Effects of salience-network-node neurofeedback training on affective biases in major depressive disorder

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1. Introduction

Over the last two decades, neuroimaging investigations of Major Depressive Disorder (MDD) have been instrumental in increasing our understanding of this prevalent and debilitating condition (Kessler and Wang, 2009). Sufficient data have now accumulated from functional neuroimaging investigations of depression that, through meta-analytic integration, we have been able to identify the neural abnormalities that have been found most reliably to characterize this disorder. Specifically, in a recent meta-analysis of studies using task-based functional magnetic resonance imaging (FMRI), we found reliably increased response in fronto-insular cortex, amygdala, and dorsal anterior cingulate cortex (dACC) to negative stimuli relative to neutral stimuli; importantly, we did not observe this pattern with respect to response to positive relative to neutral stimuli in MDD (Hamilton et al., 2012). Based on these findings, we presented a neural account of the well-documented heightened response to negative stimuli in MDD, which has been hypothesized to play a significant role in the etiology and maintenance of this disorder (Beck, 1976; Gotlib and Joormann, 2010). In this formulation, we posit that through monosynaptic projections to the amygdala, dACC, and fronto-insular cortex (Jones and Burton, 1976; Mufson and Mesulam, 1984; Padmala et al., 2010), heightened baseline activity in the pulvinar nucleus in depression (Hamilton et al., 2012) potentiates response of these primary limbic nodes to affective information.

In this model, fronto-insular cortex, dACC, and amygdala — primary nodes in the brain’s salience network (SN), which is postulated to undergird perception of and response to personally relevant stimuli (SN; Seeley et al., 2007) — play a crucial role in biasing the processing of negative information in MDD. This and similar formulations proposed by clinical neuroscientists (e.g., Menon, 2011) are difficult to test directly using traditional
correlates functional neuroimaging paradigms, which typically identify only neural correlates of cognitive or emotional activity. Given this limitation of traditional FMRI paradigms in making causal attributions, in the present study we used an FMRI-based neurofeedback system that allows individuals to see and learn to modulate regional brain responses. The implementation of this method permits investigators to examine the effects on behavior of modulating neural activation (Weiskopf et al., 2004), as opposed to the more typical examination of the effects on the brain of manipulating behavior. Such FMRI neurofeedback systems have now been used successfully to teach healthy individuals to volitionally alter response in sensorimotor (DeCharms et al., 2004), and limbic regions (Caria et al., 2007; Hamilton et al., 2011), and to reduce the experience of pain (DeCharms et al., 2005).

Recent studies using FMRI neurofeedback in MDD have explored the therapeutic utility of this method in depression. A seminal, non-placebo-controlled study showed that it is possible to teach depressed persons to increase ideiographic neural activity associated with positive affect and, in doing so, decrease depressive symptomatology (Linden et al., 2012). Another recent study showed that teaching depressed persons to increase amygdala activity during recall of happy autobiographical memories increases happiness and decreases anxiety in MDD (Young et al., 2014). While not controlling for placebo effects, these studies have provided strong preliminary support for the clinical efficacy of FMRI neurofeedback paradigms.

In the current proof-of-concept study, we take a different perspective relative to previous, clinically oriented work by using FMRI neurofeedback as a tool to test and develop neural models of MDD. For this study, we constructed an experimental paradigm for testing the role of SN node over-response in producing the negative affective biases implicated reliably in MDD. In designing this study, we reasoned that if the SN plays a crucial role in producing negative affective biases in MDD, then teaching depressed persons to decrease responding in SN nodes to negative affective information should decrease affective responding to negative but not positive information. If, on the other hand, learned down-modulation of SN response to negative information has no effect on response to negative information, the hypothesis that the SN plays a critical role in negative affective biases in MDD will be disconfirmed.

To measure the effects of SN-node neurofeedback training (NFT), we assessed responses to both negative and positive stimuli before and after a regimen of NFT. In order to determine effects on affective functioning attributable to NFT as distinct from placebo effects, we also included a group of depressed participants who received sham NFT; that is, the neurofeedback they received was not veridical but, instead, was feedback from other depressed participants who had received real neurofeedback. We predicted, first, that receiving real NFT would lead to successful down-modulation of SN node response; thus, we predicted that, compared with depressed participants who received sham NFT, depressed participants who received real NFT would show reduced response of their most reactive SN node to negative stimuli following NFT. Further, and in accord with the model we present above, we predicted that, relative to their sham NFT counterparts, depressed persons who received real SN NFT would also exhibit reduced affective responding to negative affective challenge. Finally, given that the SN has been conceptualized as part of a negative valence system (Insel et al., 2010) in MDD (Hamilton et al., 2012), we predicted that the effects of real NFT would not generalize to affective responses to positive stimuli.

2. Methods and materials

2.1. Participants

Twenty-two adults diagnosed with MDD initially participated in this study. All participants met criteria for a DSM-IV diagnosis of MDD based on their responses to the Structured Clinical Interview for DSM (SCID; First et al., 2001), administered by trained diagnostic interviewers. Depressed individuals with a current comorbid diagnosis of any Axis-I disorder other than Social Anxiety Disorder (SAD) were not included in the study. Given that we were comparing two groups of depressed participants (real versus sham NFT), we included depressed individuals who were taking antidepressant medication in this study because we would not be confounding medication status with psychiatric diagnosis and, importantly, because this would bolster the generalizability of our findings to the general population of depressed persons, over half of whom take psychotropic medications (Pratt et al., 2011). At the end of the interview session, all participants completed the Beck Depression Inventory-II (BDI-II; Beck et al., 1979) and the Positive and Negative Affect Schedule (PANAS; Watson et al., 1988). The BDI-II and PANAS are frequently used and well validated self-report measures of the severity of depressive symptoms and levels of positive and negative affect, respectively. All stages of the research presented here were carried out in accordance with The Code of Ethics of the World Medical Association (Declaration of Helsinki) for experiments involving human subjects.

To assess cognitive, behavioral, and neural effects of NFT, we assigned participants to one of two groups: REAL, in which participants saw real-time neural response data from a component of their own SN, and SHAM, in which participants saw, in the context of an otherwise equivalent neurofeedback procedure, neural response data from participants in the REAL group instead of their own neural data. We elected to use a sham NFT control group—as opposed to a control group seeing neurofeedback from a control region not implicated in depression—because this form of experimental control is the only way to ensure that the positive and negative reinforcement provided from neurofeedback, and the potential effects of this feedback, on subsequent task performance, were precisely controlled. Importantly, two researchers were involved in NFT scanning: one who interacted with participants and was blind to group assignment and one that ran the NFT interface and who was not blind to group assignment. Further, in keeping with the objective of this study was to investigate the role of the SN in the pathophysiology of MDD, we focused only on the effects of learned modulation of this network.

Given pilot data indicating that 5 out of 6 individuals were successful in using neurofeedback to learn how to control neural response, we first ran 12 participants through the REAL neurofeedback protocol and identified 10 who were successful in using NFT to learn to regulate responding of a functionally defined SN-node (we include performance data for the two non-learners in a supplement to this article). Even though we excluded only a small proportion of our recruited REAL NFT sample, to ensure that this process did not bias our sample (i.e., that selecting successful neuromodulators did not inadvertently also select for factors such as age or severity of depression that might affect performance), we selected and ran through the protocol in a SHAM NFT protocol depressed individuals who were matched to participants from the REAL group with respect to age, education, medication, symptom severity, and comorbidity with SAD. Importantly, all participants provided consent for participation in the NFT procedure knowing that there would be a chance that they would see sham neurofeedback.

2.2. Neurofeedback scanning protocol

2.2.1. Overview

Participants were first shown the neurofeedback interface and neuromodulation task outside of the scanner. In addition, before and after scanning, participants completed two computer-based tasks (described below) to assess response to affective challenge. After entering the scanner, participants underwent a functional-localizer/pre-training assessment scan, three NFT scans, and a post-training assessment scan. Finally, following scanning and assessment, all participants were interviewed about whether they believed the NFT signal was real and, for exploratory purposes, what technique they used to control the NFT signal.

2.2.2. Pre- and post-scanning assessments

To assess changes in affective responding due to NFT, participants completed, both before and after training, an out-of-scanner picture-rating task in which they viewed and rated on a scale of 1–9 the intensity of 15 novel, negatively valenced pictures from the International Affective Picture System (IAPS; Lang and Greenwald, 1993). We used a total of 78 novel, negative IAPS pictures (mean intensity: 4.18; SE: 0.17; mean arousal: 5.11; SE: 0.15) for the behavioral testing and scanning portions of the study (15 for each rating task, 15 for each of the pre- and post-training scans, and 6 for each of three NFT scans). To ensure their appropriateness for use with depressed participants, the negative pictures were all rated by two trained clinicians on a 1–9 scale as reflecting higher levels of sadness than of fear or disgust (mean sadness: 7.5; mean fear: 2.5; mean disgust: 2.0). In addition, before and after NFT, participants completed a brief version of the self-referent encoding
In this task, participants rated on a 1–9 scale the self-relevance of ten positive and ten negative adjectives from the Affective Norms for English Words list (ANEW; Bradley and Lang, 1999), matched with respect to frequency and intensity. For both the picture-rating task and the SRT, stimuli were presented pseudorandomly and counterbalanced such that the words and pictures that were presented before NFT for half of participants were presented after NFT for the other half of the participants.

2.2.3. Scanner and pulse sequence

We conducted fMRI scans using a 3.0 T General Electric Signa MR 750 scanner with an eight-channel, whole-head quadrature imaging coil at the Richard M. Lucas Center for Imaging at the Stanford University School of Medicine. Following whole-brain shimming and high-resolution in-plane anatomical scans, we conducted five fMRI scans [28 sagittal slices with 3.44 mm3 in-plane and 4 mm through-plane resolution, TE = 30 ms, flip angle = 80°, FOV = 22 cm, acquisition time (TR) = 2000 ms per frame, number of frames = 170 per run for each of two assessment scans and 119 per run for each of three neuromodulation scans] using a spiral in/out pulse sequence (Glover and Law, 2001). We used a photoplethysmograph fitted over the left toe to measure heart-rate and a pneumatic respiratory belt fitted around the abdomen to measure respiratory fluctuations.

2.2.4. rtfMRI Software configuration

Processing and analysis of blood-oxygen-level dependent (BOLD) data in real time was conducted with an in-house software suite comprising C/C++ programs and Matlab scripts running on a Linux computer with a socket connection to the scanner for image transfer. At the end of each volume repetition, scanner software reconstructed spiral in-out data (Glover and Law, 2001) from k-space to native brain space and sent it to the rtfMRI computer. The neurofeedback program then calculated a voxel-wise weighted-average of spiral-in and spiral-out acquisitions to optimize signal-to-noise ratio. Reconstructed data were then passed to a module for signal processing and converting data to graphical renderings. For all functional scans, we used this program to co-register individual images to the second functional image of the scan and used multiple regression to factor out effects on BOLD time course and used multiple regression to factor out effects on BOLD signal due to head motion and image processing and analyzing time series data that correlated with a gamma-function-convolved boxcar covariate reflecting the onset and offset of negative IAPS pictures. Directly following the localizer/pre-training assessment scan, we conducted an automatically generated statistical map (overlaid on brain structural data) showing the degree of correlation between voxel time series data and the task covariate. Using this map with a statistical threshold set at p = .05 for each voxel, we identified the single voxel within the SN (dACC, amygdala, or fronto-insular cortex) with a time series that had the highest correlation with the task covariate. We then selected this peak SN voxel and its eight within-plane neighbors as the ROI for NFT (REAL group) or for comparison to the REAL NFT group (SHAM group). We decided to use as the ROI for each participant the most responsive node of the SN rather than the entire SN both to accommodate individual differences in SN responding and to provide the most stable and reliable training signal to the REAL NFT participants. As an additional quality check of this ROI selection process, on the brain-wide BOLD data collected for the localizer scan we conducted simple functional connectivity analysis using the ROI BOLD data for each participant as the seed time series. We hypothesized that if we were, in fact, identifying SN regions with the localizer scan, then we should see significant SN connectivity, across one or more nodes of this network when we combined connectivity maps at the group level. Please see Supplementary Fig. 1 for a summary of these findings.

2.2.5. Prescan preparation

Prior to scanning, participants were introduced to the neurofeedback interface and the task design of the study. They were told that they would see a neurofeedback signal from a brain structure involved in emotional response and that they should try to adopt strategies that brought about a decrease in the response of this structure. Consistent with previous research (Carter et al., 2007), the results of pre-testing indicated that NFT with the SN progressed slowly if participants were not given a set of possible strategies. Therefore, at the outset of scanning, we provided participants in both the REAL and SHAM groups with strategies involving cognitive reappraisal (Ochsner et al., 2002), attentional redirection (Kalisch et al., 2006), and imagery (Jarvinen and Gold, 1981) to try at their discretion (see Supplementary Fig. 2 for a depiction of the trial structure and calculation of SN-node response for NFT scans).

2.2.6. Functional-localizer/pre-training assessment scan

For their first functional scan—designed both to identify a region of interest (ROI) for NFT (REAL group) and to assess pre-training response in this ROI (REAL and SHAM groups)—participants engaged in 15 trials of viewing negative IAPS pictures. Participants were instructed to attend to and stay focused on each picture for the six seconds that it was presented and then to engage in an active control task for 16 s following the offset of each picture. Given that response in neural regions that subserve affect can persist beyond the duration of an affective challenge (Siegle et al., 2002), we used a simple, active control task—pressing a different button (1–4) every two seconds on an MR-compatible keypad—to distract participants from any persisting, ruminative thoughts following the offset of affective stimuli. Our goal in administering this control task was to make analysis of BOLD time-series data more tractable by facilitating deactivation in neural structures activated by emotional stimuli following emotional provocation, thereby increasing coherence between BOLD data and task covariates.

To identify the SN ROI for each participant we used multiple regression to identify voxels in the SN–SN structures were identified during the scanning session in native brain space by an experienced neuroanatomist (JPH)—with corrected time series data that correlated with a gamma-function-convolved boxcar covariate reflecting the onset and offset of negative IAPS pictures. Directly following the localizer/pre-training assessment scan, we consulted an automatically generated statistical map (overlaid on brain structural data) showing the degree of correlation between voxel time series data and the task covariate. Using this map with a statistical threshold set at p = .05 for each voxel, we identified the single voxel within the SN (dACC, amygdala, or fronto-insular cortex) with a time series that had the highest correlation with the task covariate. We then selected this peak SN voxel and its eight within-plane neighbors as the ROI for NFT (REAL group) or for comparison to the REAL NFT group (SHAM group). We decided to use as the ROI for each participant the most responsive node of the SN rather than the entire SN both to accommodate individual differences in SN responding and to provide the most stable and reliable training signal to the REAL NFT participants. As an additional quality check of this ROI selection process, on the brain-wide BOLD data collected for the localizer scan we conducted simple functional connectivity analysis using the ROI BOLD data for each participant as the seed time series. We hypothesized that if we were, in fact, identifying SN regions with the localizer scan, then we should see significant SN connectivity, across one or more nodes of this network when we combined connectivity maps at the group level. Please see Supplementary Fig. 1 for a summary of these findings.

2.2.7. NFT scans

Each participant completed three NFT scans, each of which consisted of six, 34-second trials. Each trial began with six seconds of passive viewing of a fixation cross followed by six seconds of attempting to decrease emotional response while viewing a novel, negative IAPS picture. Following this, participants engaged in the active, button-pressing control task for 16 s before seeing a line graph for six seconds showing the degree of SN response to the negative picture they just viewed, in addition to the SN response on previous trials for that training scan. We defined SN-node response for each trial as the average, noise-covariate corrected BOLD signal for the 4th–7th TRs (h4–h7) following onset of the picture—corresponding to the epoch of peak hemodynamic response resulting from six seconds of picture presentation—minus the average BOLD signal during a baseline epoch comprising the first two TRs (o1–o2) following picture onset, divided by the average of o1 and o2 (see Fig. 1 for a depiction of the trial structure and calculation of SN-node response for NFT scans).

2.2.8. Post-training assessment scan

Following the three NFT scans, participants engaged in a final scan equivalent in structure to the pre-training scan with the exceptions that novel IAPS pictures were used and that upon seeing the negative pictures, participants were asked to invoke the affective regulatory strategy that had proven most effective in reducing the neurofeedback signal they saw during NFT runs; no neurofeedback signal was provided during this post-training scan.

2.3. Analysis

2.3.1. ROI and behavioral data

Given that participants were trained using the neurofeedback index described above, we used this index as the primary dependent variable for assessing the effects of NFT on SN-node response. We first calculated for each participant the average response across trials of the SN ROI for the pre-training and post-training scans and converted these data to a single percent-change index:

\[(i_{post} – training response) – \dfrac{pre}{training response} \times 100\]

We then compared this index of SN-node response change in the REAL and SHAM groups. Similarly, for ratings of the intensity of the IAPS pictures and of the self-relevance of the negative and positive adjectives that were obtained before and after NFT training, we calculated percent-change scores and examined differences in these scores between participants in the REAL and the SHAM groups. Given our a priori directional predictions, we used one-tailed t-tests to compare the REAL and
SHAM groups. Further, we calculated effect sizes of NFT effects (Cohen, 1988). Finally, given that motion can affect BOLD signal, to ensure that participants in the REAL relative to the SHAM group were not learning to move in order to influence their neurofeedback signal, we also compared the REAL and SHAM groups on percent-change indices of the Euclidean norm of the derivatives of their motion covariates and on percent change of correlations between motion and the task timing.

2.3.2. Functional connectivity

To examine whether depressed participants in the REAL group, relative to participants in the SHAM group, recruited additional brain regions in the service of learning to modulate their respective NFT ROIs, we conducted a functional connectivity (FC) analysis—via a procedure described elsewhere (Hamilton and Gotlib, 2008)—using as the seed region each participant’s ROI. Following normalization of each participant’s FC coefficient maps to standard space (Talairach et al., 1988) we conducted a voxel-wise, mixed model, two-by-two analysis of variance (ANOVA) of Group (REAL versus SHAM) repeated over Training (PRE versus POST NFT) using a family-wise error corrected $\alpha = 0.05$. Importantly, this analysis was conducted for exploratory purposes and, given the small sample size and the degrees of freedom used in the two-by-two factorial model, was relatively insensitive to detect effects.

3. Results

3.1. Demographic and clinical measures

As shown in Table 1, the REAL and SHAM groups did not differ significantly with respect to age, years of education, depressive symptomatology, or levels of negative or positive affect (all t-tests $p > 0.15$); further, the two groups also did not differ significantly in the proportion of participants who had comorbid Social Anxiety Disorder or who were taking psychotropic medications (all chi-square $p > 0.15$).

3.2. Neuromodulation

We present in Fig. 2A, the loci of the SN-node ROIs—both in Talairach coordinates and in the context of a brain map—for each of the ten REAL neurofeedback participants. The SN region showing the strongest response during the localizer/pre-training assessment scan was typically in fronto-insular cortex (8 of 10 participants); two participants, however, showed the highest response in the dACC. For comparison purposes, we also identified in the SHAM group the component of the SN that was most responsive during the pre-training scan; as in the REAL group, 8 of the 10 SHAM participants showed the strongest response in fronto-insular cortex and two participants showed the greatest response in the dACC (Talairach coordinates presented in Fig. 2A.). As expected, participants in the REAL NFT group exhibited a greater decrease in SN-node ROI response from pre- to post-NFT than did participants in the SNFT group ($p = 0.06$; Cohen’s $d = 0.70$; see Fig. 2B). More specifically, REAL and SHAM groups did not differ with respect to ROI response before NFT ($p > 0.10$), ROI response did not change from pre- to post-NFT in the SHAM group ($p > 0.10$), but ROI response did decrease significantly in the REAL NFT group ($p < 0.05$). Importantly, in none of the three NFT runs did the REAL and SHAM groups differ with respect to ROI response; this is perhaps not surprising, however, given that several participants reported trying both to increase and decrease the NFT signal during NFT runs in order to get a better sense for cause and effect relations between NFT strategies and ROI activity. Finally, the REAL and SHAM groups did not differ in pre- to post-NFT either in absolute motion or in the correlation between motion and task timing (both $p > 0.15$).

3.3. Affective responses

Compared with the SHAM NFT group, the REAL NFT group showed a greater decrease from pre- to post-NFT in emotional response to negative IAPS pictures ($p < 0.05$; Cohen’s $d = 0.78$; see Fig. 2C) and in ratings of self-relevance of the negative adjectives ($p = 0.06$; Cohen’s $d = 0.73$; see Fig. 2D); the two groups did not differ in the change from pre- to post-NFT in their ratings of the self-relevance of the positive adjectives ($p > 0.15$; $p > 0.15$; Cohen’s $d = 0.24$). In neither group did changes in IAPS or self-relevance ratings correlate significantly with changes in SN response. See Supplemental Fig. 2 for performance data from the REAL and SHAM groups in addition to the two EXCLUDED participants.

3.4. Functional connectivity

Our FC analysis identified no regions that changed connectivity with participant ROIs as a function of NFT training in the REAL group relative to the SHAM group. To augment this analysis, we also calculated at all voxels the degree of response to the emotion regulation task in all participants for both the pre- and post-training scans and then entered these estimates into a two-(Group) -by-two (Time) factorial analysis of variance. See Supplemental Fig. 3 for the results of this analysis.

3.5. Post NFT and assessment debriefing

All participants from both the REAL and SHAM groups believed that the NFT signal they saw was a real NFT signal from their own brain.

4. Discussion

The present study was designed to test the hypothesis that the SN plays a critical role in the negative affective bias reliably associated with MDD (Beck, 1976; Gotlib and Joormann, 2010). To test this hypothesis, we examined whether learning to control reactivity of nodes of the SN using NFT during negative affective provocation affected emotional response in MDD. Consistent with our hypotheses, we found that compared with depressed persons who received SHAM NFT, depressed persons who received REAL NFT learned to control reactivity in components of the SN and, as a result of NFT, showed decreased emotional response to negative, but not to positive, stimuli. These findings have important implications for neural conceptualizations of depression.

Theorists have postulated that cognitive biases facilitating the processing of negative material in depression contribute to the etiology and maintenance of this disorder (Beck, 1976; Gotlib et al., 2004). In a synthesis of functional neuroimaging investigations of MDD, we identified a small number of structures showing reliable

<table>
<thead>
<tr>
<th>Sample size</th>
<th>Age</th>
<th>Years education</th>
<th>Proportion receiving psychotropic medication</th>
<th>Proportion with comorbid social anxiety disorder</th>
<th>BDI-II</th>
<th>PANAS-Negative</th>
<th>PANAS-Positive</th>
</tr>
</thead>
<tbody>
<tr>
<td>REAL 10</td>
<td>31.2 (± 2.9)</td>
<td>16.4 (± 0.83)</td>
<td>60%</td>
<td></td>
<td>30%</td>
<td>33.3 (± 2.3)</td>
<td>36.7 (± 3.8)</td>
</tr>
<tr>
<td>SHAM 10</td>
<td>34.5 (± 3.7)</td>
<td>17.0 (± 0.75)</td>
<td>40%</td>
<td></td>
<td>20%</td>
<td>34.6 (± 4.0)</td>
<td>31.3 (± 3.6)</td>
</tr>
</tbody>
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Note: all between-group comparison $p > 0.15$; BDI—Beck Depression Inventory; PANAS—Positive and Negative Affect Schedule
over-response to negative stimuli in MDD and postulated that, among these, the nodes of the SN play a primary role in contributing to negative processing biases in depression (Hamilton et al., 2012). In the present study we showed that teaching depressed individuals to decrease SN-node reactivity leads to a reduction in emotional reactivity to negative stimuli. Importantly, we found no evidence of involvement of non-SN structures in this SN-NFT effect. These findings, considered alongside the putative functional role of the SN (Seeley et al., 2007), are consistent with the formulation that nodes of the SN play a key role in negative processing biases in MDD. It is important that we note here that participants learned to control as opposed to reduce NFT ROI response given that several participants reported trying both to decrease and increase NFT reactivity during the training runs. The neural and behavioral effects of NFT, therefore, may be best conceptualized as resulting from general mastery of ROI response as opposed simply from learning to decrease ROI reactivity.

We should note four limitations of the present study. First, we did not include a healthy control group in this study that could allow us to replicate the documented finding of heightened SN response to negative affective challenge in MDD. Rather, based on meta-analytic results presented above (Hamilton et al., 2012), we assume here that elevated response to negative stimuli in nodes of the SN is reliable in MDD. Second, like recent preliminary investigations of neurofeedback effects in MDD (Linden et al., 2012; Young et al., 2014), our proof-of-concept investigation of SN NFT effects on negative processing biases in MDD incorporated a relatively small sample. While we observed large effects of NFT both on changes in SN node responding and on responses to negative affective challenge—with Cohen’s d scores all .70 or higher (Cohen, 1988)—it will be important in subsequent work to examine NFT effects in larger depressed samples. Further, we hasten to point out that our objectives in this study were to examine short-term neural and behavioral changes resulting from NFT; thus, the data we present are equivocal with respect to any long-term effects of learning to modulate the SN. Finally, based on results from early piloting that healthy males were relatively ineffective at learning to control neurofeedback signals from regions involved in affective responding, we recruited only female MDD participants for this study; our results, therefore, may not generalize to the full population of individuals with MDD.

While we designed this study as a critical test of the hypothesis that SN over-response plays a vital role in negative affective biases in MDD, the present results do have potential implications for non-pharmacological neural interventions for depression. Specifically, along with recent and more clinically oriented work (Linden et al., 2012; Young et al., 2014) our findings indicate that NFT may be a useful therapeutic tool for depression. In this context, however, it is important to acknowledge that we did not examine the effects of NFT on depressive symptomatology, but instead, given our formulation that SN over-response affects acute but not chronic emotional expression in MDD, we assessed its effects on affective response. Subsequent investigations should test this formulation more explicitly by examining the effects of multiple NFT
sessions on mood and diagnostic status in MDD, and by assessing the effectiveness of NFT as a supplement to, or in lieu of, more traditional cognitive-behavioral therapies for depression. Finally, given that fMRI-based neural interventions have a number of exclusion criteria (e.g., claustrophobia, weight restrictions) it will be important in future work to identify peripheral biomarkers of effective neural regulation (e.g., changes in electroencephalographic or cardiac measures) for use in more traditional biofeedback paradigms.

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Appendix A. Supplementary material

Supplementary data associated with this article can be found in the online version at http://dx.doi.org/10.1016/j.pscychresns.2016.01.016.

References