the frequency response provides other insights into the structure of the autoregulatory system. The parameters of the system can be read from the measured data. The frequency response of the mean values behave like the response of a classical linear system to input signals. The new aspects are those related to fluctuations. Like $X_{pp}(t)$ and $X_{rr}(t)$, the correlation coefficient between the mRNA and protein number will oscillate in time: $X_{rp}(t) = X_{rp,0} + X_{rp,1}e^{i\omega t} + X_{rp,1}^*e^{-i\omega t}$ with amplitude $X_{rp,1}$. Taking the ratios of the amplitudes $|X_{rp,1}|^2/|X_{r,1}|^2 = (1/4h^2)\omega^2 + \gamma_r^2/h^2$, $|X_{rp,1}|^2/|X_{p,1}|^2 = (1/4k_p^2)\omega^2 + \gamma_p^2/k_p^2$, we observe that all four parameters of the system can be estimated from the slopes and the intercepts of the above ratios as a function of ω^2 . Detail formulas for each amplitude are given in *Supporting Text*.

The Spectrum, the Experimental Noise, and the Importance of the Input Stimulus

We described the use of a periodic signal to decipher a genetic network. Traditionally, a step stimulus is used in biology for pathway detection (i.e., adding a growth factor to the culture). From the response to a step stimulus we can extract, in principle, the parameters of the system. The natural question is then: why should we generate a periodic stimulus when there is already a step stimulus in use? Seeking an answer, we notice that the measured data in our studied example can be expressed as a sum of exponentially decaying functions, $e^{-\lambda t}$, if a step stimulus was used (*Supporting Text*). For a periodic input, the response contains only exponentials with imaginary argument, $e^{i\omega t}$. Mathematically, the main difference between exponentials with real arguments, $e^{-\lambda t}$, and those with imaginary arguments, $e^{i\omega t}$, is that with the former we cannot form an orthogonal basis of functions, whereas such a basis can be formed with the latter. If we depart from our example, we can say that, in general, the response of the network to a step input will be a sum of components that are not orthogonal on each other. The time dependence of these nonorthogonal components can be more complex than an exponential function; they can contain polynomials in time or decaying oscillations, depending on the position in the complex plane of eigenvalues of the transfer matrix H . In contrast, the permanent response obtained from a periodic input is a sum of Fourier components that form an orthogonal set. Orthogonal components are much easier to separate than nonorthogonal ones. This mathematical difference explains the advantage of using oscillatory inputs. However, an argument can be made that increasing the number of replicates will be enough to separate the step response from noise. In what follows we study how many replicates are needed to successfully fight the experimental noise. We will show that fewer replicates are needed if the genetic network is probed with an oscillatory generator rather than a step signal. To keep the argument simple, we will study the difficulty of separating nonorthogonal components for a network for which the response to a step stimulus is a sum of decaying exponentials. The argument can be extended to other types of nonorthogonal components, but this line of thought falls outside the scope of this article. The measured data being a superposition of exponential terms can be written as:

$$f(t) = \int_{x_1}^{x_2} S(x)K(xt)dx, \quad [4]$$

with $K(xt) = e^{-ixt}$ for the periodic response and $K(xt) = e^{-xt}$ for the step stimulus. The spectral function $S(x)$ depends on the network's parameters and the type of the input signal. For example, the spectrum of the autoregulatory system for a periodic input is $S(x) = S_0\delta(x) + S_1\delta(x - i\omega) + S_1^*\delta(x + i\omega)$, where $\delta(x)$ is the Dirac delta function. The coefficients S_0 , S_1 take specific values if the spectrum refers to mean mRNA, proteins, or their correlations. For example, for the protein fluctuation:

$$S_0 = X_{p,0} = \frac{k_p^2 k_0 (\gamma_p - h) \gamma_r}{\omega_0^4 \omega_1}, \quad [5]$$

$$S_1 = X_{p,1} = \frac{ia(-i\gamma_p + \omega + ih)(\omega - 2i\gamma_r)k_p^2}{(\omega^2 - \omega_0^2 - i\omega\omega_1)(\omega^2 - 2i\omega\omega_1 - 4\omega_0^2)(\omega - i\omega_1)}. \quad [6]$$

A detailed description of the spectrum for an autoregulatory network is given in *Supporting Text*. For oscillatory inputs that are not pure cosine function and for more complicated networks, the spectrum is more complex, but is still connected with the measured data like in 4. The spectrum $S(x)$ carries information about the parameters of the genetic network and can be recovered from the data $f(t)$. The network's parameter can be estimated from the spectrum once a model of the network is chosen. Our goal is to show that the spectrum obtained from an oscillatory input signal is much less distorted by the experimental noise than the spectrum obtained from a step input. Laboratory measurements are samples of $f(t)$ at N discrete time points. Given a finite number N of measured data points, f_1, \dots, f_N , the spectrum for the periodic case $S(x)$ can only be approximated as a weighted sum of N terms (*Supporting Text*): $S(x) = \sum_{k=1}^N (s_k + \varepsilon_k/\beta_k)\Theta_k(x)$. Each term, $(s_k + \varepsilon_k/\beta_k)\Theta_k(x)$, contains a function $\Theta_k(x)$ that does not depend on the measured data and the weights $s_k + \varepsilon_k/\beta_k$ that are computed from the measured data f_1, \dots, f_N . In the absence of experimental noise, $\varepsilon_k = 0$, all N coefficients s_k can be computed from the measured data. When experimental noise is present, $\varepsilon_k \neq 0$, what we compute from measured data is $s_k + \varepsilon_k/\beta_k$, and we cannot separate s_k from it because we do not know the actual value for ε_k . The best we can do is to use only those terms for which $s_k > \varepsilon_k/\beta_k$, so the effect of the distortion on s_k is not large. Unfortunately, the distortion increases as β_k gets smaller, which actually happens when k increases. A term can be recovered from noise if $\beta_k^{-1} < s_k/\varepsilon_k$. Usually, this relation is valid for $k = 1 \dots J_p$, with J_p being the last term that can be recovered. A similar relation holds for the exponential case, with α_k instead of β_k and J_e instead of J_p . It is desirable that both cutoffs (J_p, J_e) be as close as possible to the number of sampled points, N . The striking difference between the two cases is that the cutoff J_p is much larger than the cutoff J_e . This difference is a consequence of the fact that the numbers α_k decrease exponentially to 0 (22), whereas β_k stays close to 1 for many k before eventually dropping close to zero (23). This huge difference between α_k and β_k has its origin in the fact that the set of functions of time, $\exp(-\lambda t)$, indexed by λ , do not form an orthogonal set, whereas the functions $\exp(i\omega t)$, indexed by ω , are orthogonal.

In theory, however, we can still hope that a step stimulus can deliver good estimates if the noise ε_k is reduced by using r replicates ($\varepsilon_k \rightarrow \varepsilon_k/\sqrt{r}$). This is not the case. Fig. 4 represents the number of replicates needed to recover the component J_e or J_p if the signal-to-noise ratio (SNR) is 10 (SNR $\equiv s_{J_e}/\varepsilon_{J_e} = s_{J_p}/\varepsilon_{J_p} = 10$). The number of replicates grows very fast in the exponential case (for SNR = 10 and $N = 20$ we need 269 replicates for the fourth spectral component), whereas in the periodic case, the number of replicates stays low for many spectral components (only for the 17th component it raises to 14,

mRNA production can be influenced by the protein concentration, and this feedback effect is described by the elements of the $2n \times 2n$ matrix A (7). The structure of the matrix A is a consequence of the topology of the genetic network. The equation for the probability $P(\vec{q}, t)$ of the network to be in the state \vec{q} at time t is: $\partial P(\vec{q}, t) / \partial t = \sum_{i=1}^M (E_i^- - 1) \sum_{k=1}^M \tilde{A}_{ik} \tilde{q}_k P(\vec{q}, t) + \sum_{i=1}^M (E_i^+ - 1) \sum_{k=1}^M \tilde{\Gamma}_{ik} \tilde{q}_k P(\vec{q}, t)$, where the shift operators E_i^\pm are given by $E_i^\pm P(\vec{q}, t) = P(\vec{q}, \dots, \tilde{q}_i \pm 1, \dots, \tilde{q}_M)$.

We need the time evolution equations for mRNAs and proteins: $\mu_i = \langle q_i \rangle$ and $v_{ij} = \langle q_i q_j \rangle - \langle q_i \rangle \langle q_j \rangle$, $i, j = 1, \dots, 2n$. In matrix notation, for the column vector μ and for the matrix X with elements given by $X_{ij} = v_{ij} - \delta_{ij} \mu_i$ we obtain:

$$\frac{d}{dt} \mu = H\mu + G, \tag{8}$$

$$\frac{d}{dt} X = HX + HT^T + H \text{diag}(\mu) + \text{diag}(\mu)H^T + 2\text{diag}(\Gamma\mu). \tag{9}$$

Here H^T is the transpose matrix of $H = A - \Gamma$ and $\text{diag}(\mu)$ has nonzero elements only on the principal diagonal: $\text{diag}(\mu)_{ij} =$

$\delta_{ij} \mu_i$. Using the Laplace transform, the solution to **8** is **1**. Eq. **9** is a matrix equation. To solve this equation we first transform it to an equation where the unknown is a column vector. The transformation needed is $X \rightarrow \text{vec}(X)$, where the column vector $\text{vec}(X)$ contains the columns of the matrix X one on top of the other, starting with the first column and ending with the last column. The vec mapping has the useful property that $\text{vec}(HX) = (1 \otimes H)\text{vec}(X)$, $\text{vec}(XH) = (H^T \otimes 1)\text{vec}(X)$, where 1 is the unit matrix and $A \otimes B$ is the tensor product of matrices A and B . The column vector $\text{vec}(\text{diag}(\mu))$ can be expressed in terms of the column vector μ : $\text{vec}(\text{diag}(\mu)) = L\mu$, where L is a lift matrix from a space of dimension of μ to the square of this dimension: $L = (P_1, \dots, P_{2n})^T$, $(P_k)_{ij} = \delta_{ik} \delta_{jk}$. The solution to **9** takes the form **2**.

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1. Gardner, T. S., di Bernardo, D., Lorenz, D. & Collins, J. J. (2003) *Science* **301**, 102–105.
2. Vance, W., Arkin, A. & Ross, J. (2002) *Proc. Natl. Acad. Sci. USA* **99**, 5816–5821.
3. Sheng, H. Z., Fields, R. D. & Nelson, P. G. (1993) *J. Neurosci. Res.* **35**, 459–467.
4. Itoh, K., Stevens, B., Schachner, M. & Fields, R. D. (1995) *Science* **270**, 1369–1372.
5. Shimizu-Sato, S., Huq, E., Tepperman, J. M. & Quail, P. H. (2002) *Nat. Biotechnol.* **20**, 1041–1044.
6. Storch, K. F., Lipan, O., Leykin, I., Viswanathan, N., Davis, F. C., Wong, W. H. & Weitz, C. J. (2002) *Nature* **417**, 78–83.
7. Izumo, M., Johnson, C. H. & Yamazaki, S. (2003) *Proc. Natl. Acad. Sci. USA* **100**, 16089–16094.
8. Reppert, S. M. & Weaver, D. R. (2002) *Nature* **418**, 935–941.
9. van der Horst, G. T. J., Muijtjens, M., Kobayashi, K., Takano, R., Kanno, S., Takao, M., de Wit, J., Verkerk, A., Eker, A. P. M., vanLeeuwen, D., et al. (1999) *Nature* **398**, 627–630.
10. Smolen, P., Baxter, D. A. & Byrne, J. H. (1998) *Am. J. Physiol.* **43**, C531–C542.
11. Hasty, J., Dolnik, M., Rottschäfer, V. & Collins, J. (2002) *Phys. Rev. Lett.* **88**, 148101.
12. Simpson, M. L., Cox, C. D. & Sayle, G. S. (2003) *Proc. Natl. Acad. Sci. USA* **100**, 4551–4556.
13. Thattai, M. & van Oudenaarden, A. (2001) *Proc. Natl. Acad. Sci. USA* **98**, 8614–8619.
14. Swain, P. S., Elowitz, M. B. & Siggia, E. D. (2002) *Proc. Natl. Acad. Sci. USA* **99**, 12795–12800.
15. van Kampen, N. G. (1992) *Stochastic Processes in Physics and Chemistry* (North-Holland, Amsterdam).
16. Ljung, L. (1999) *System Identification-Theory for the User* (1999) (Prentice-Hall, Upper Saddle River, NJ), 2nd Ed.
17. Lee, T. I., Rinaldi, N. J., Robert, F., Odom, D. T., Bar-Joseph, Z., Gerber, G. K., Hannett, N. M., Harbison, C. T., Thompson, C. M., Simon, I., et al. (2002) *Science* **298**, 799–804.
18. Becskei, A. & Serrano, L. (2000) *Nature* **405**, 590–593.
19. Rosenfeld, N., Elowitz, M. & Alon, U. (2002) *J. Mol. Biol.* **323**, 785–793.
20. Isaacs, F., Hasty, J., Cantor, C. & Collins, J. (2003) *Proc. Natl. Acad. Sci. USA* **100**, 7714–7719.
21. Kennell, D. & Riezman, H. (1977) *J. Mol. Biol.* **114**, 1–21.
22. Bertero, M., Brianzi, P. & Pike, E. R. (1985) *Proc. R. Soc. London A* **398**, 23–44.
23. Slepian, D. (1983) *SIAM Rev.* **25**, 379–393.
24. Panda, S., Antoch, M.P., Miller, B. H., Su, A. I., Schook, A. B., Straume, M., Schultz, P. G., Kay, S. A., Takahashi, J. S. & Hogenesch, J. B. (2002) *Cell* **109**, 307–320.
25. Gadgil, C., Lee, C.-H. & Othmer, H. G. (2005) *Bull. Math. Biol.*, in press.