



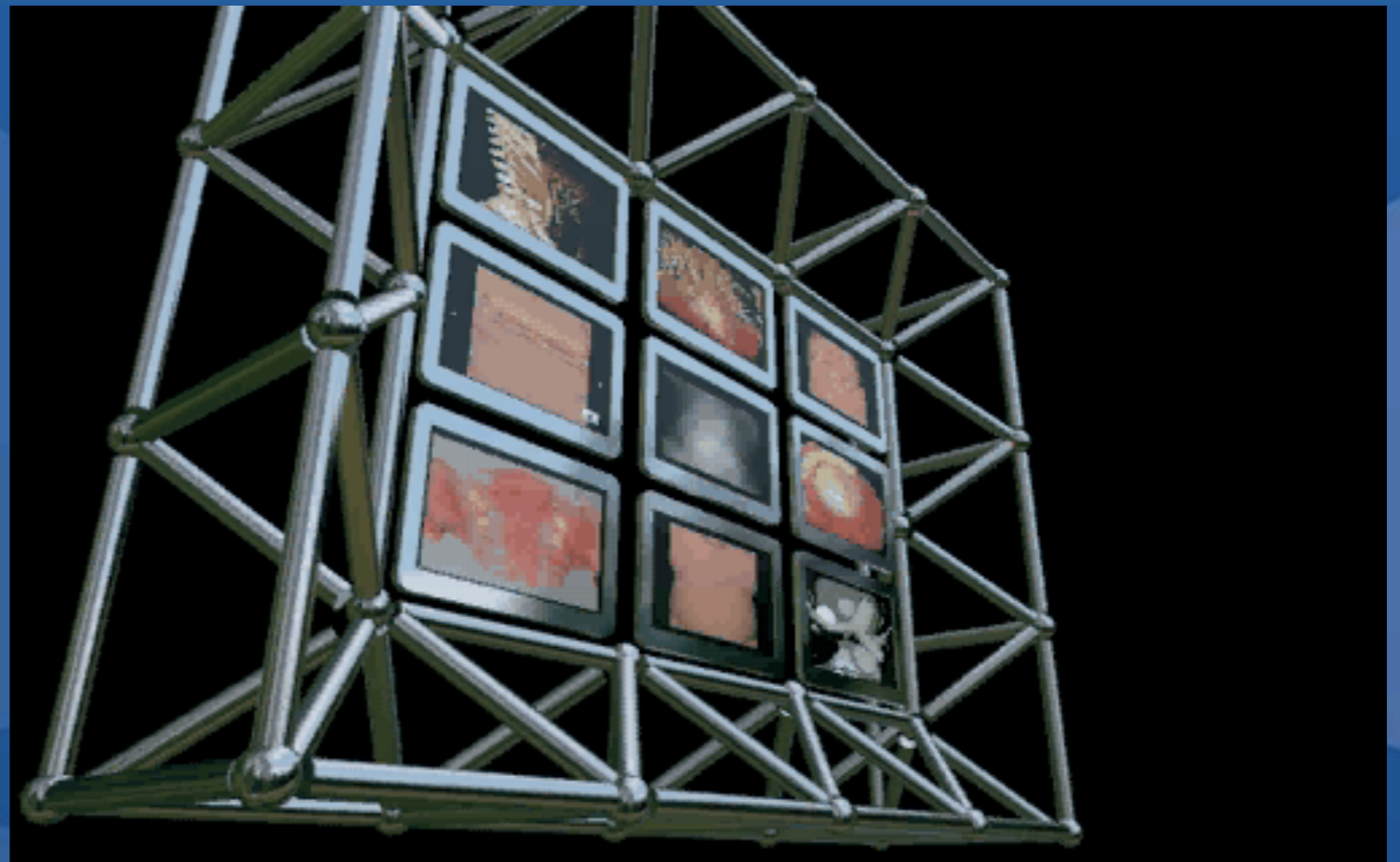
SIR 36TH ANNUAL SCIENTIFIC MEETING
IR RISING:
LEADING IMAGE GUIDED MEDICINE
CHICAGO, ILLINOIS • MARCH 26-31, 2011
SOCIETY OF INTERVENTIONAL RADIOLOGY

CTA/MRA: Image Reconstruction, Post-Processing, Workflow

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Indianapolis, IN*

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Stanford, CA*



*SIR 2010 27-28 March 2011
0800-1000*

Disclosures: None

Online Handouts from Lecture:

www.stanford.edu/~hallett

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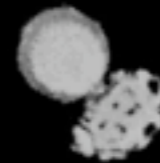
Outline

Outline

**I. Image
reconstruction**

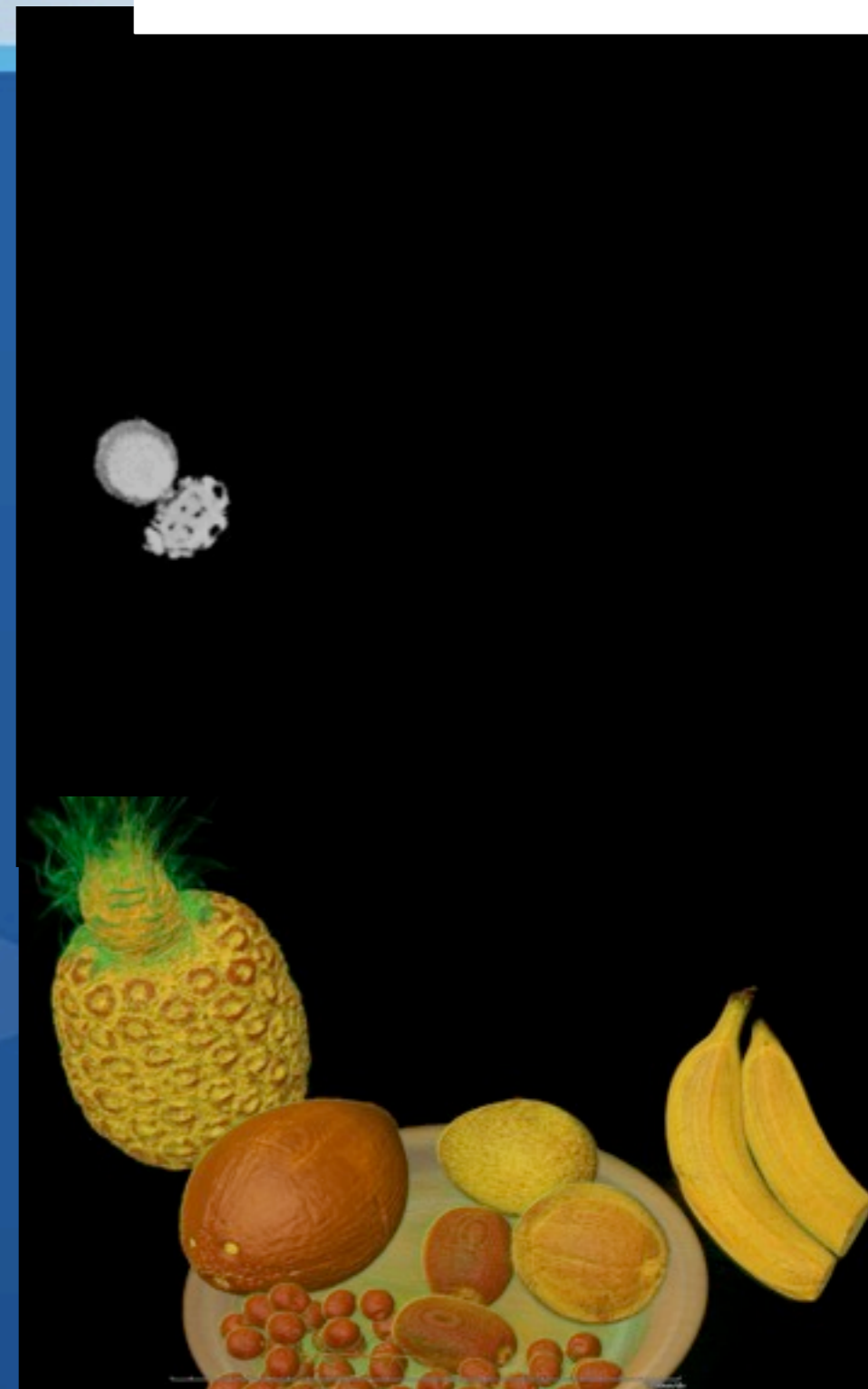
**II. Post-processing
techniques**

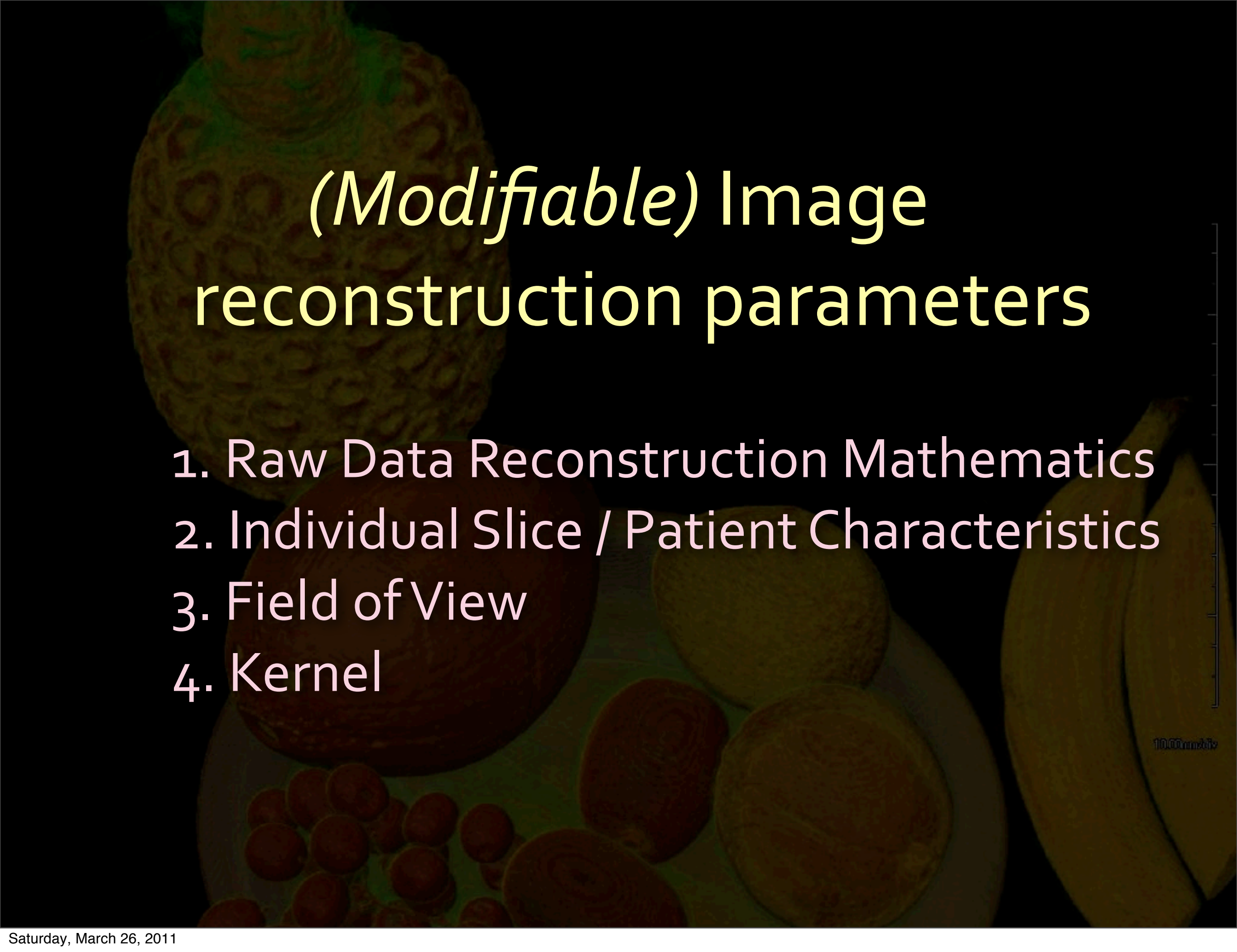
**III. Workflow /
Interpretation**



Outline

- I. Image reconstruction
- II. Post-processing techniques
- III. Workflow / Interpretation

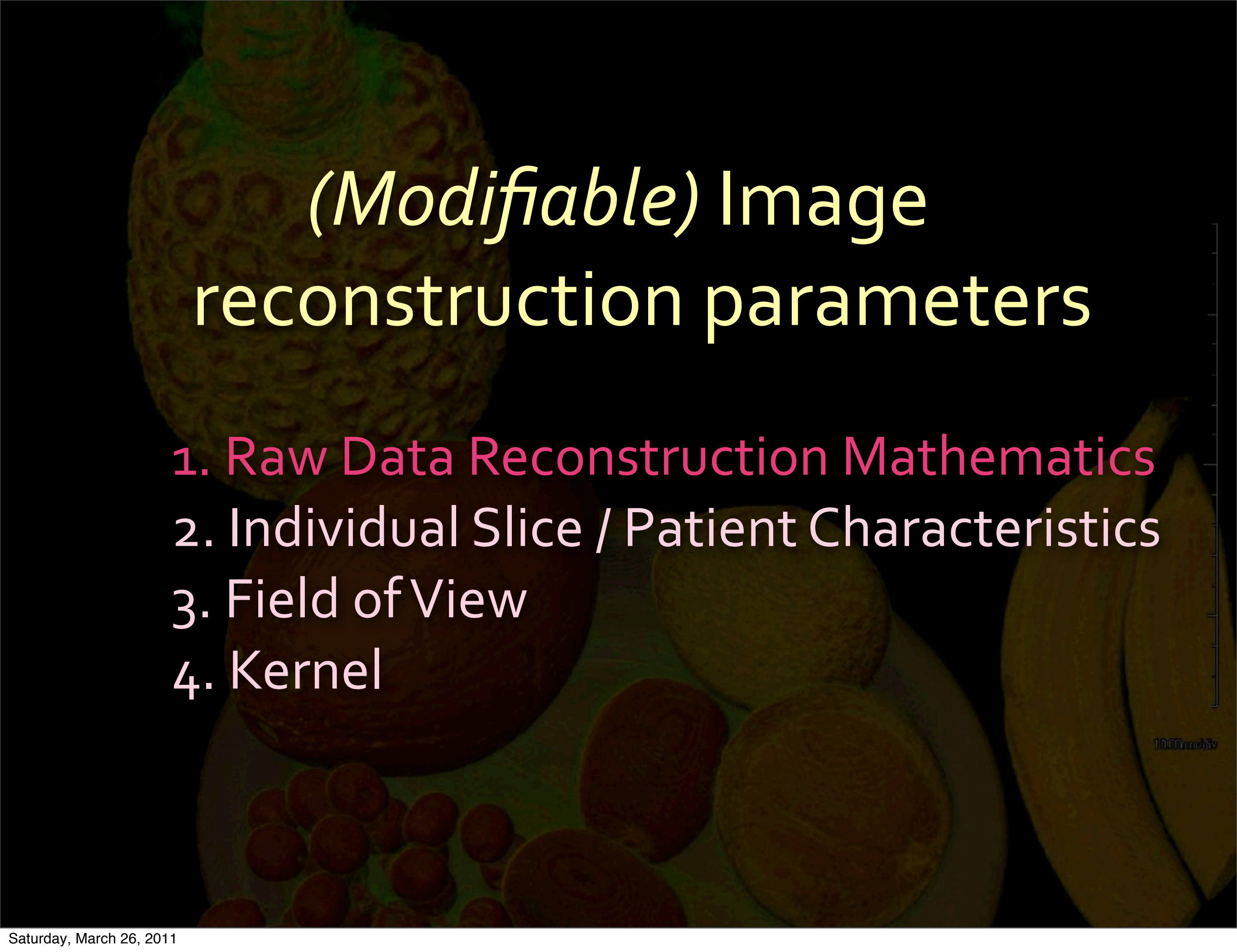




(Modifiable) Image reconstruction parameters

1. Raw Data Reconstruction Mathematics
2. Individual Slice / Patient Characteristics
3. Field of View
4. Kernel

1000mm/s



(Modifiable) Image reconstruction parameters

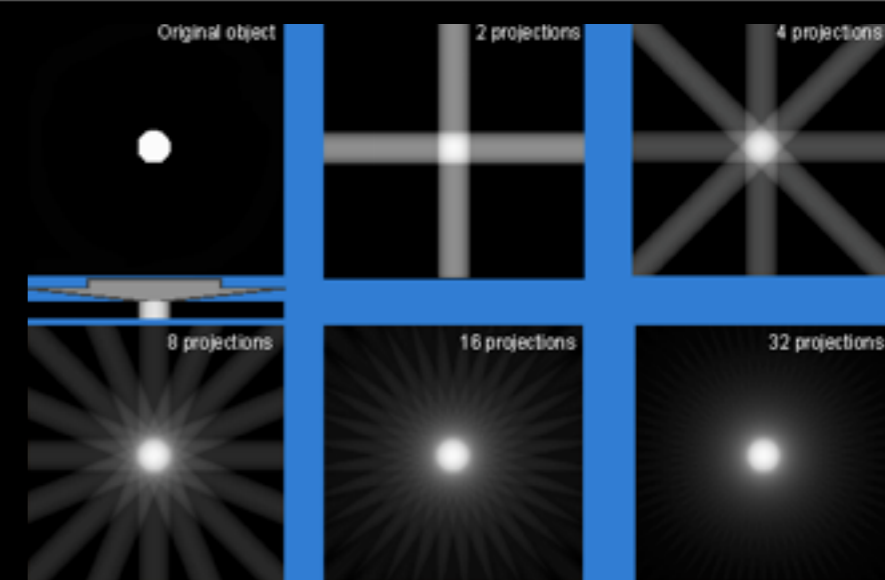
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100mm/s

TRADITIONAL

Raw Data Reconstruction

- Traditionally reconstructed using Filtered Back Projection (FBP)
- Necessary ASSUMPTIONS:
 - Focal spot infinitely small
 - Detector is single point in center of detector cell
 - Reconstructed voxel - no shape or size
 - Measured signal has no error from photon statistics or image noise



“New” Data Reconstruction

- Iterative Reconstruction (IR)
 - Used in SPECT and PET years ago.....
 - Models CT system optics (geometric information) as well as statistics (noise)
 - ➔ Compares model to real raw data, correct, repeat
 - ➔ Model can be *iterated* over and over until image is essentially constant
 - Reduced noise, but computationally expensive

Hara AK, et al. Am J Roentgenol. 2009;193(9):764-771

Iterative Reconstruction

- Up to 50% dose reduction is possible at same image noise

OR:

Improved image quality at same dose

- 40% improvement in low contrast detectability



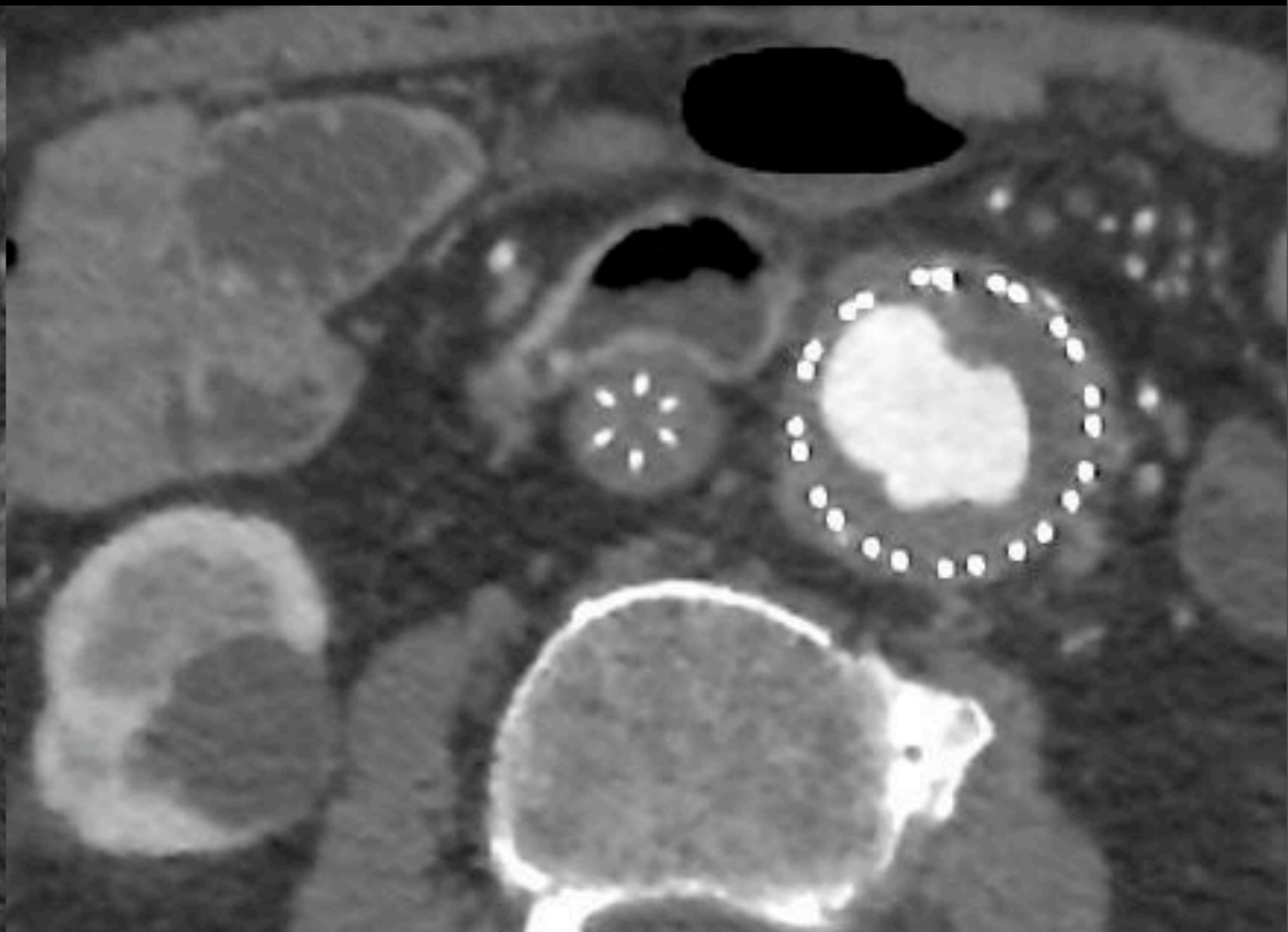
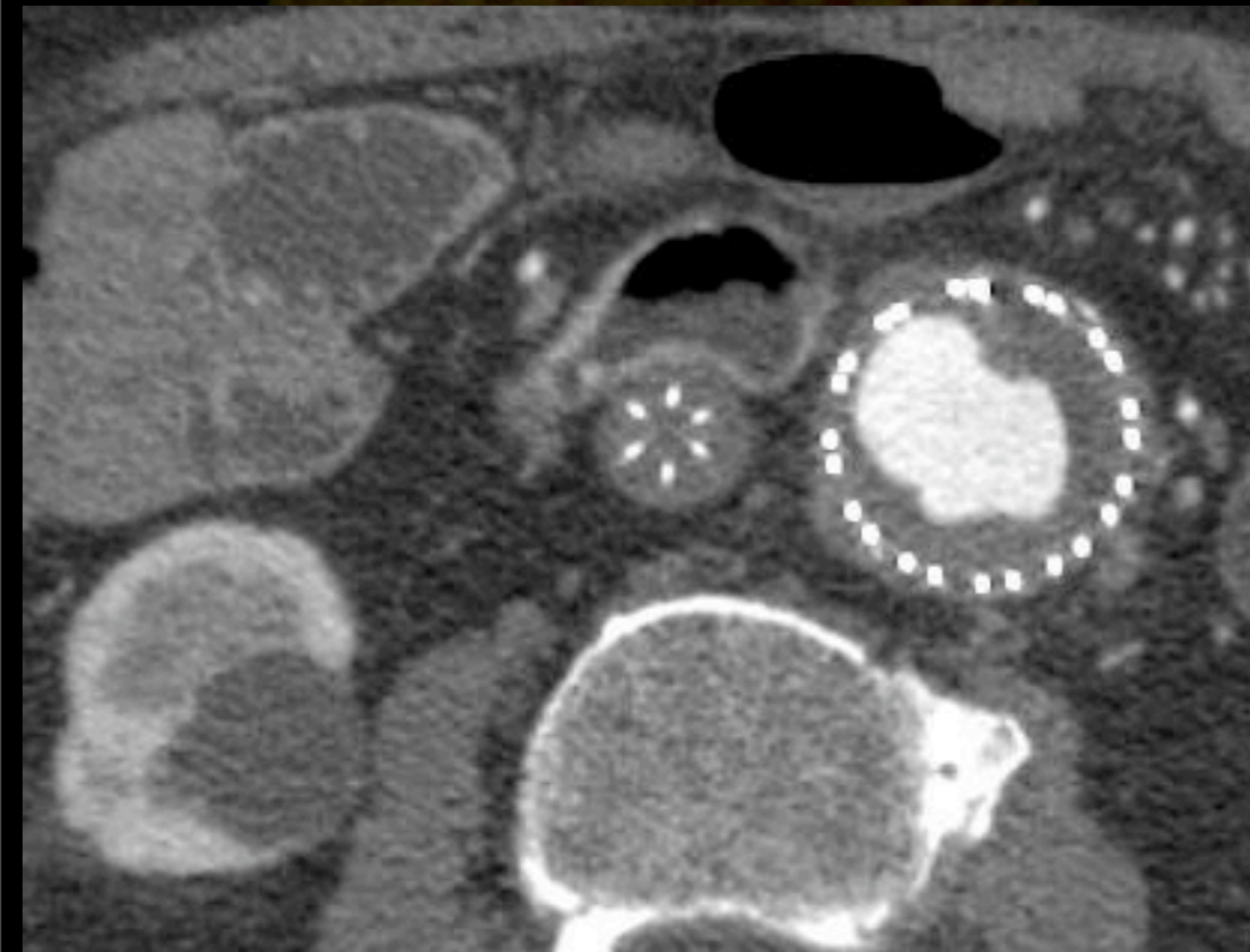
2007, Std.
Technique
CTDI=19



2008
ASiR
CTDI=9

Images courtesy of Mayo Clinic Arizona

Iterative Reconstruction:

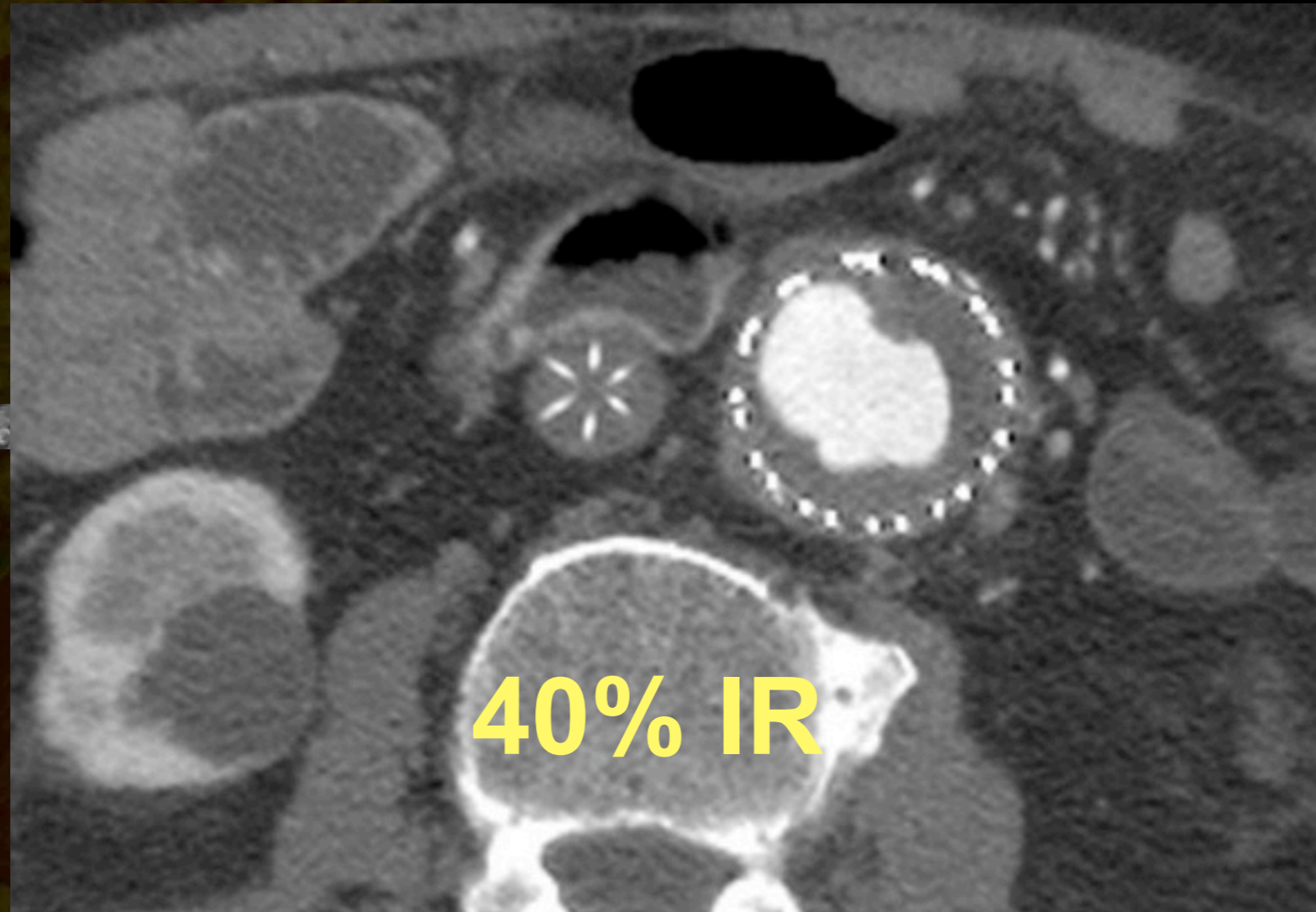


0% IR

**100%
IR**

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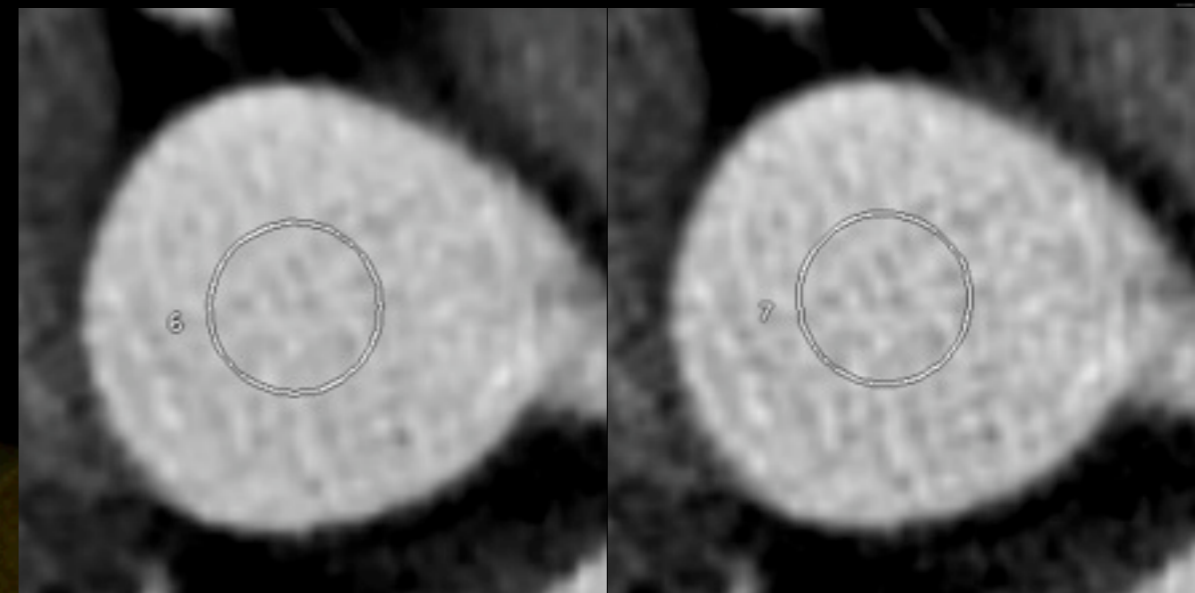
Iterative Reconstruction:



100mm/div

Iterative Recon for CCTA: the ERASIR STUDY

- 574 consecutive pts at 3 sites referred for CCTA: FBP vs. 40% ASiR blend
- 27% dose reduction from IR utilization, without increased image noise or non-evaluatable segments
- 45% total reduction including other scan parameters (100 kV, etc)

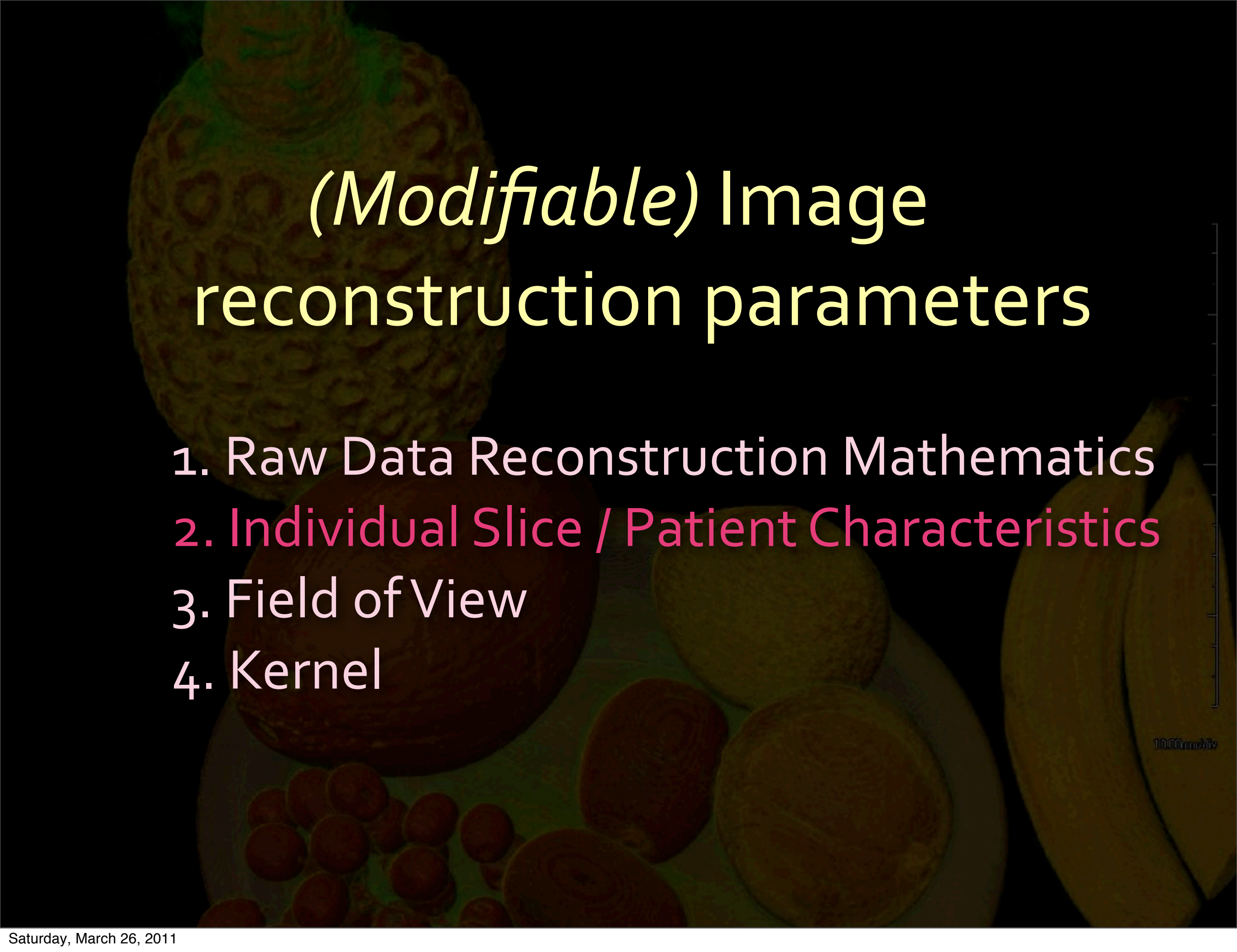


FBP

40% ASIR

	FBP	40% ASIR
Density, HU	718.6	719.3
SD (noise)	52.3	38.5

Leipsic J, et al. AJR 2010; 195:655-660



(Modifiable) Image reconstruction parameters

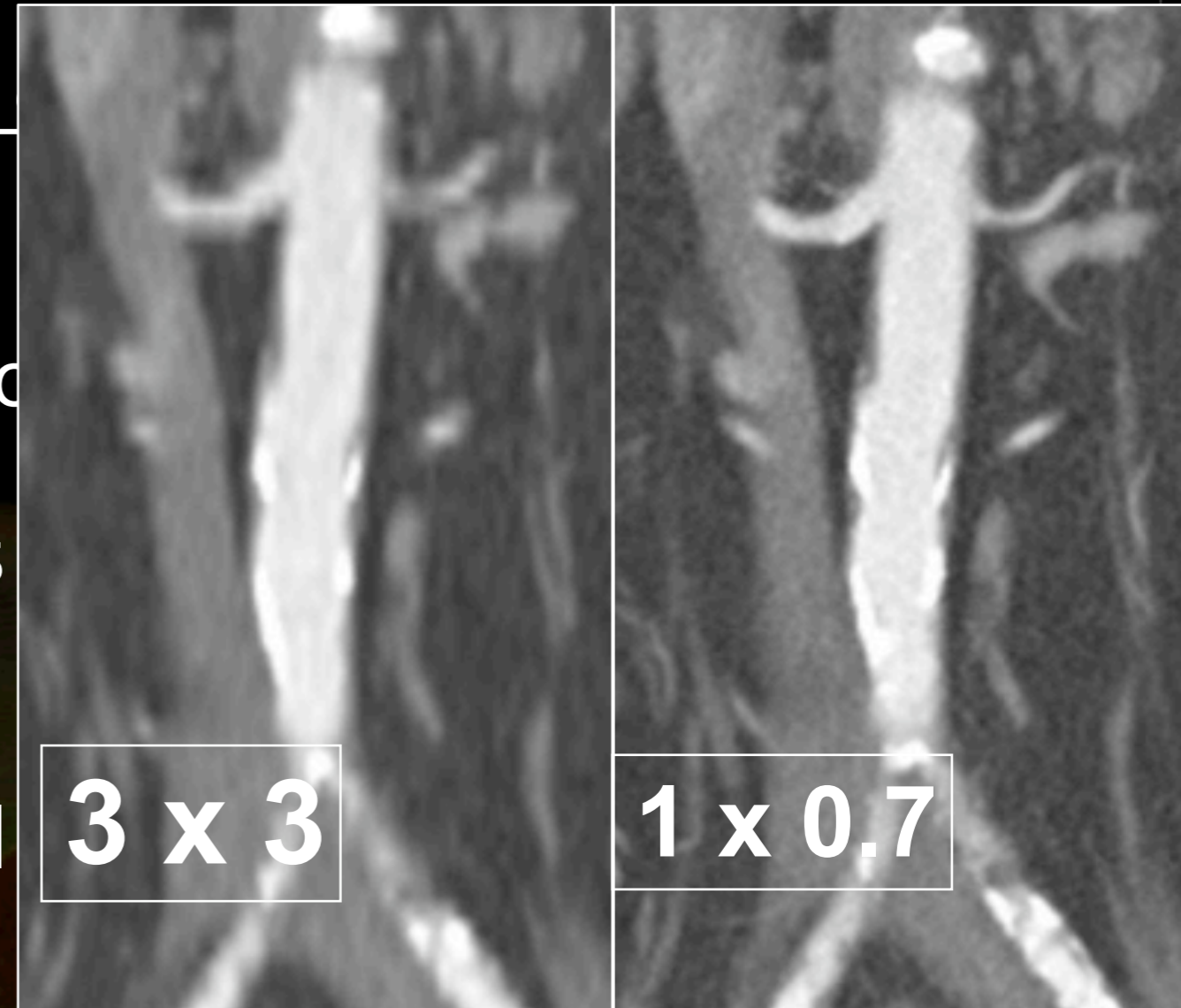
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Characteristics of the CT “slice” ...

- “Effective” slice thickness
 - defined by the selection of collimator thickness during scan acquisition
- Thicker (but not thinner) recons
- Multi-planar reconstructions (MPR) obtained by *interpolation*
- MPR enhanced if your initial dataset is overlapped by ~ 30%
 - e.g. 1mm ST at 0.7 mm RI
 - Less “aliasing” (stairstep)

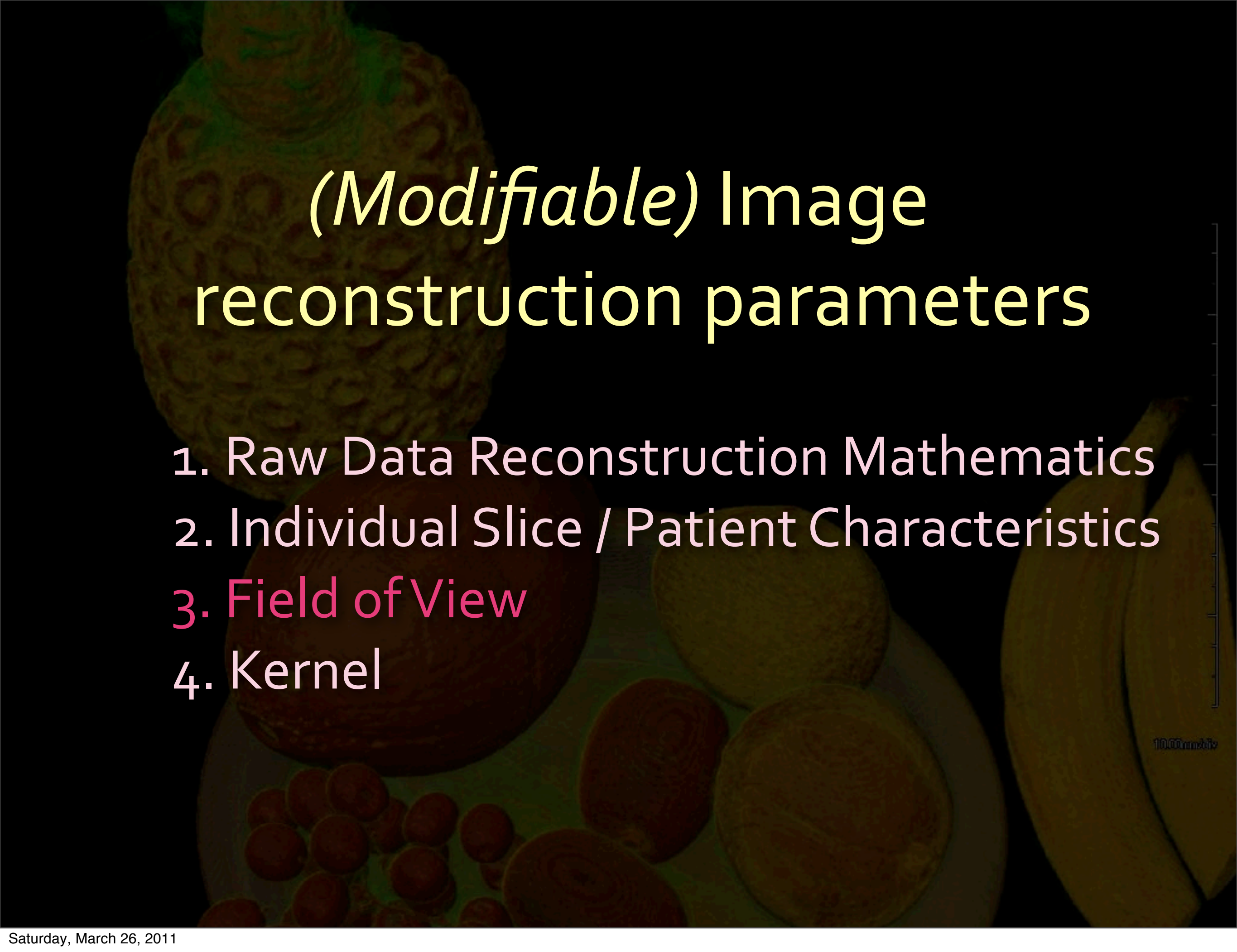
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Tweaking / Help for Tough Datasets

- **LARGE** Patients:
 - Scan with thicker collimation (1.25 - 2.5 mm)
 - Use 140 kV
 - Slow down gantry rotation
- Smaller Patients:
 - Use 100 kV



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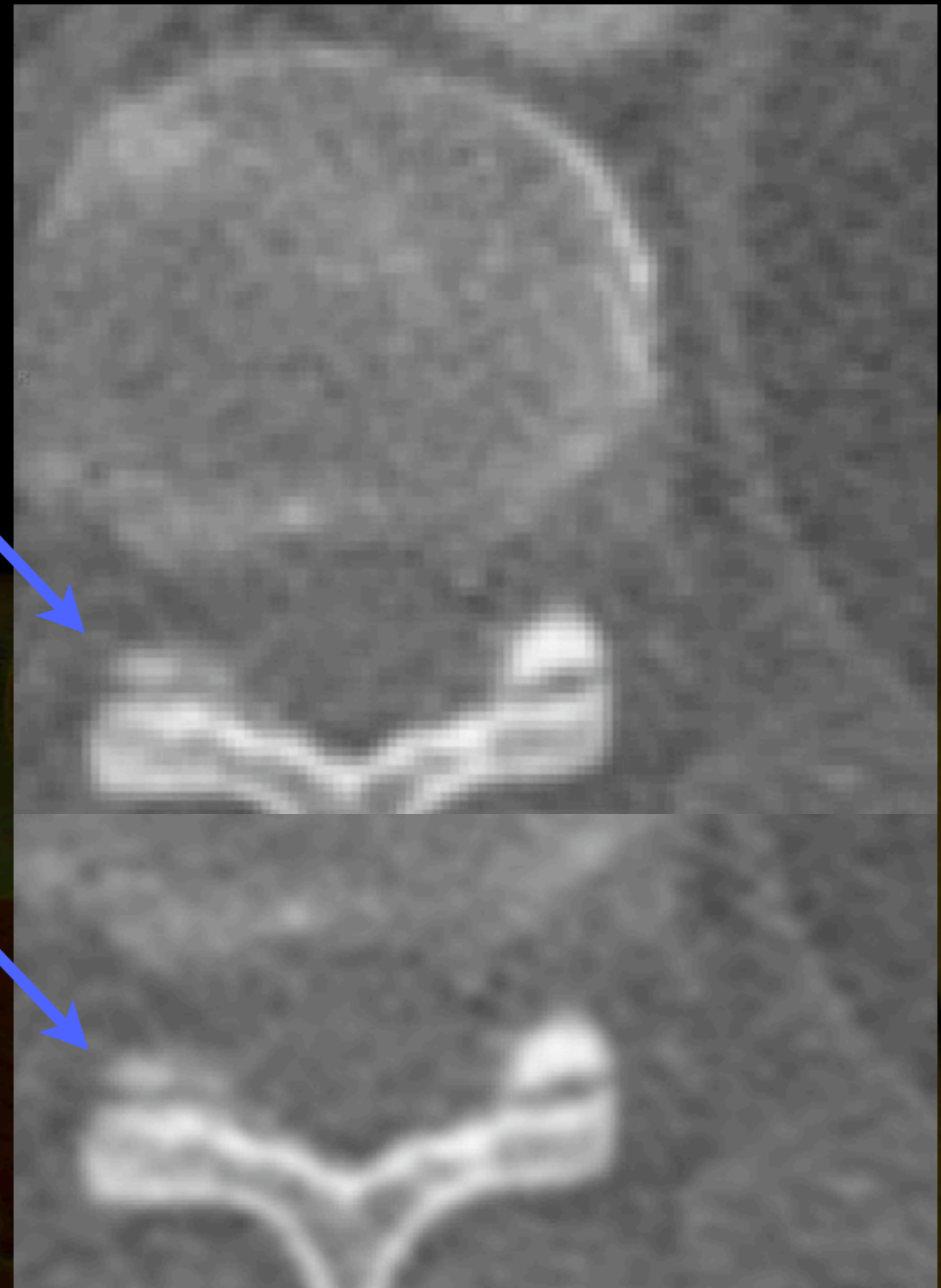
Effect of changing FOV

- Standard CT image:
 - 512x512, FOV = 30 cm
 - Pixel size ~ 0.35 mm²
- Small FOV:
 - 512x512, FOV = 15 cm
 - Pixel size ~ 0.10 mm²
- BUT: "Isotropic" voxels easier to obtain at thicker slice / larger FOV

100mm/div

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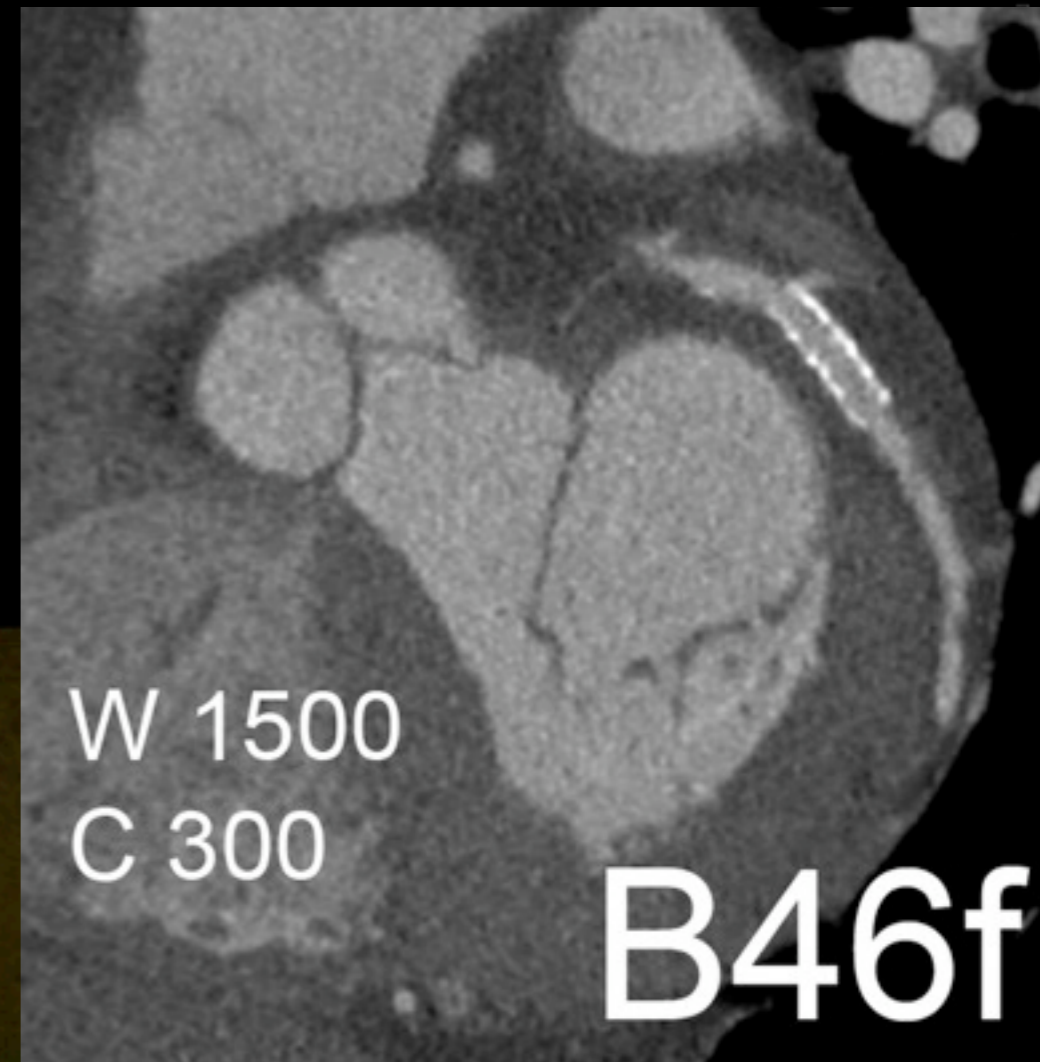


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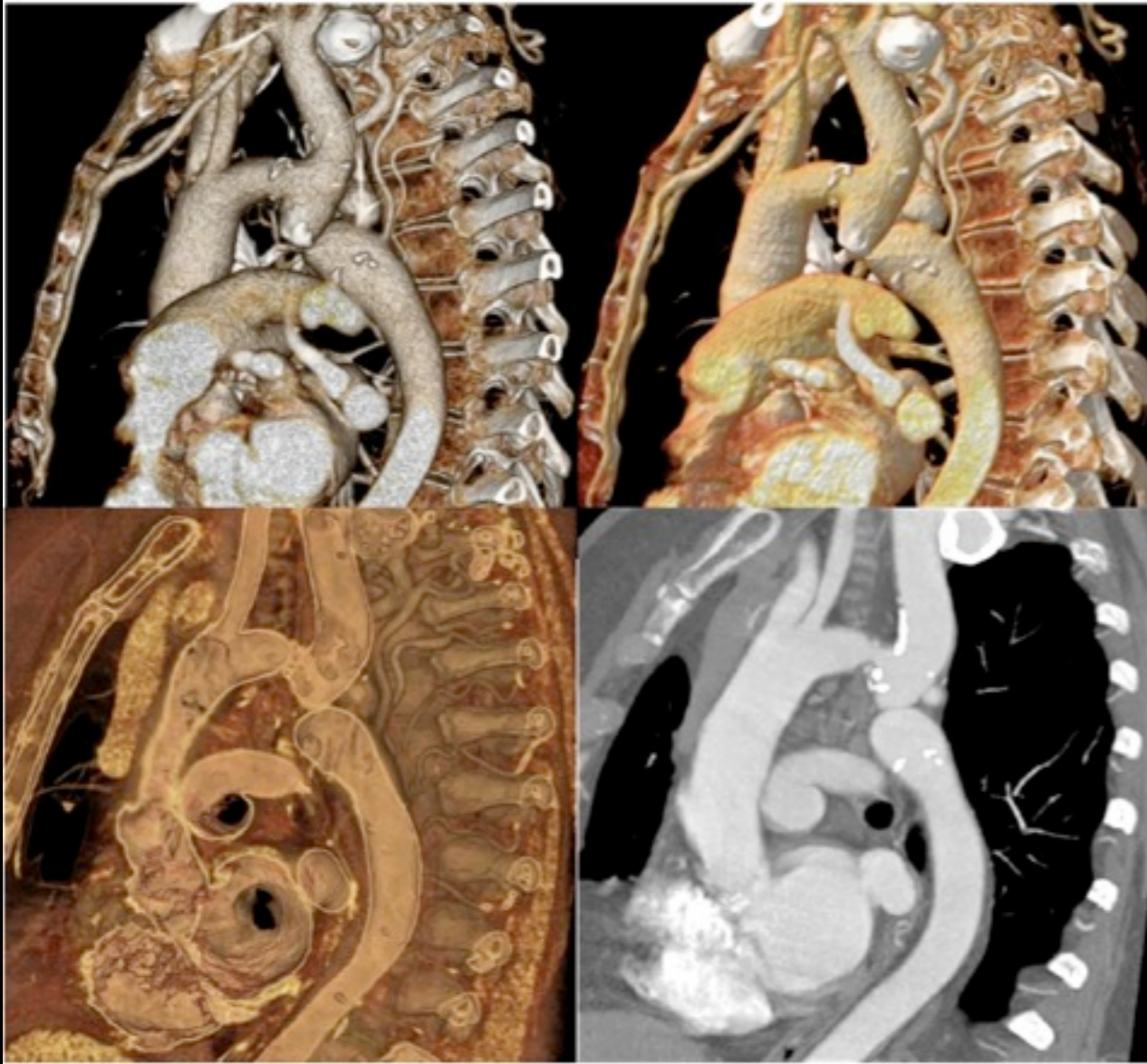
Effect of Recon Kernel

- **Softer kernel: Less noise, less sharp**
 - Better 3D / Multiplanar recons
- **Sharper kernel: Higher detail, more noise**
 - **STENTS!!** (coronary, peripheral)



Pugliese, F. et al. Radiographics
2006;26:887-904

Image Post-Processing



Review of Image Types
New Directions

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Reconstruction “Alphabet Soup”

- MPR
- MIP
- MINIP
- AIP (R)
- CPR
- VR
- BPI-VI
- 4-D



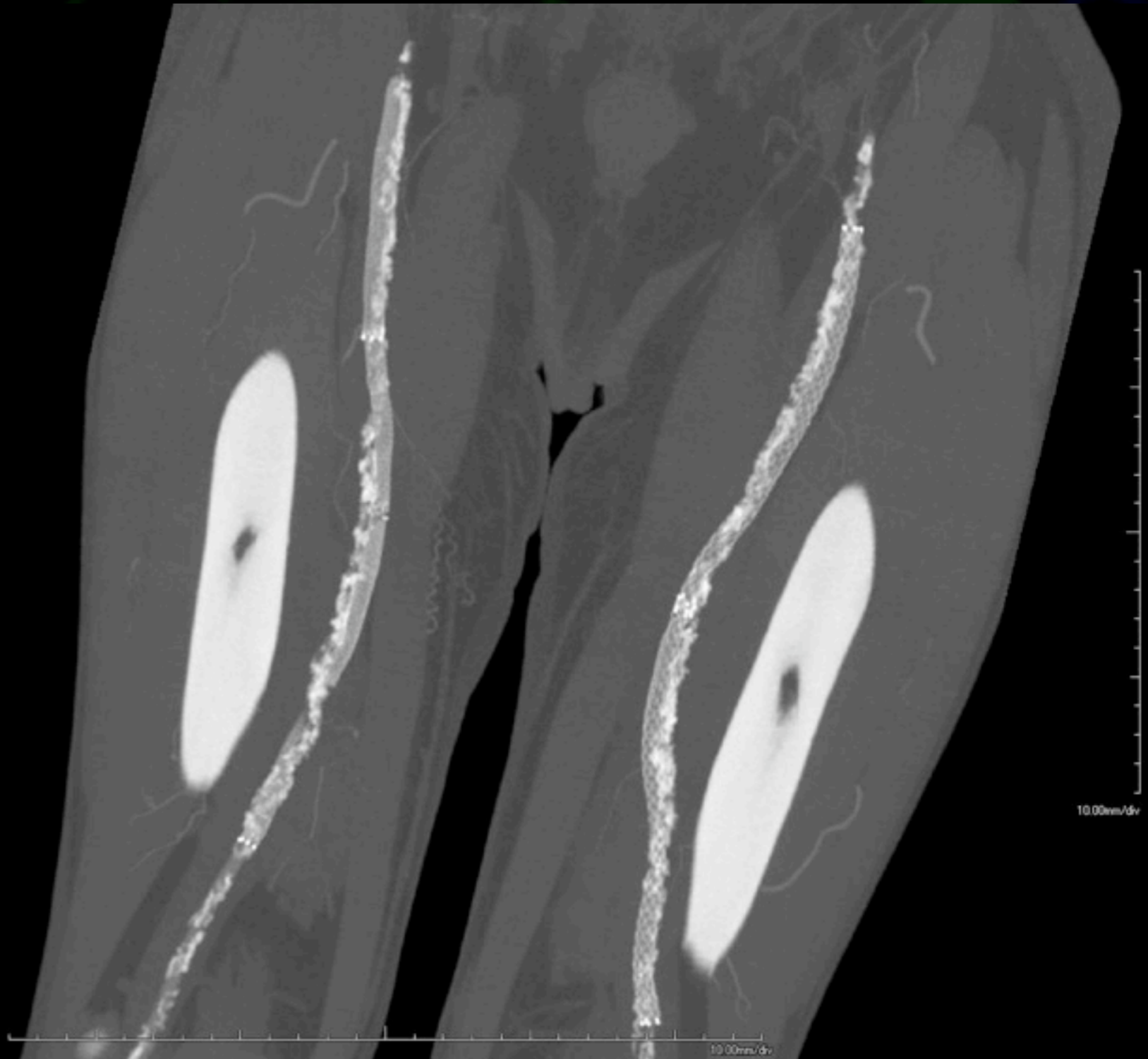
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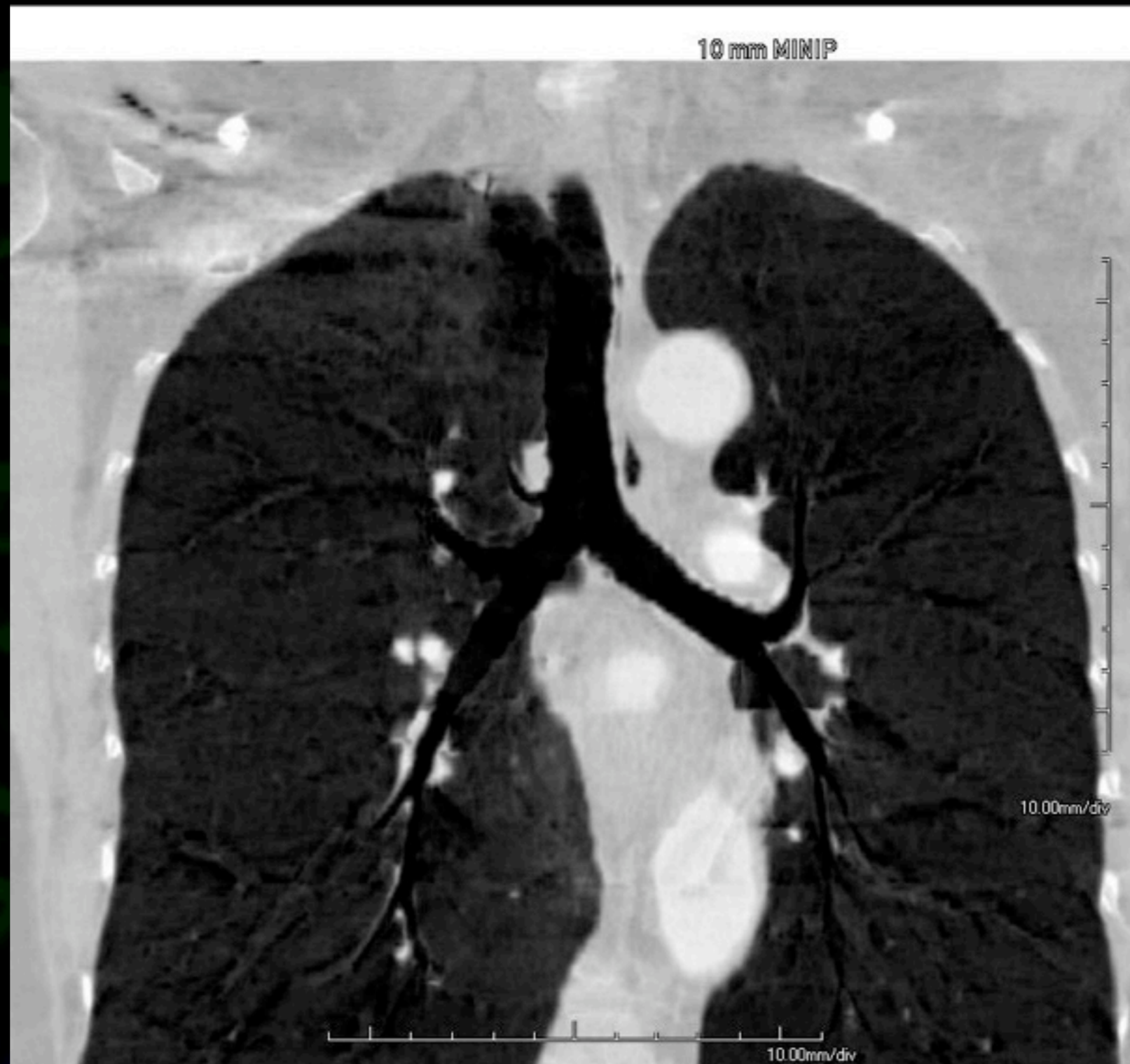
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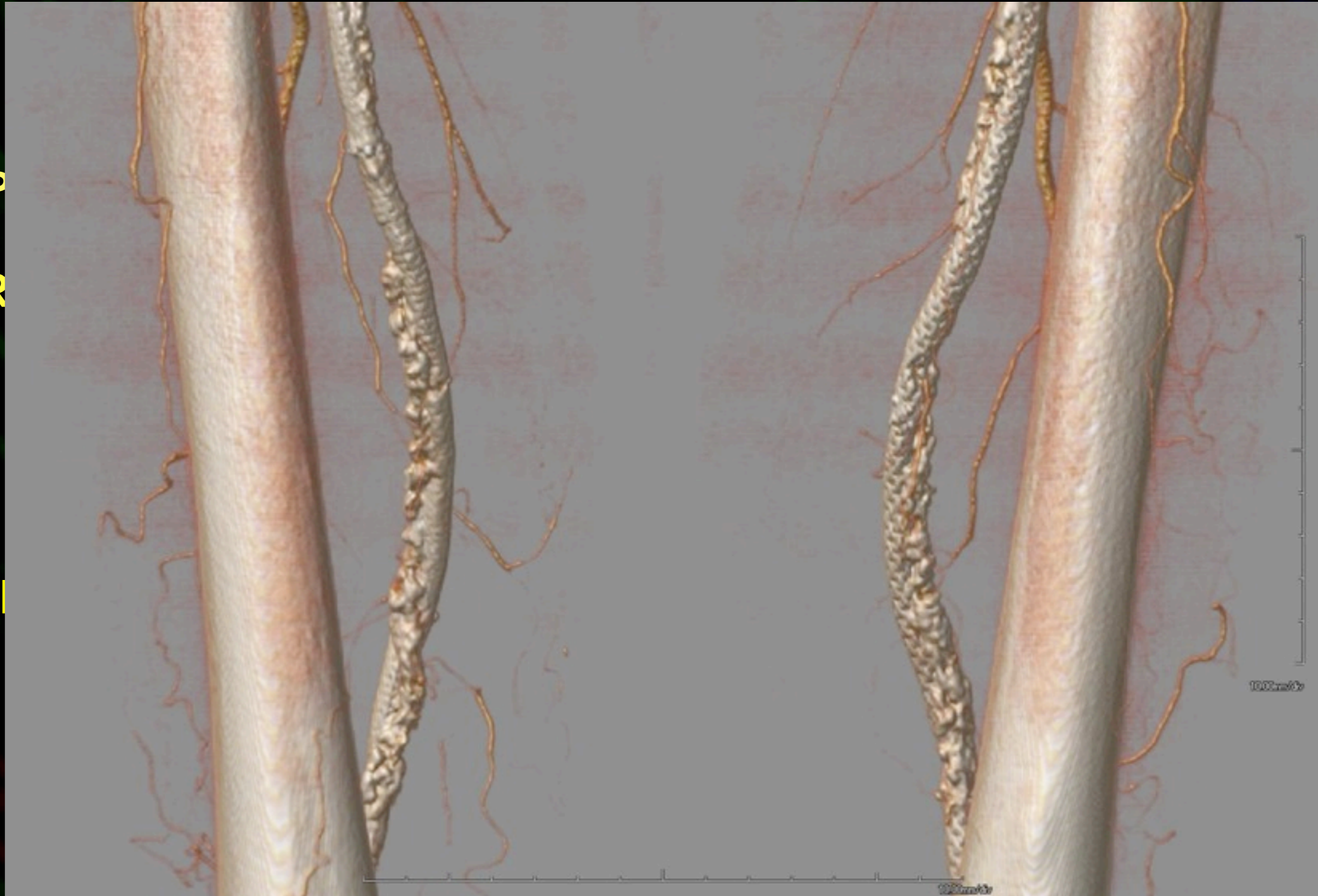
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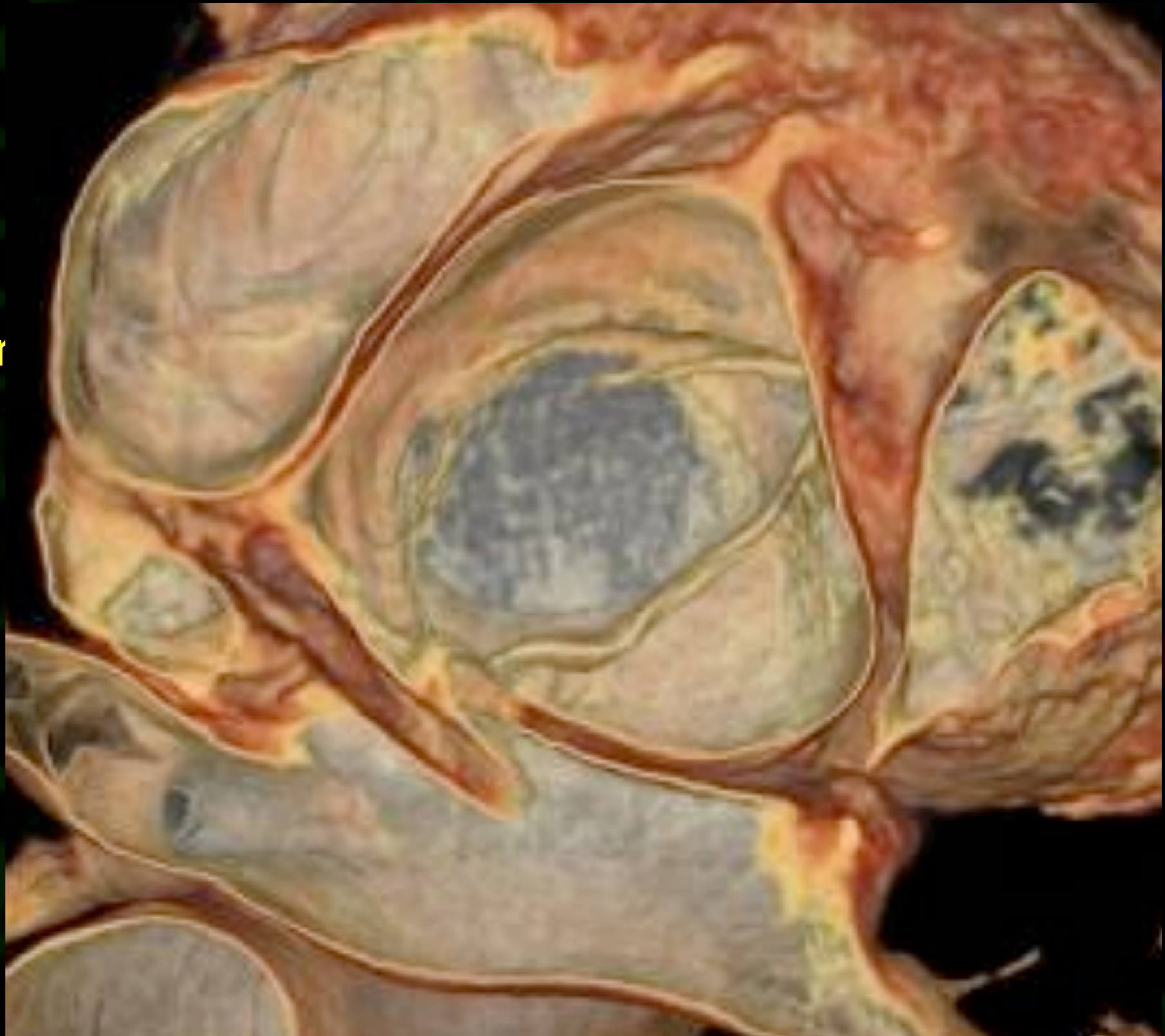
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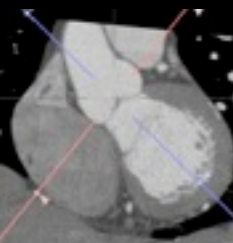
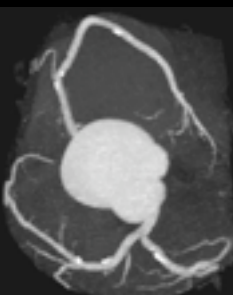
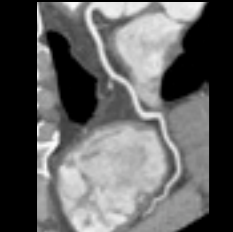
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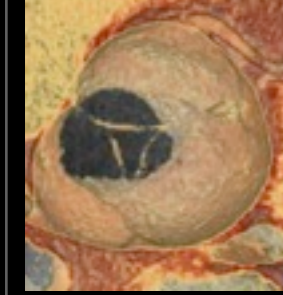


Reconstruction “Alphabet Soup”

- 4-D

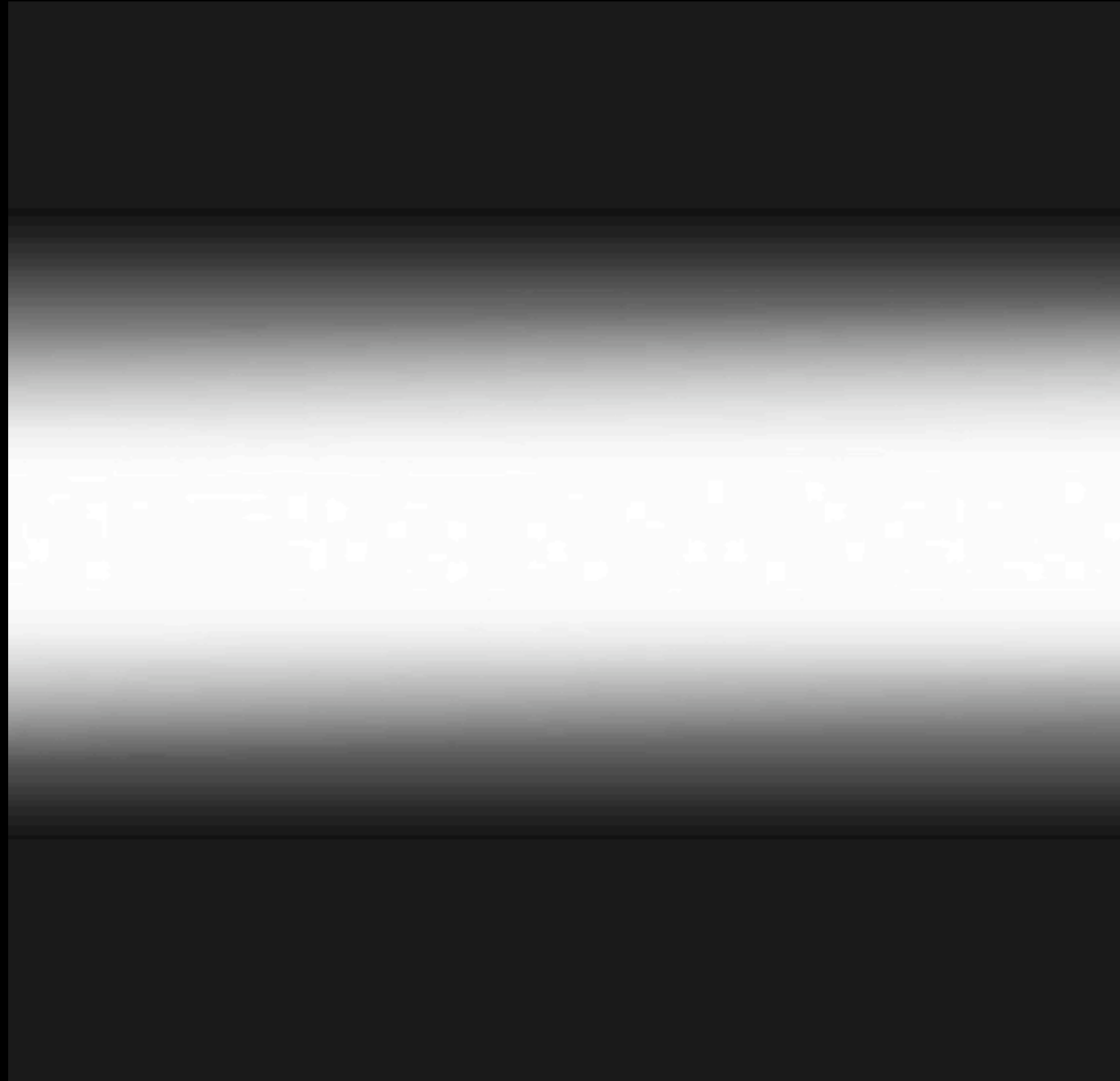


	Major Uses	Advantages	Disadvantages
<p>MPR</p> 	<p>Stenosis, vessel wall analysis</p> <p>Lung nodule measurement</p> <p>Orthogonal Measurements</p>	<p>Accurate for stenosis, nodule, orthogonal measurements</p> <p>Calcification, stent evaluation</p> <p>“Thick MPR”: salvage noisy datasets</p>	<p>Limited spatial relationships</p> <p>Limited display if curving vessel</p>
<p>MIP (MINIP)</p> 	<p>Angiographic overview, contextual with adjacent structures</p> <p>Lung nodule detection (coronal STS)</p> <p>Valves, Airways (MINIP)</p>	<p>Depicts course of small and/or poorly enhancing vessels</p> <p>Object - background contrast</p>	<p>Vessel, bone, visceral overlap</p> <p>Limited stent, calcium evaluation</p> <p>Stenosis Overestimation</p> <p>NOISE IS ADDITIVE!!</p>
<p>CPR</p> 	<p>Flow lumen, vessel wall analysis</p> <p>Curved Objects</p>	<p>Best for mural stenosis, occlusions, calcifications, stents</p> <p>• Slice through display (perpendicular to CPR)</p>	<p>Distortion of extra-vascular structures</p> <p>Dependent on accurate centerline (Needs Oversight)</p>

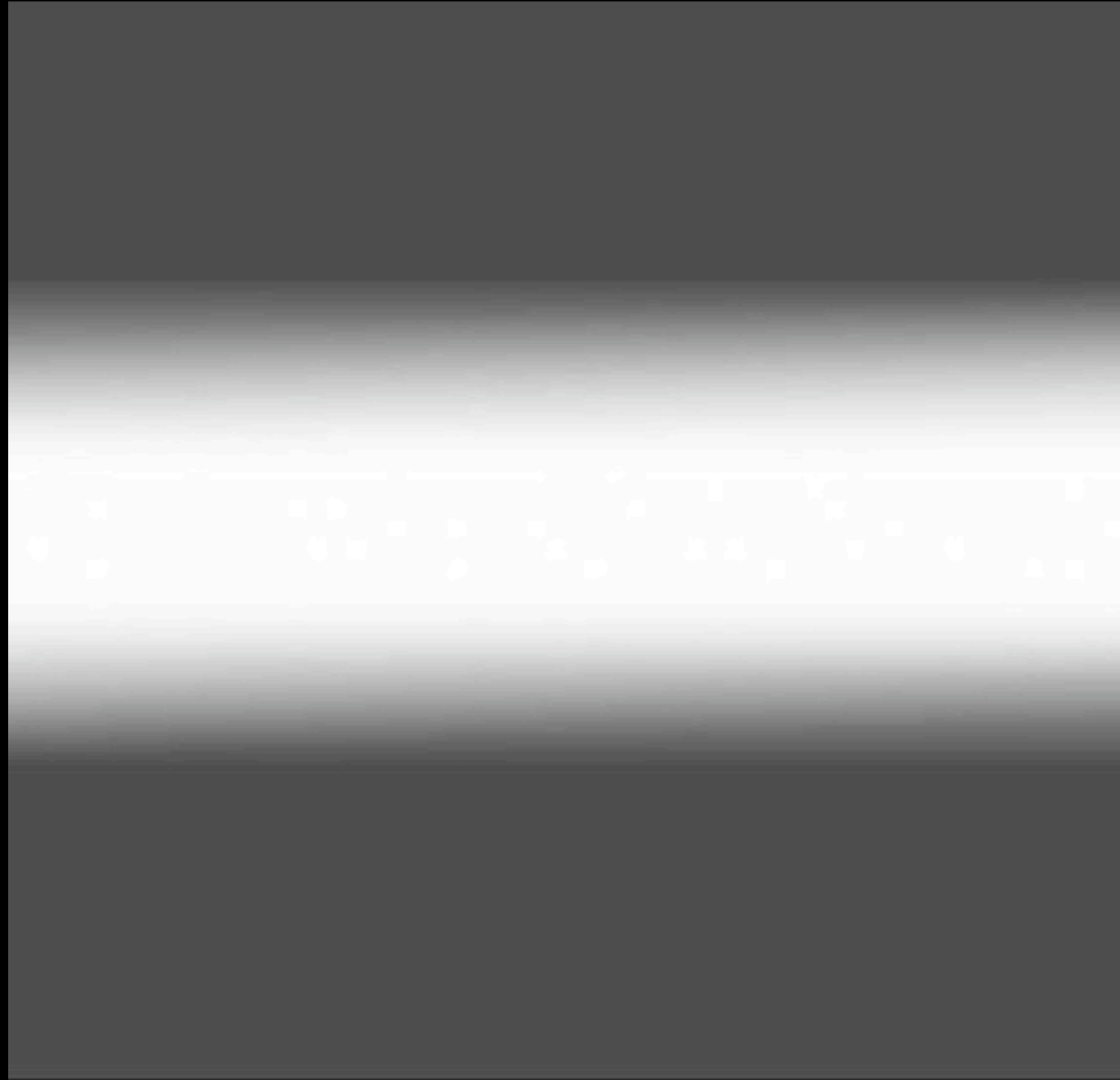
	Major Uses	Advantages	Disadvantages
<p>VR</p> 	<p>Angiographic overview, contextual with adjacent structures</p> <p>Pre-procedural planning</p>	<ul style="list-style-type: none"> • Best for complex relationship display • Valves • Vessel Origins • EVAR, DSX, etc 	<p>Opacity transfer function and operator dependent</p> <p>No accurate measurements</p>
<p>BPI-VR</p> 	<p>Valves, vessel orifices, DSX flaps</p>	<p>WOW factor</p>	



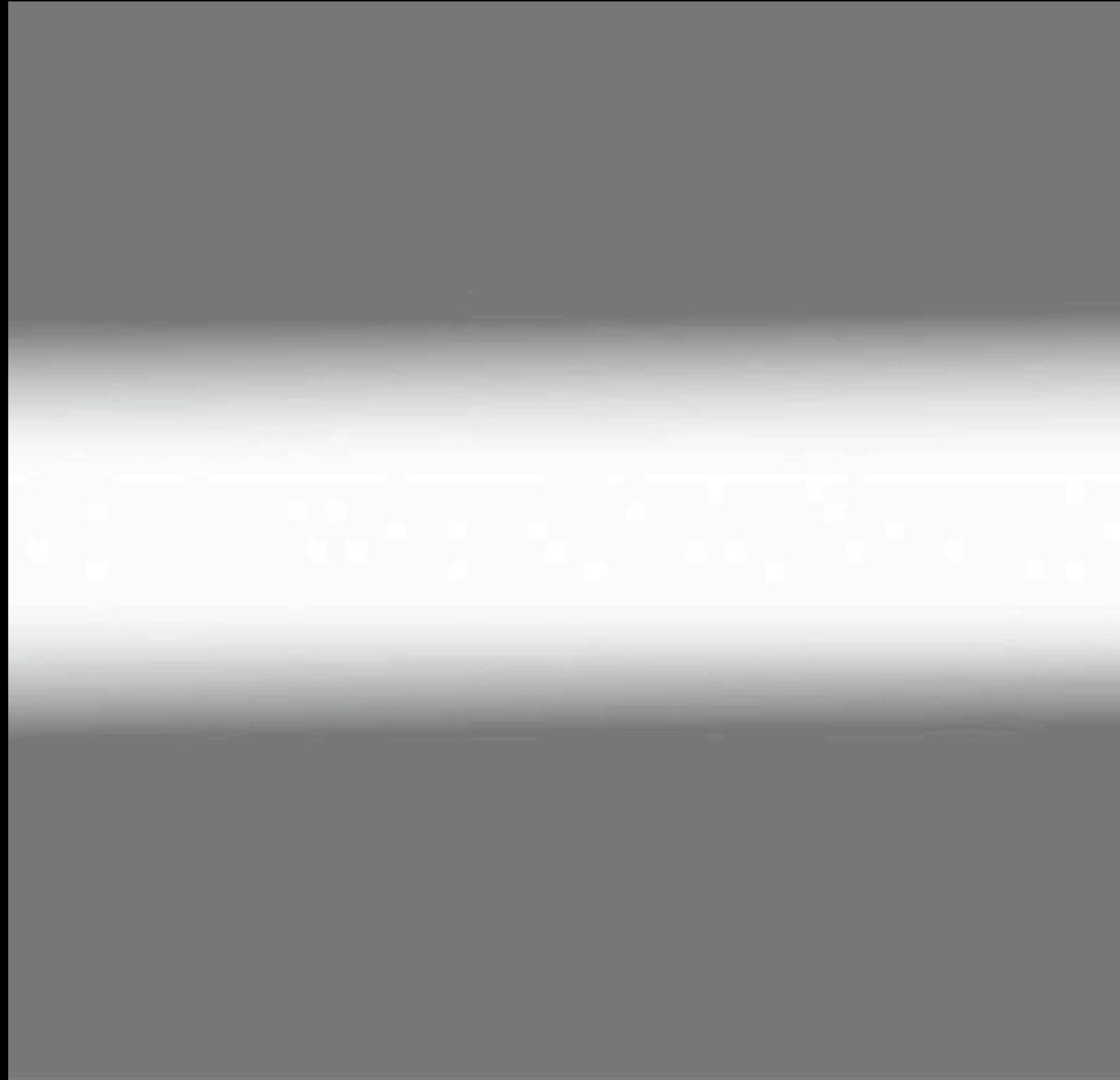
Caveat for MIP: Effect of Background Noise on apparent stenosis



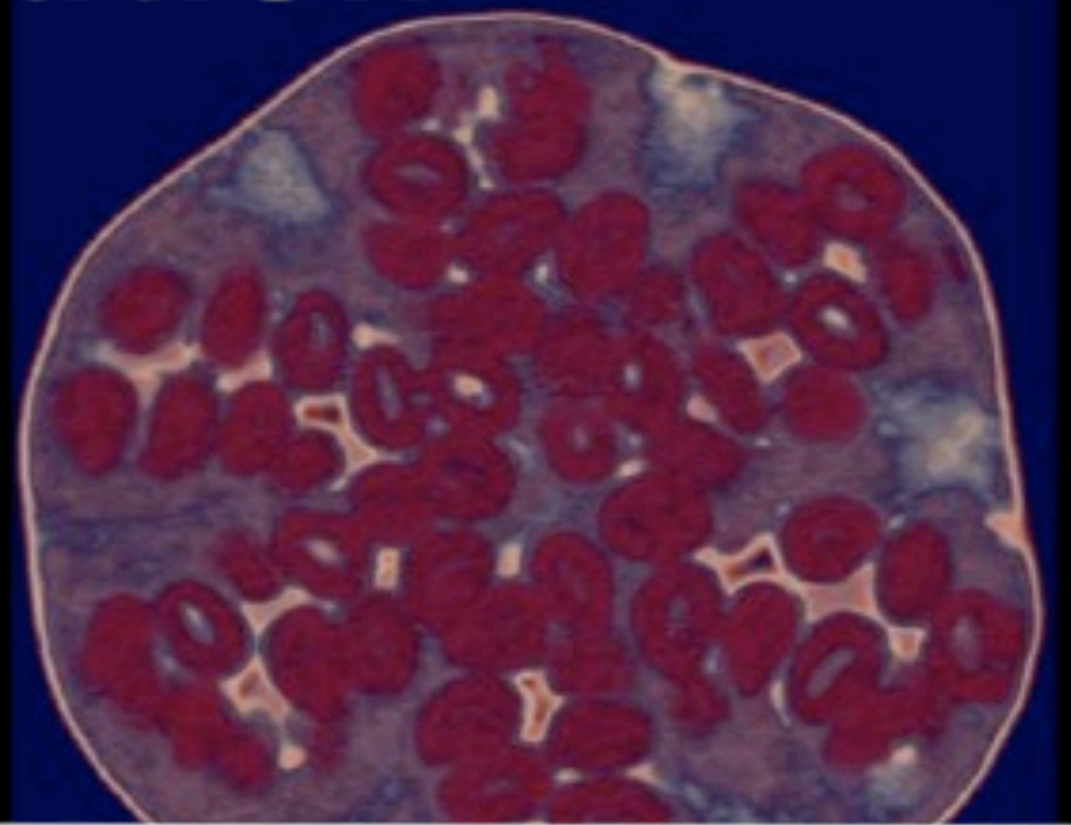
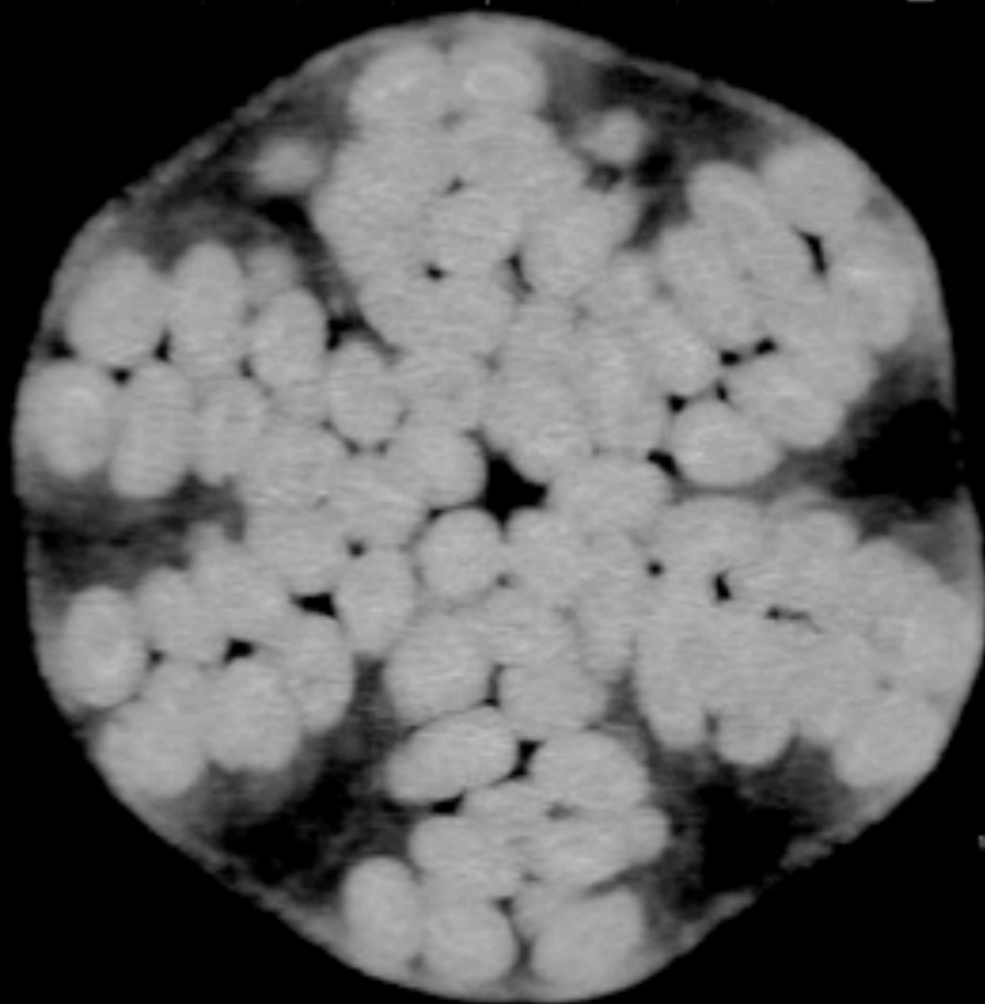
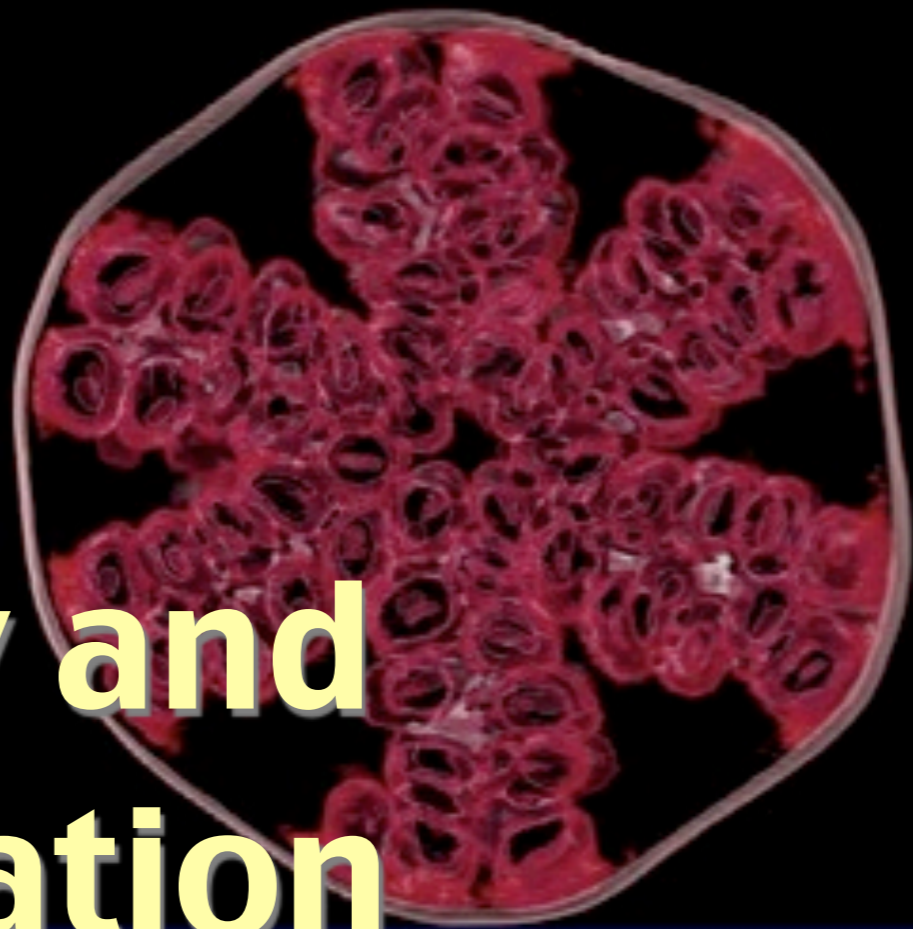
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Caveat for MIP: Effect of Background Noise on apparent stenosis



CTA Workflow and Interpretation



Online Handouts from Lecture:
www.stanford.edu/~hallett

Goals of CTA workflow

- Process studies efficiently
- Capture all appropriate charge codes
- Provide access to thin-slice datasets for radiologist interpretation and review
- Provide timely reports to referring clinicians / services

Coordinated Efforts Yield Best Results

- **Physician-directed** - for primary interpretation
- **Technologist-directed** - for protocol-driven reconstructions and measurements

Physician -Directed CTA

- Volumetric Interpretation via:
 - Workstation
 - Thin Client - Server
 - PACS
- Like Ultrasound, “Clarify” images obtained by 3D Lab / Techs
- Output:
 - Sent to PACS, emailed to referring MD
 - can also real-time “consult”

Technologist (3D Lab) Tasks

- Template-Driven processing of cases:
 - Segmentation
 - Detailed measurements, volumes
 - Consistent output format
- Triage urgent exams
- Temporal tracking of measurements (AAA)
- Transfer of data to MDs, clinical reports, and PACS

Interpretation: How I do it.....

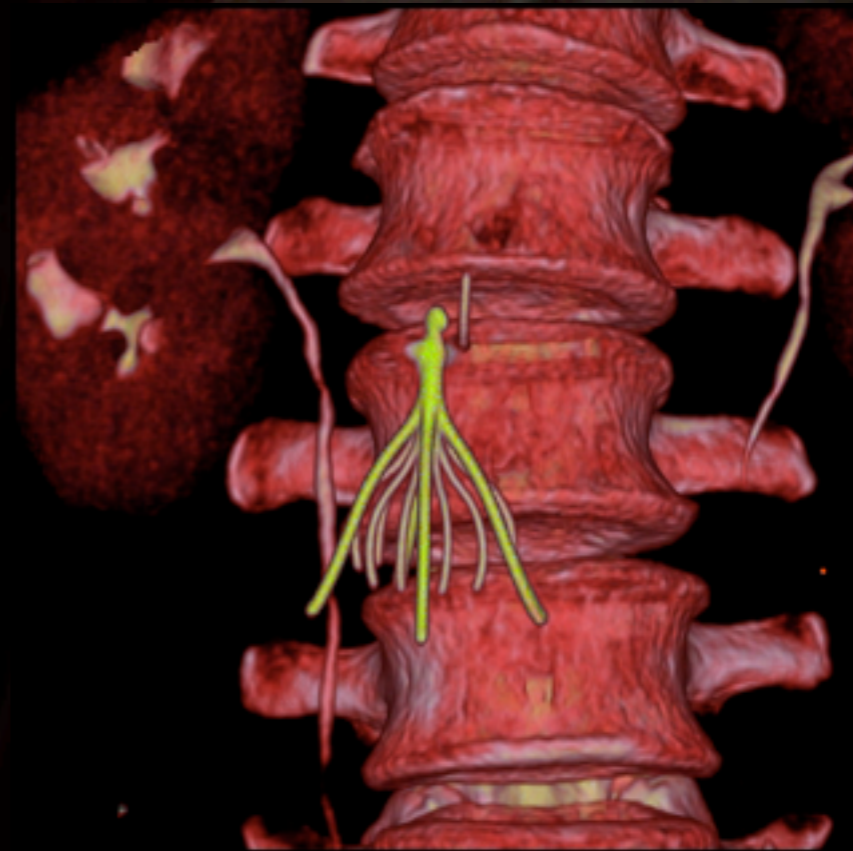
- RTs: process CPR, MIP, volumes
- Read from thin client whenever possible
- VR Overview then review axials
- Targeted interactive STS MIP and MPR evaluation of abnormalities
- My pertinent images - sent to PACS as a series
- VR images, stenosis evaluation emailed to referring MD
- Web-based “consult” feature: Use for intra-op consultation

How you should do it.....

- Find a workflow that works for you
- Review all the data
- Be efficient
- Communicate your results!

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Conclusions

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- Image Reconstruction:
 - Use iterative reconstruction- save dose and/or improve quality
 - Improve and troubleshoot image reconstruction
 - Remember inherent advantages, limitations, and differences in each type of image display

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- Workflow:
 - View 3D like ultrasound- develop, train, trust techs

1000mm/s

Conclusions

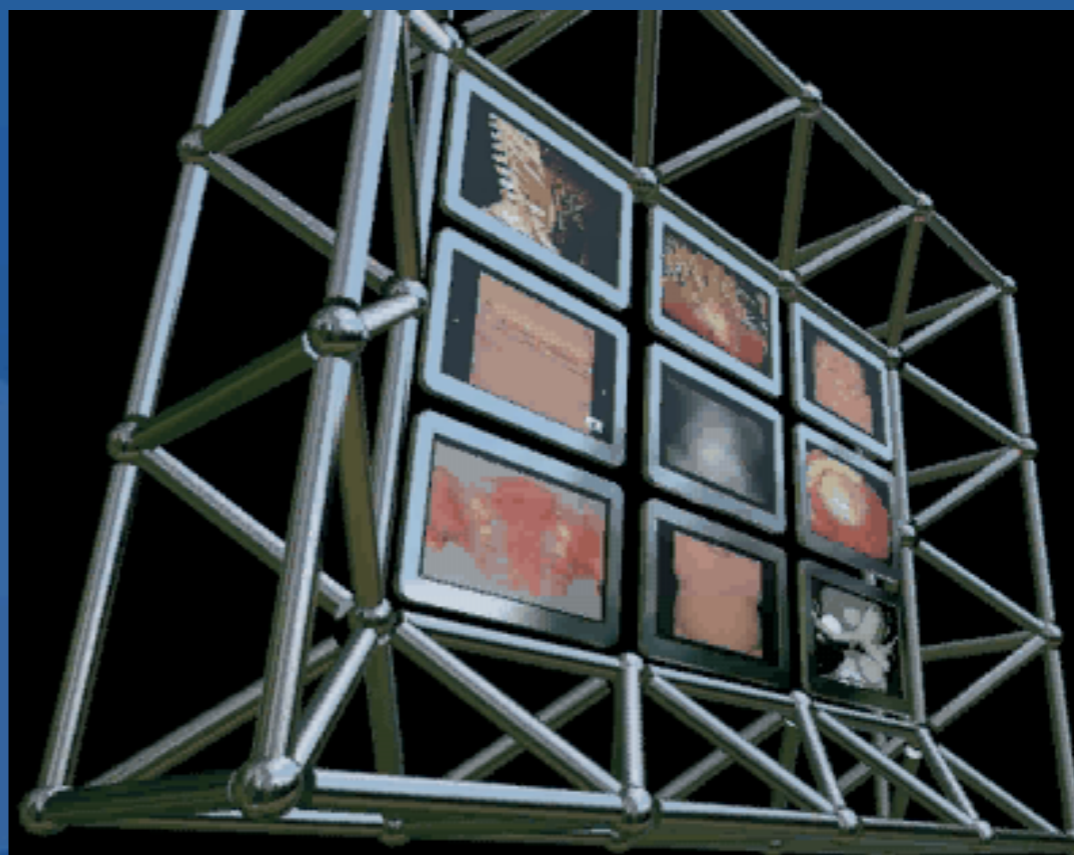
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 - Improve and troubleshoot image reconstruction
 - Remember inherent advantages, limitations, and differences in each type of image display
- Workflow:
 - View 3D like ultrasound- develop, train, trust techs
- Interpretation:
 - Develop a consistent reading algorithm, always have the source (thin) data available
 - Share your results!

1000mm/s



***Special
Thanks:
TeraRecon
Vital Images***

*Online Handouts from Lecture:
www.stanford.edu/~hallett
Choose "SIR 2011"*



Further Reading:

- Image Reconstruction:

- Rubin GD, Sedat P, Wei JL: *Ch. 6. Postprocessing and Data Analysis*. In: Rubin GD and Rofsky N. CT and MR Angiography: Comprehensive Vascular Assessment Lippincott, Williams and Wilkins, 2008
- Barrett JF, *RadioGraphics* 2004;24:1679-1691
- Ch. 4: Image Reconstruction and Review. In: Lipson SA: MDCT and 3D Workstations. Springer, 2006.
- Luccichenti G, et al. *Eur Radiol* 2005; 15: 2146 - 2156
- Parrish FJ, *AJR* 2007; 189:528-534
- Dalrymple NC, *RadioGraphics* 2005;25:1409-1428
- Hara AK, et al. *Am J Roentgenol*. 2009;193(9):764-771
- Roos JE, et al. *Acad Radiol* 2009; 16 (6) 646-653.

100mm

Further Reading

- CTA Workflow:
 - http://www.imagingcenterinstitute.com/RadInformatics/Volume1_No1/Radinformatics_CTA_0208.asp
 - http://209.85.173.104/search?q=cache:4gicroz9cPMJ:images.ctisus.com/cta_web/12_06/%20AR_12_06_CTA_Jacobs.pdf+%22applied+radiology%22+jacobs+CTA&hl=en&ct=clnk%20&cd=4&gl=us&client=safari
 - http://www.imagingeconomics.com/issues/articles/2004-07_10.asp

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Further Reading

- CTA Interpretation Strategies:
 - Ferencik, M. Radiology 2007;243:696-702
 - Saba, et al. J Comput Assist Tomogr. 2007 Sep-Oct;31(5):712-6.
 - Maintz, D. et al. Am. J. Roentgenol. 2002;179:1319-1322
 - Pugliese, F. et al. Radiographics 2006;26:887-904
- OSIRIX (Free Image Viewer for MAC):
 - <http://www.osirix-viewer.com/>
 - WIKI: http://osirixmac.com/index.php/Main_Page

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